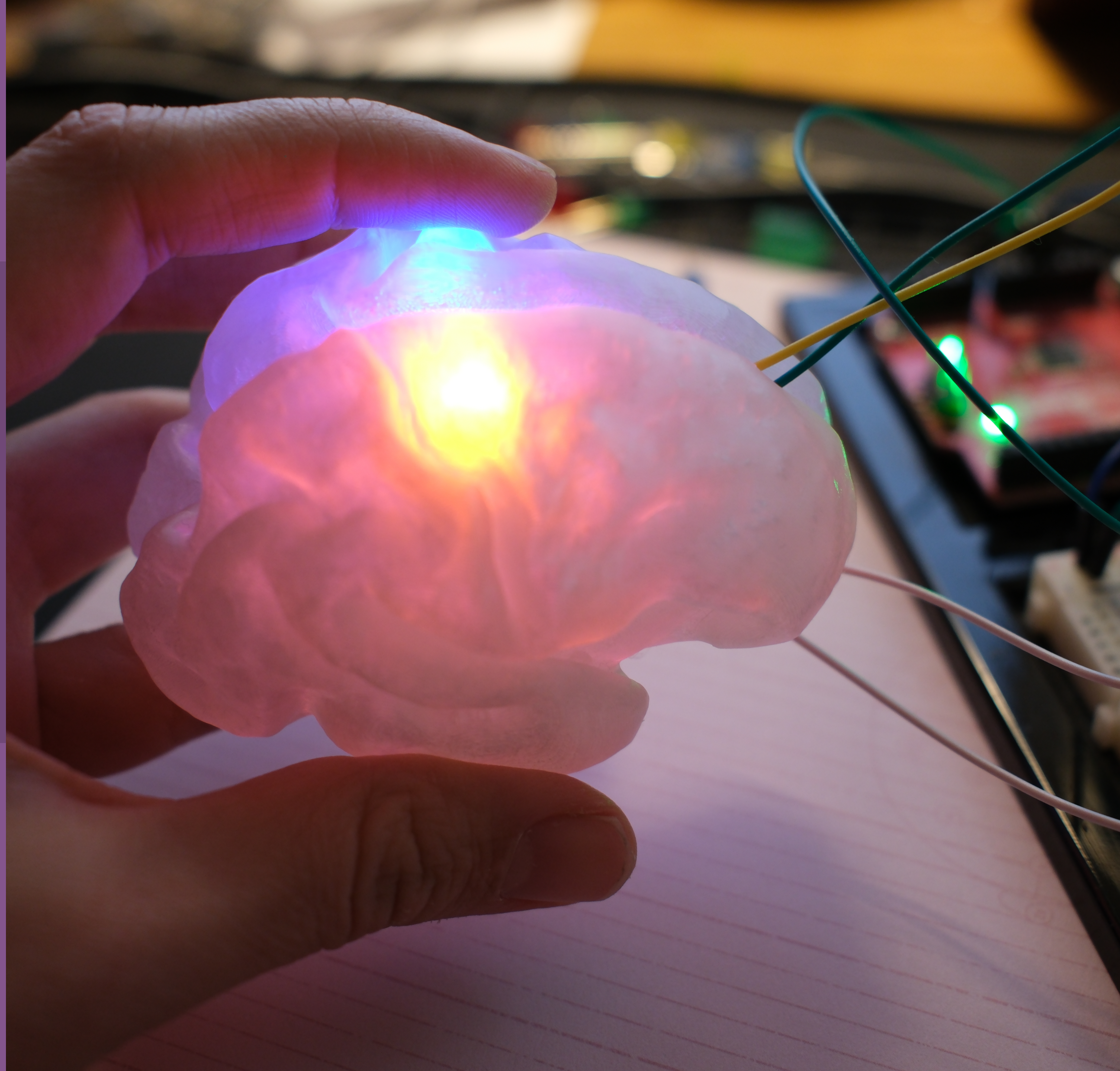


Spectral & Time-Frequency Analysis

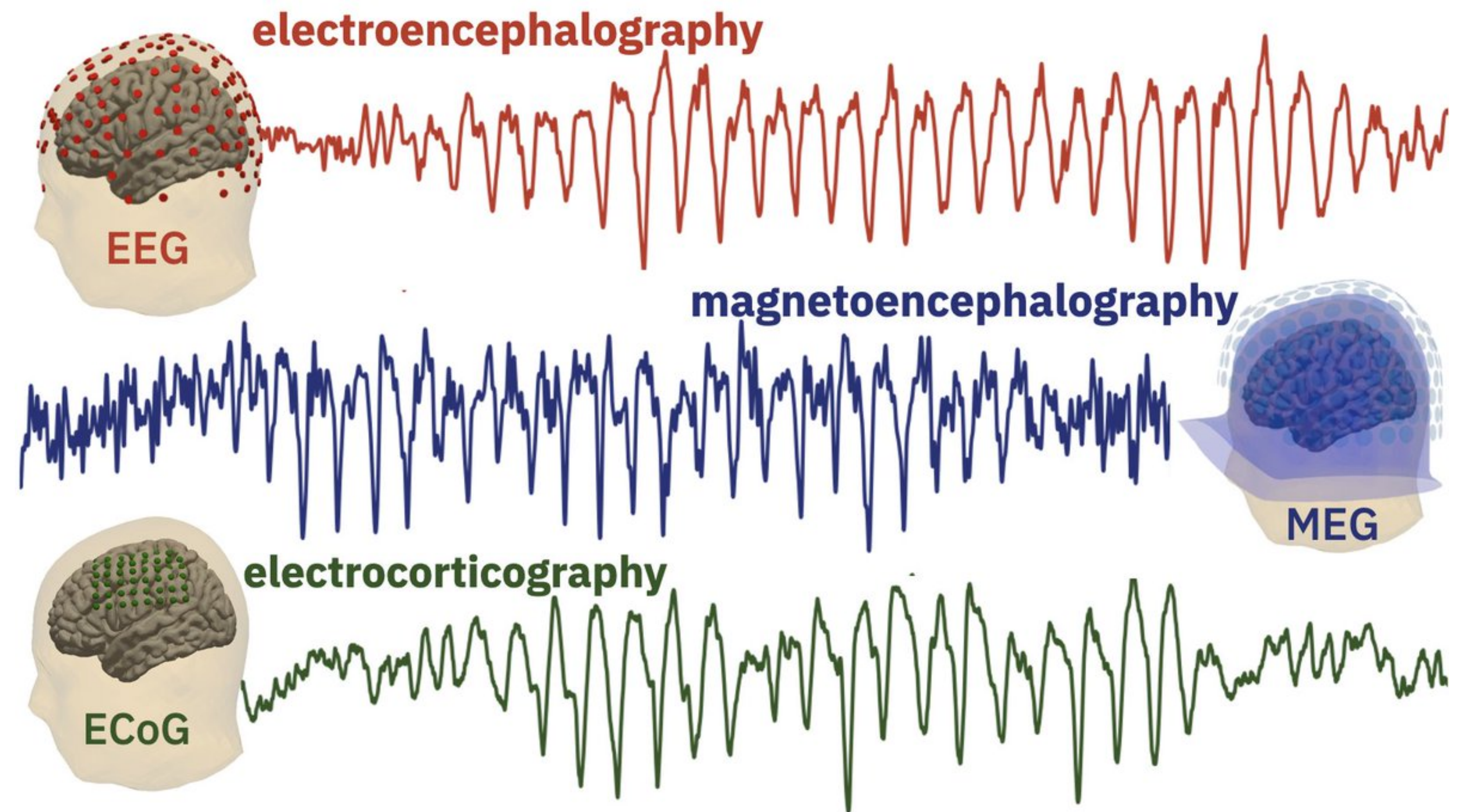
Natalie Schaworonkow

Oct 28th 2025



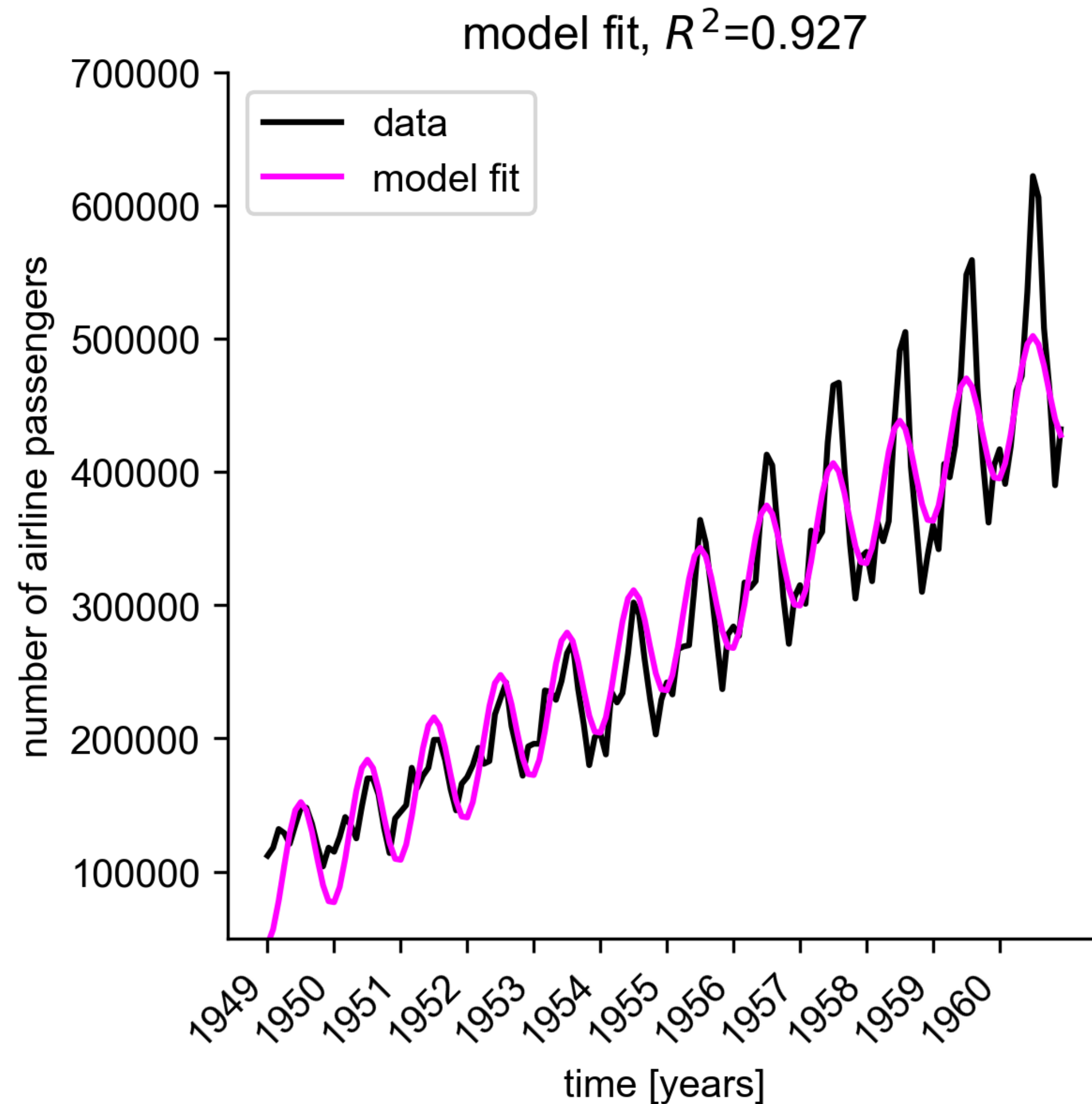
Outline

1. spectral analysis – computation
2. spectral analysis – interpretation
3. time-frequency analysis
4. volume conduction



spectral analysis – computation

motivation



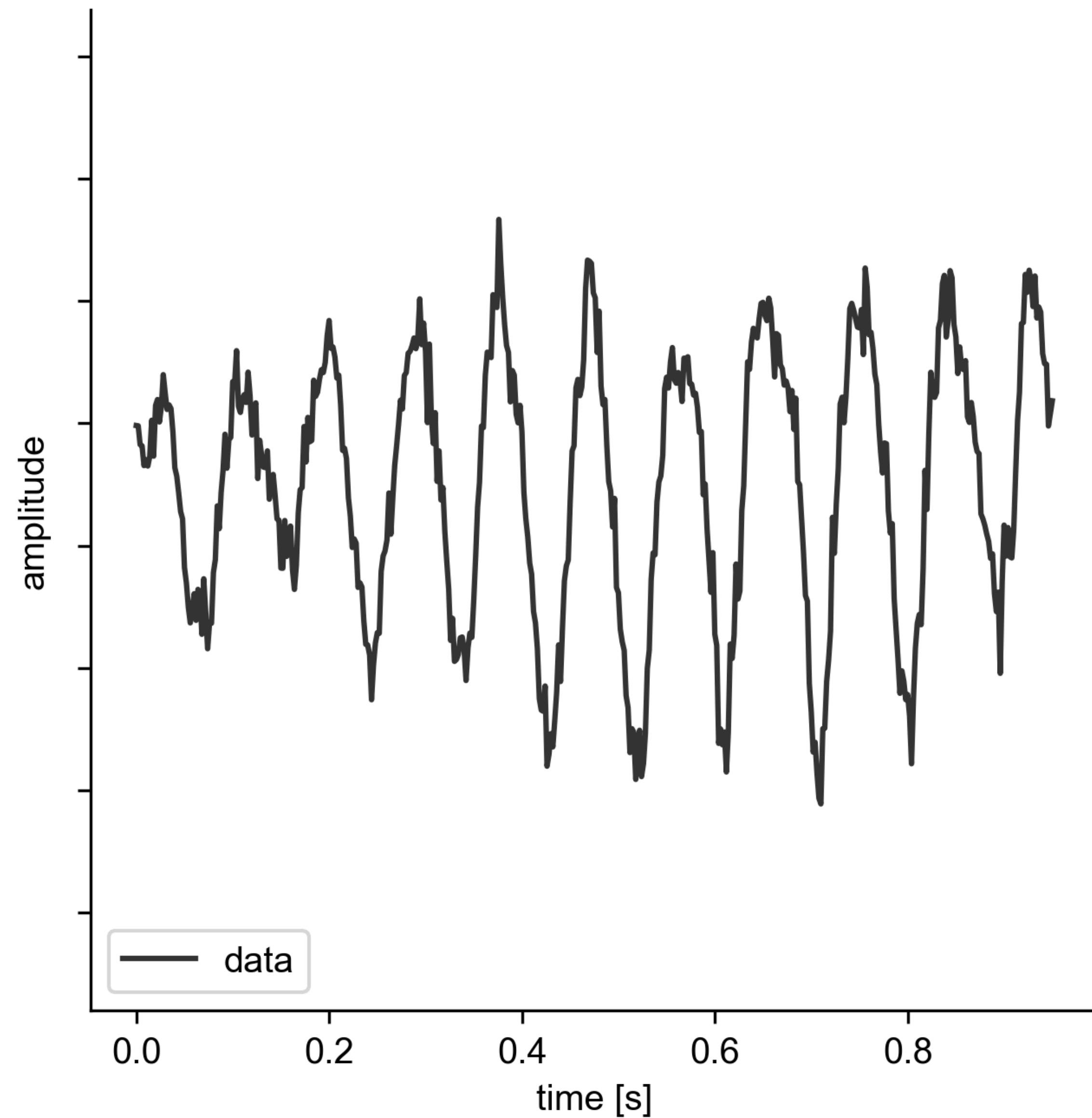
- how to detect systematic patterns in data?
- express measured data as a linear combination of several factors
- fit a model consisting of two factors
 - $\text{data} \sim \text{coeff}_1 * X_1 + \text{coeff}_2 * X_2$
here: linear sine

purpose

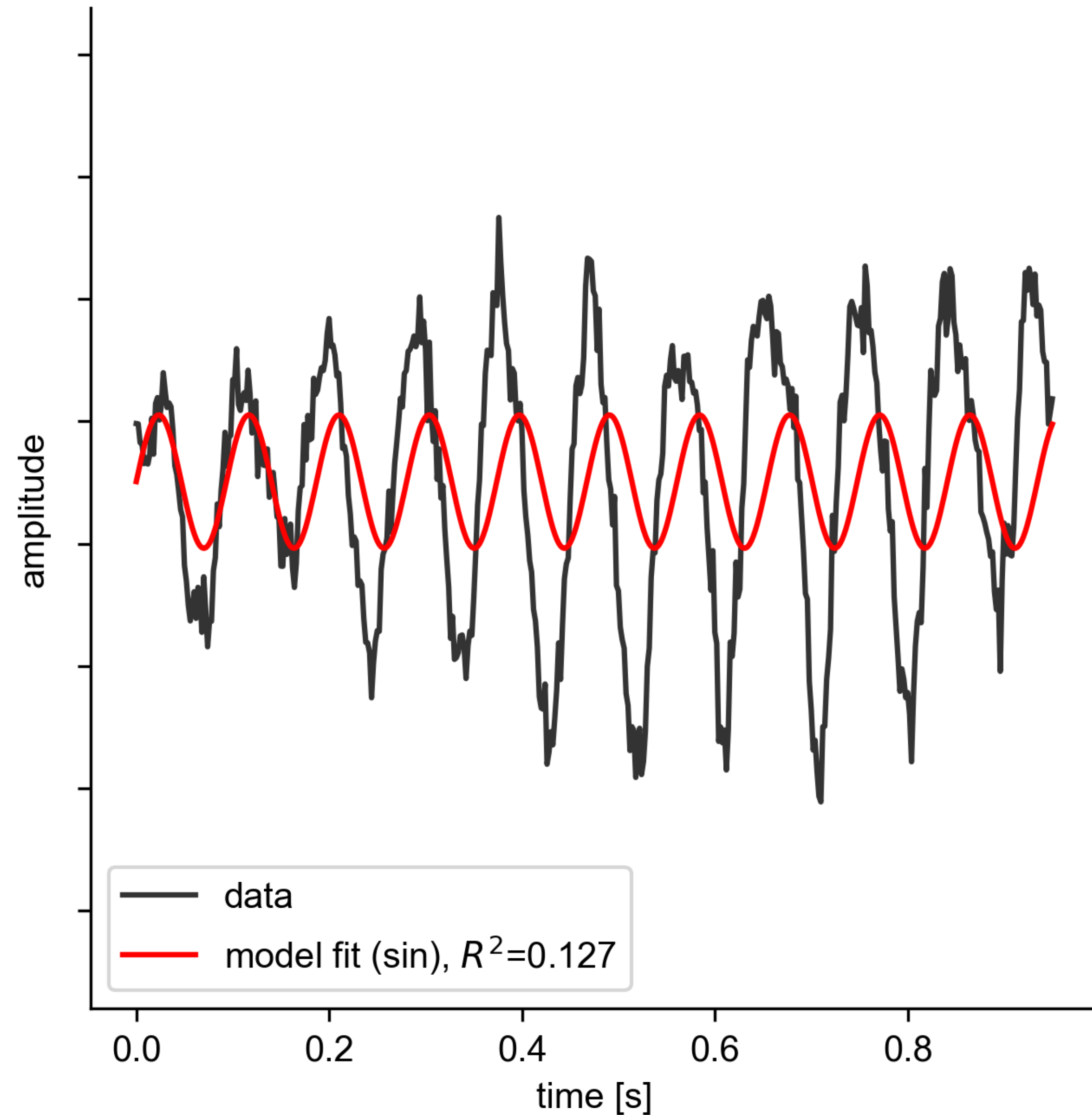
- description of data in an efficient way
- explain the data

data + model fitting

- 1 second of EEG data (500 data points)

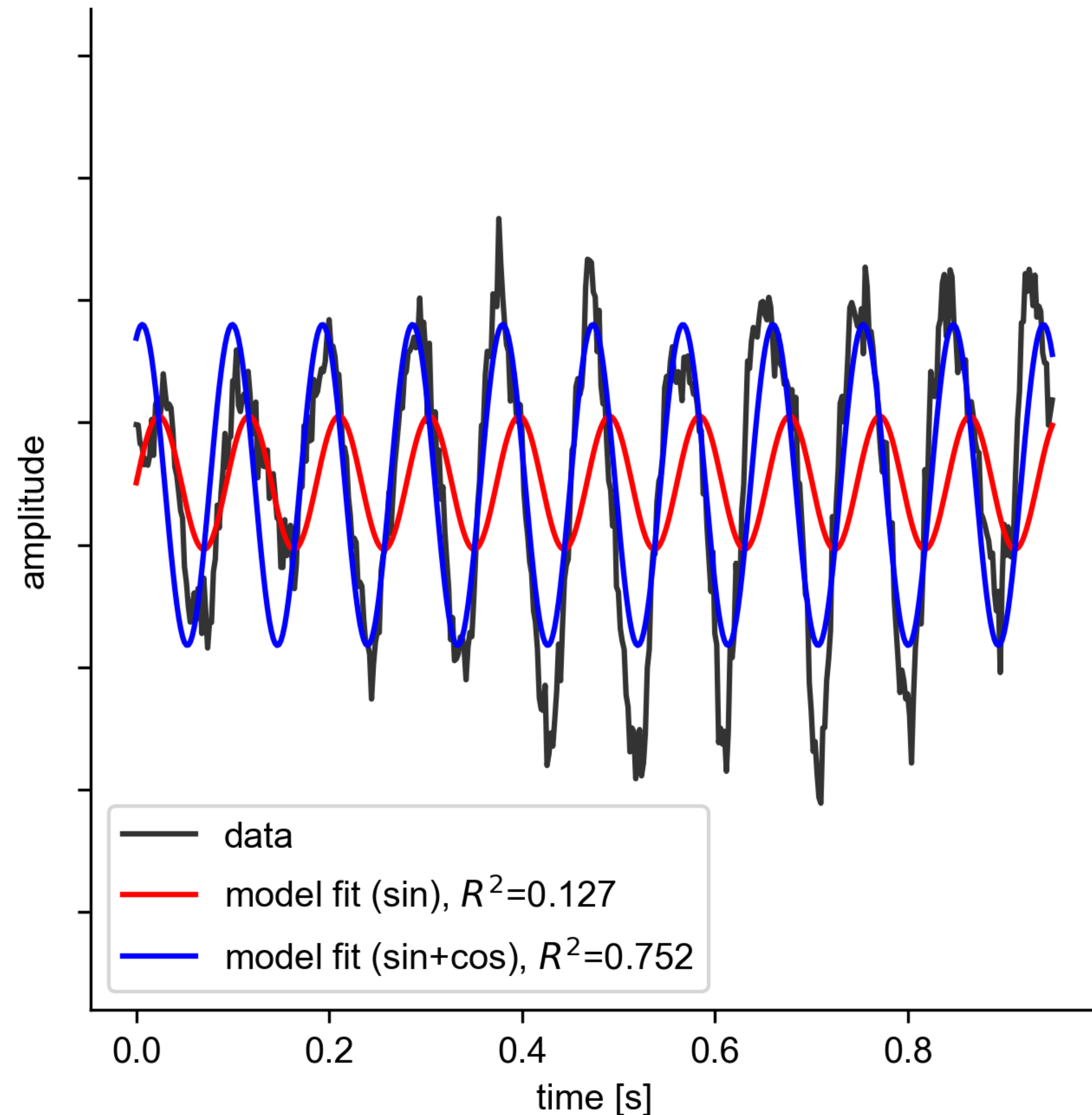


data + model fitting



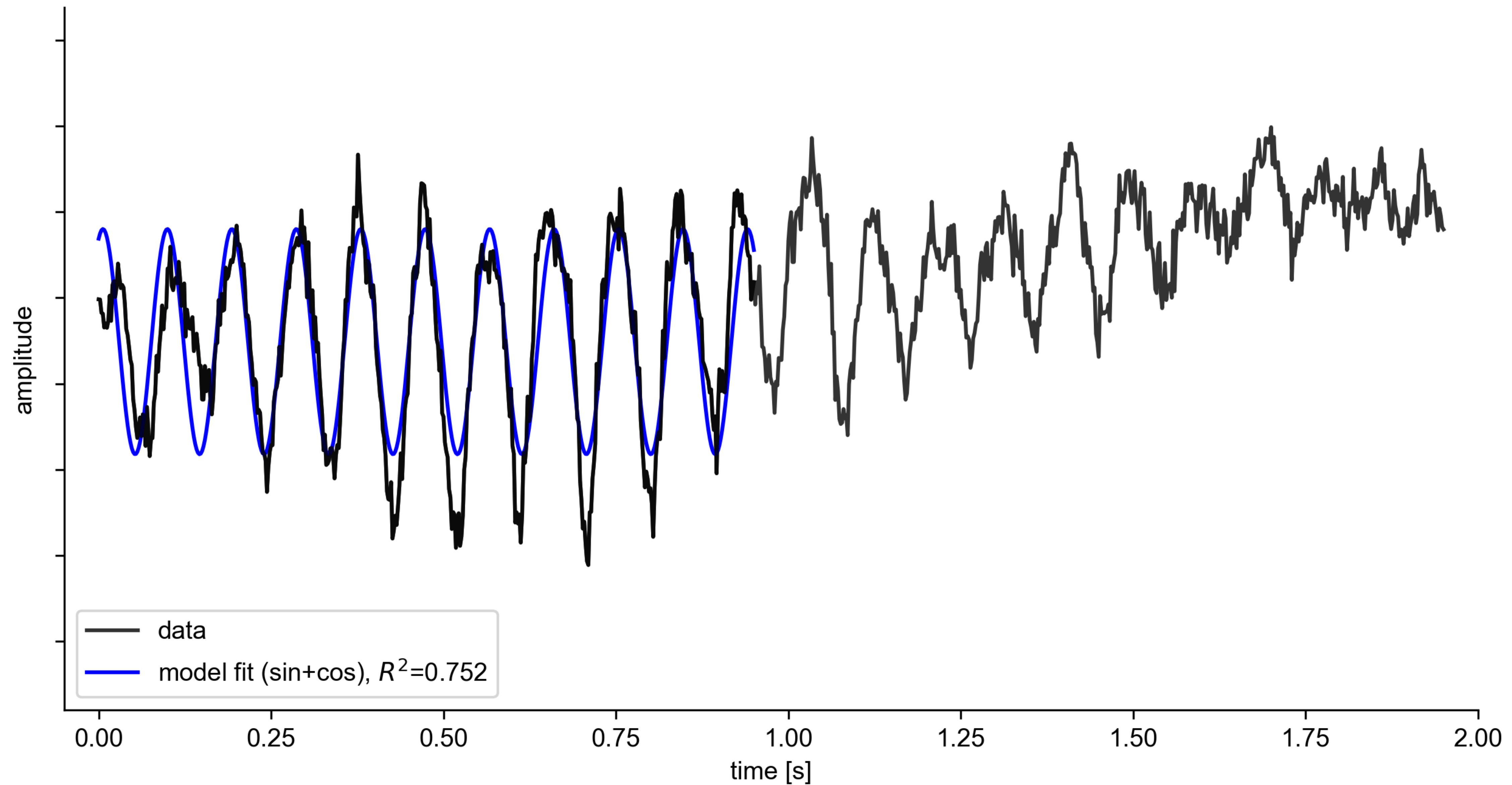
- 1 second of EEG data (500 data points)
- **attempt 1:**
model fit with 1 sine with fixed frequency
 $\text{data} \sim \text{coeff}_1 * \text{sine}_1$

data + model fitting

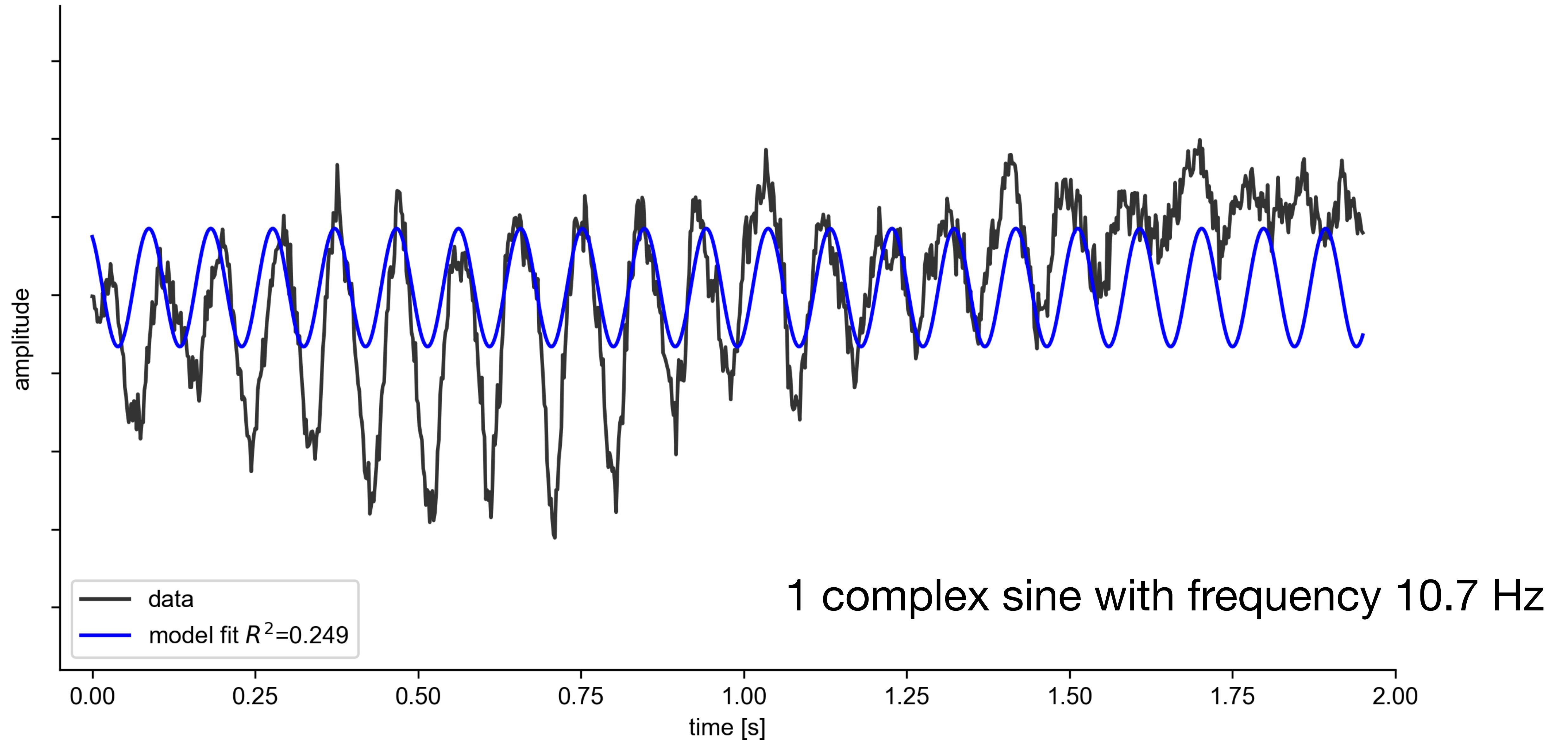


- 1 second of EEG data (500 data points)
- **attempt 1:**
model fit with 1 sine with fixed frequency
$$\text{data} \sim \text{coeff}_1 * \text{sine}_1$$
- **attempt 2:**
model fit with 1 complex sine (sine + cosine) with fixed frequency
$$\text{data} \sim \text{coeff}_{1A} * \text{sine}_1 + \text{coeff}_{1B} * \text{cosine}_1$$

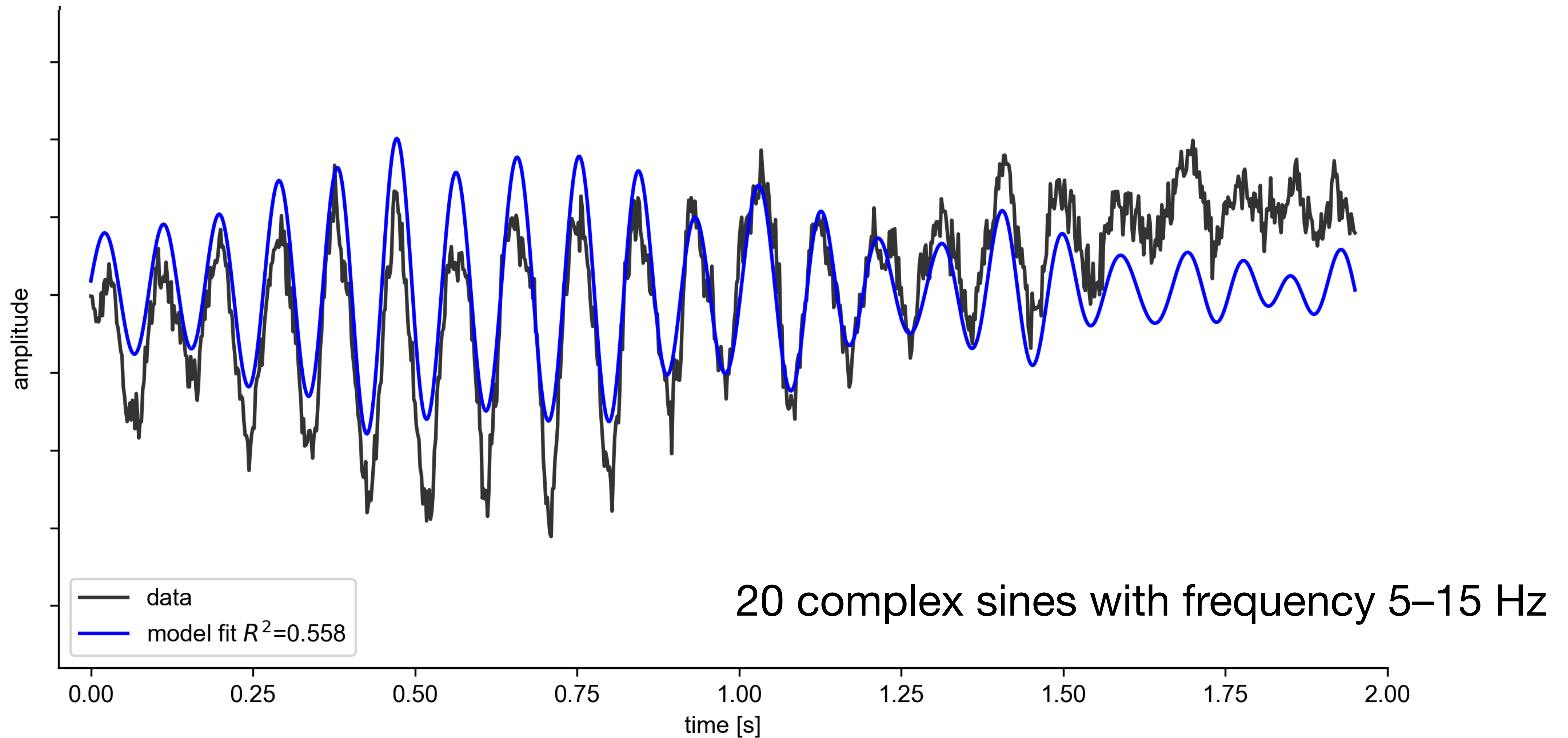
data + model fitting



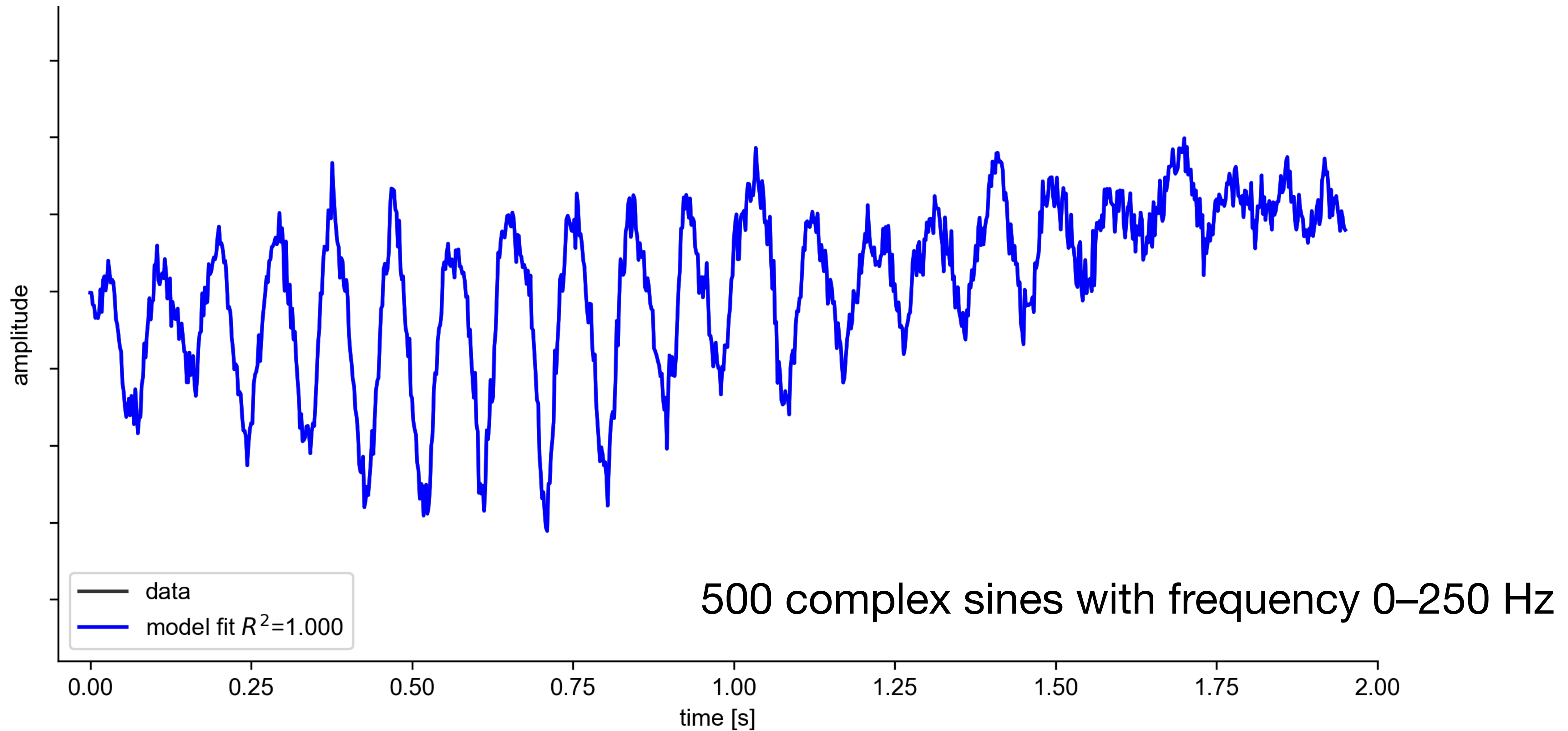
data + model fitting – more data



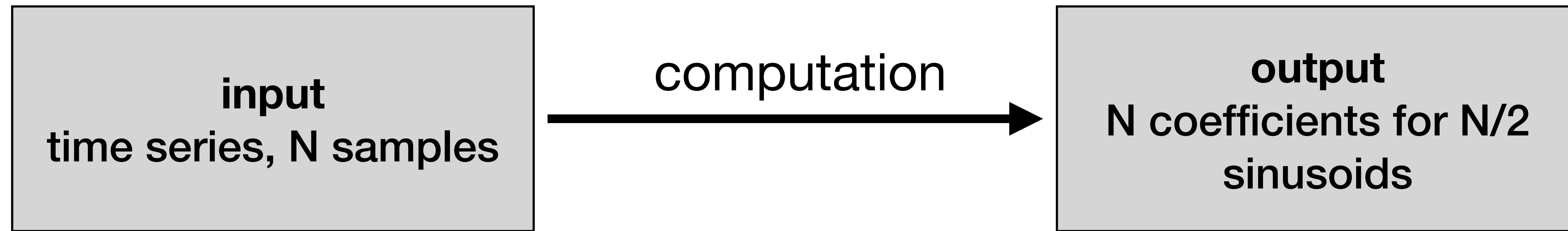
data + model fitting – more data



data + model fitting



concepts / different views



two views on the same procedure

statistical modeling

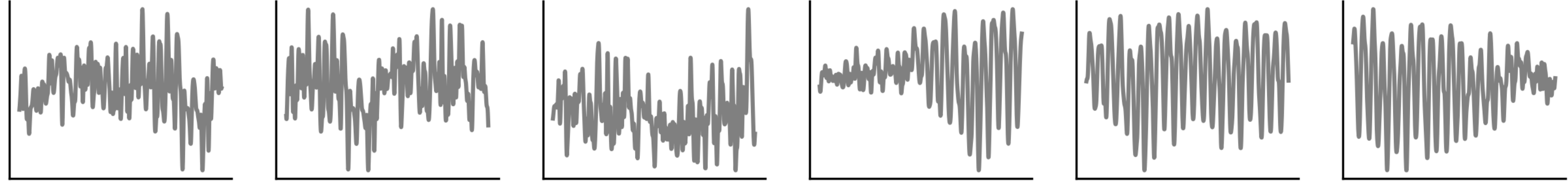
- “multivariate linear model with complex sinusoids as regressors”
- no degrees of freedom, no remaining residual → overfitting

signal processing

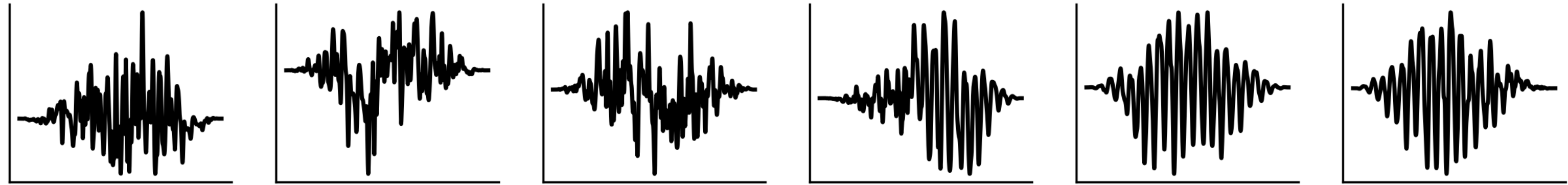
- “Fourier transform”, a transform into the spectral domain
- signal representation, perfect reconstruction possible

computation: Welch's method

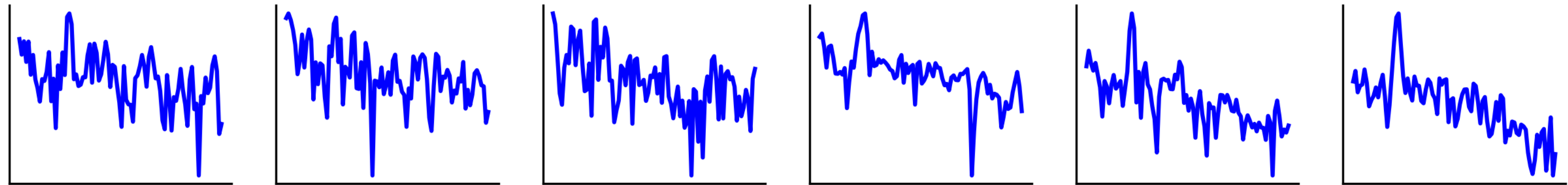
time series, cut into small segments
[nr_segments x nr_samples]



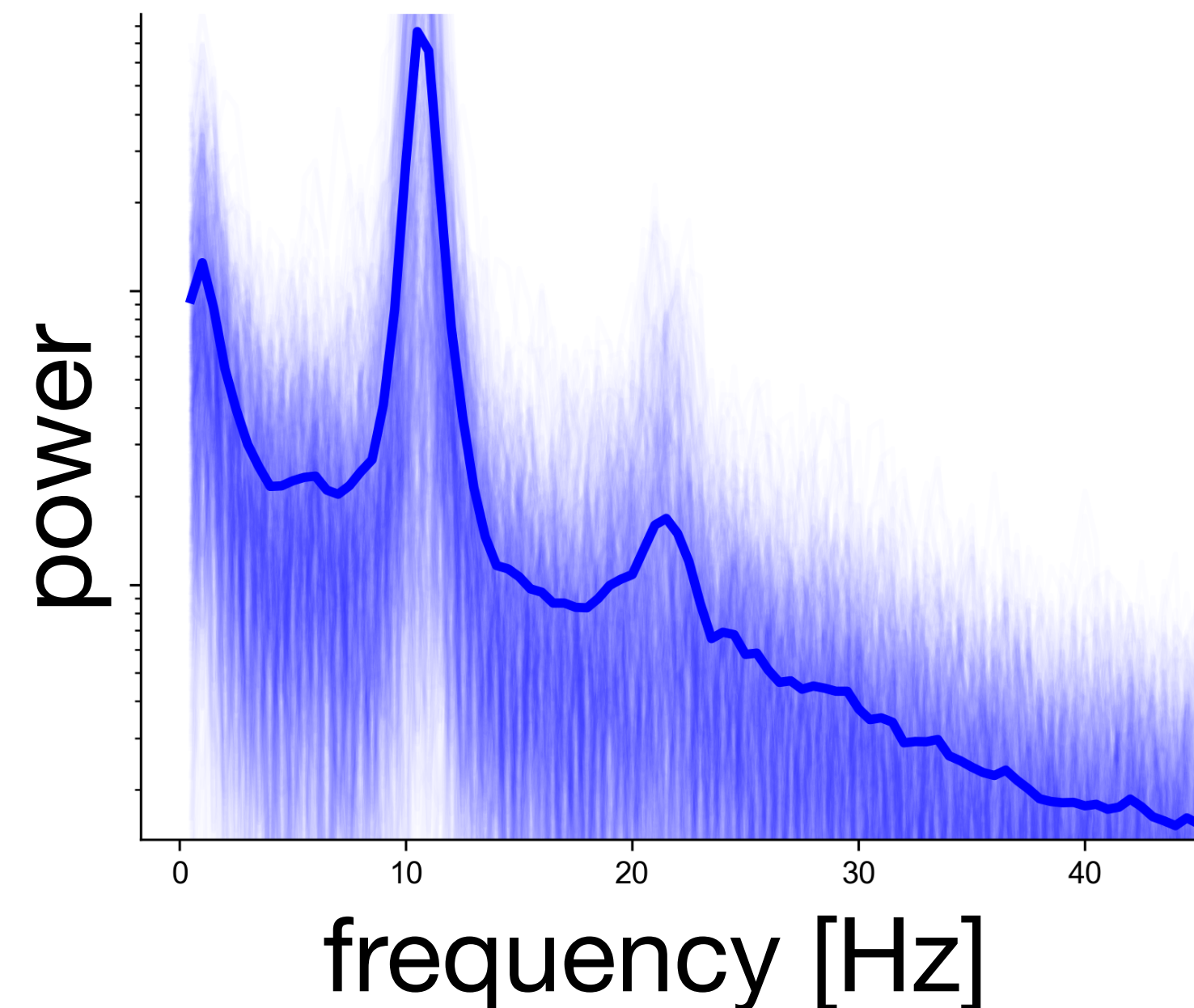
time series, multiplied with a
windowing function
[nr_segments x nr_samples]



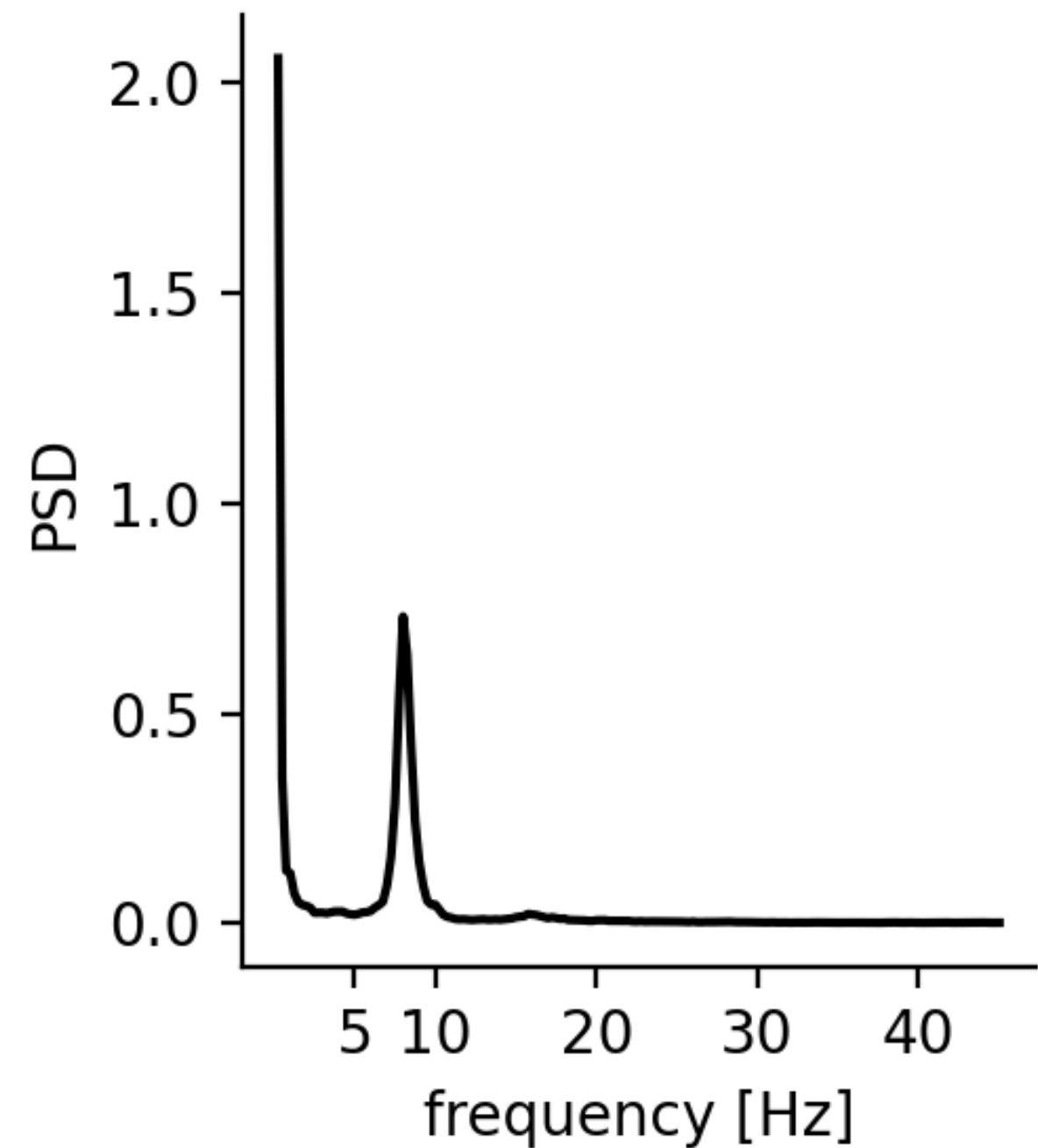
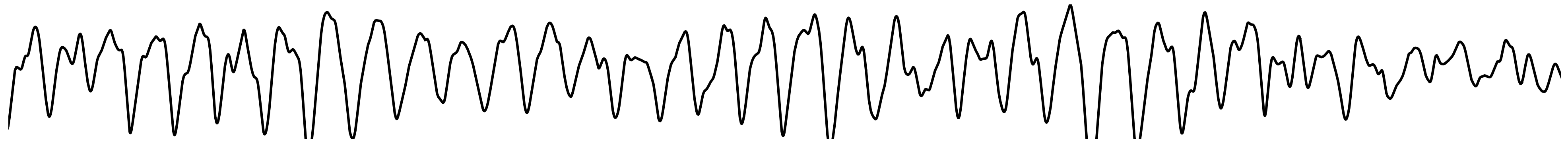
spectra for each segment
[nr_segments x nr_frequencies]



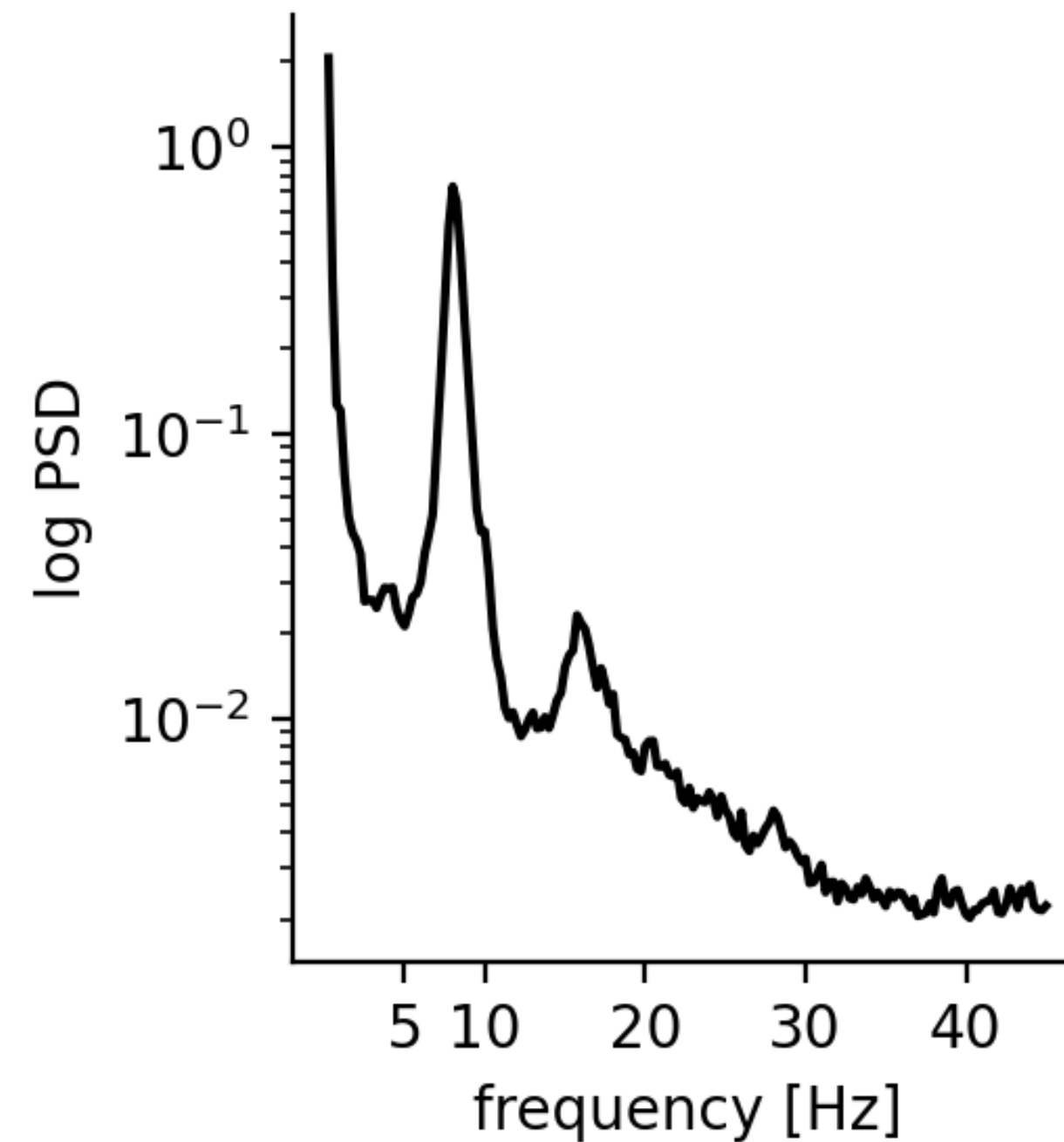
average across frequencies to
obtain the spectrum
[1 x nr_frequencies]



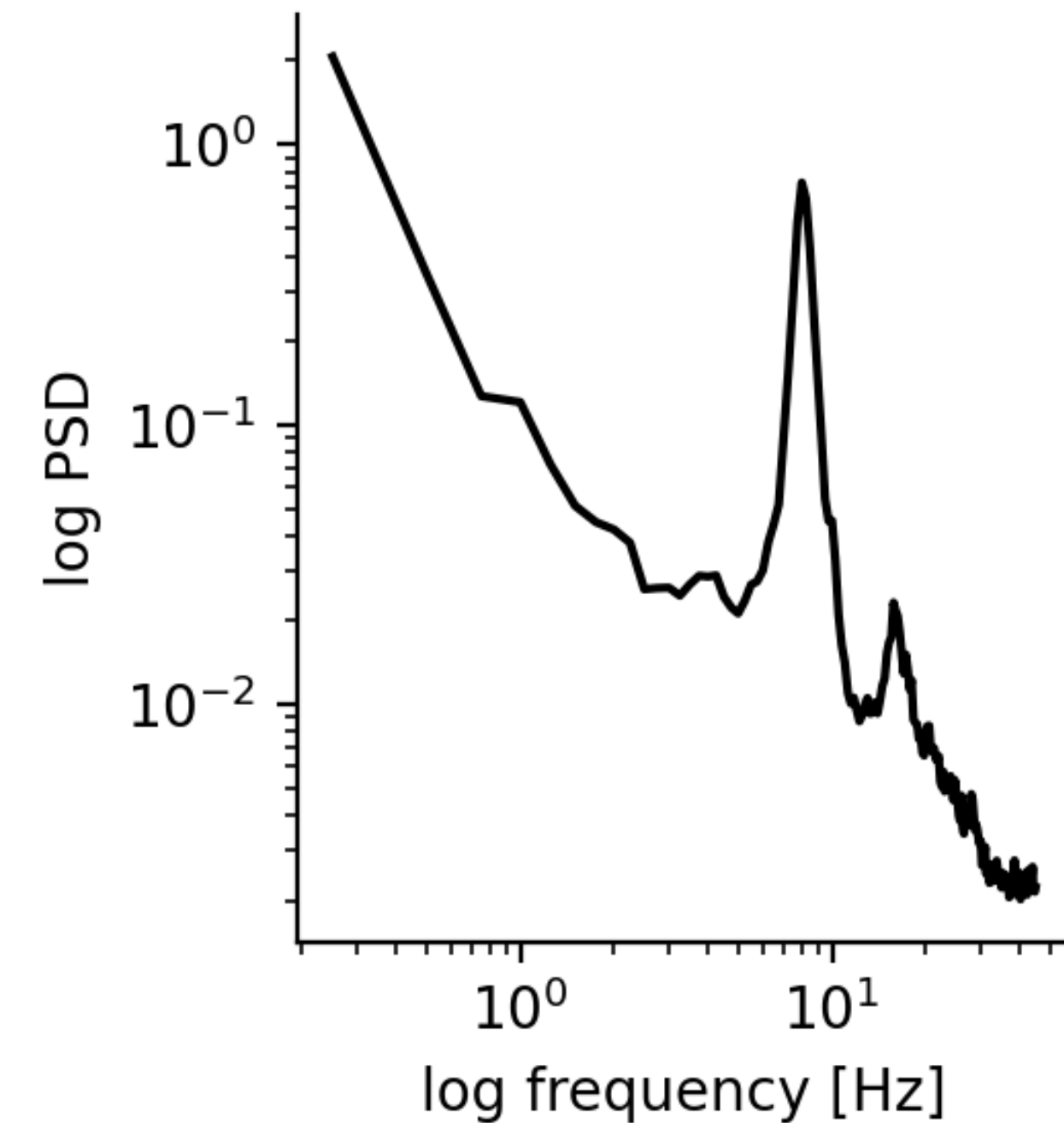
example output for real EEG data



linear-linear



linear-log



log-log

different ways to show the same output of the spectral estimation

methods: parameters in general

common spectral analysis parameters

- length of data segments
- number of points per segment
- percentage of overlap
- type of taper

What are the “correct” parameters?

Choice depends on analysis goal. Different parameters enable flexibility in analysis.

if in doubt:

- starting point: take the ones from your elders / previous literature
- change parameters and observe effects, effects should be robust for similar parameters
→ sensitivity analysis
- simulate!

methods: frequency resolution

- frequency resolution of the spectrum depends on the number of used samples for each segment

Example

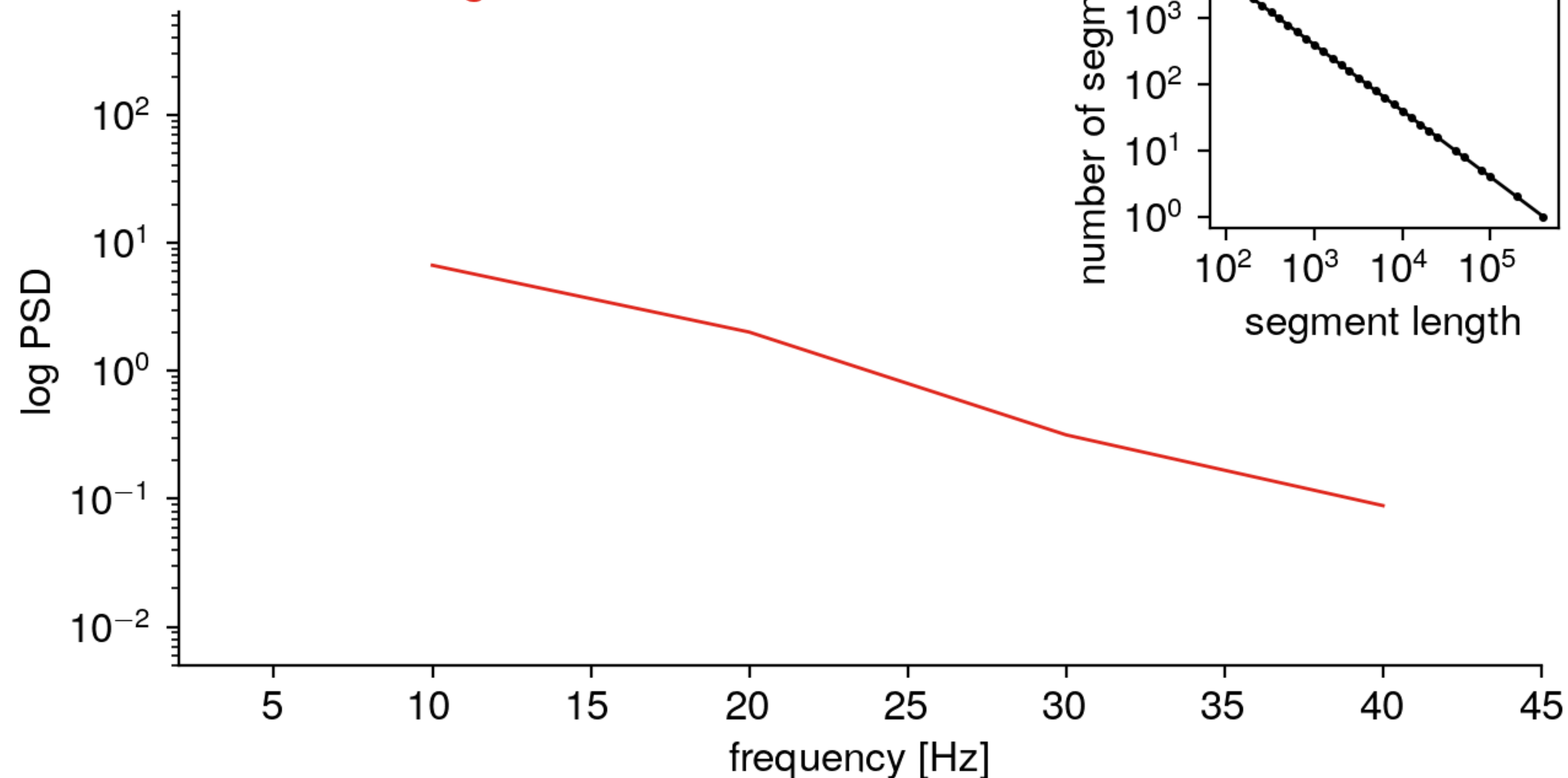
frequency resolution

- segment length: $1\text{ s} \rightarrow 1 \quad 2 \quad 3 \quad 4 \quad \dots \text{ Hz}$
- segment length: $2\text{ s} \rightarrow 0.5 \quad 1 \quad 1.5 \quad 2 \quad \dots \text{ Hz}$
- segment length: $0.1\text{ s} \rightarrow 10 \quad 20 \quad 30 \quad 40 \quad \dots \text{ Hz}$

methods: frequency resolution

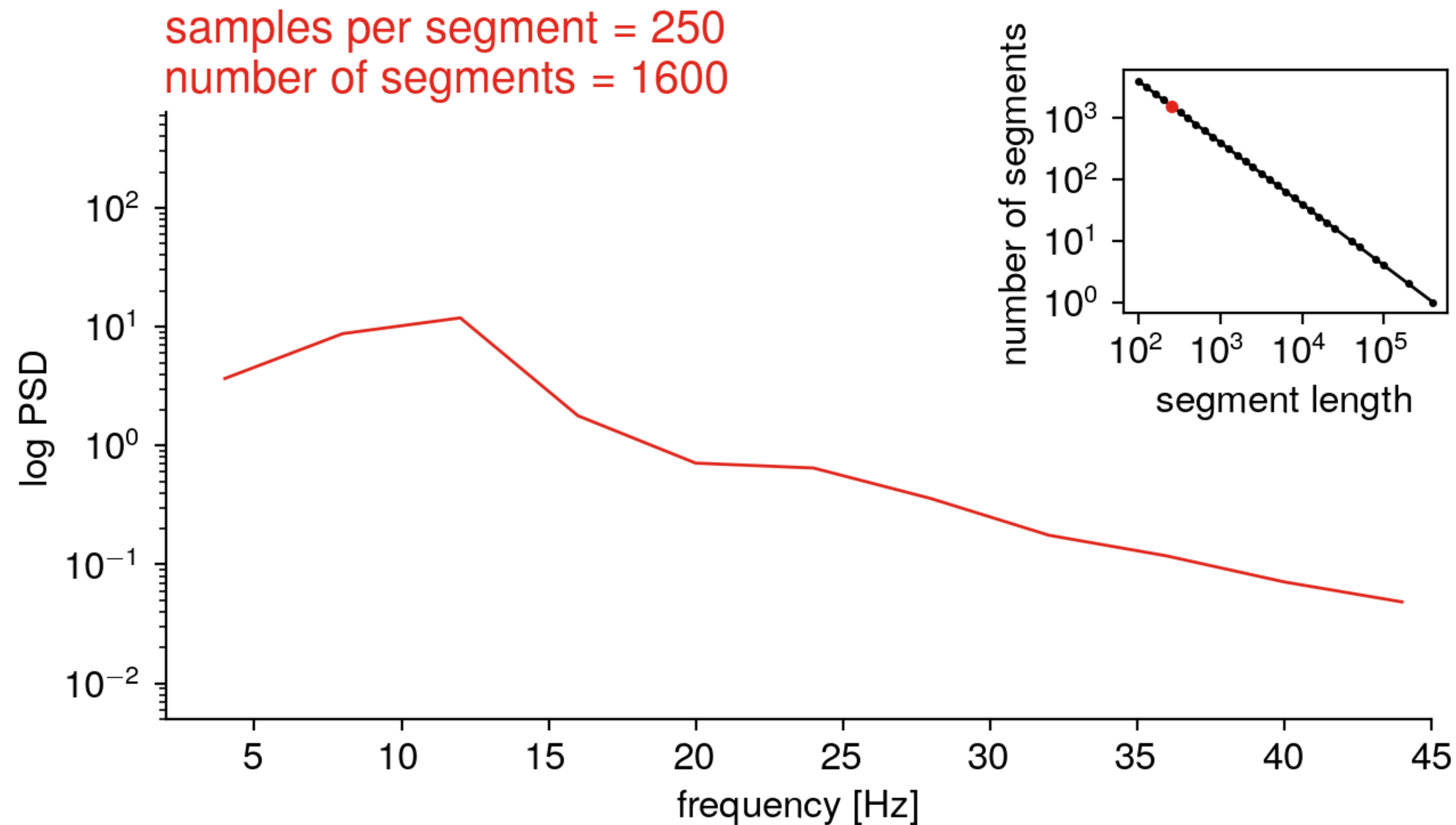
- changing the settings how many samples per segment are used determines frequency resolution.

0.1 s = samples per segment = 100
number of segments = 4000



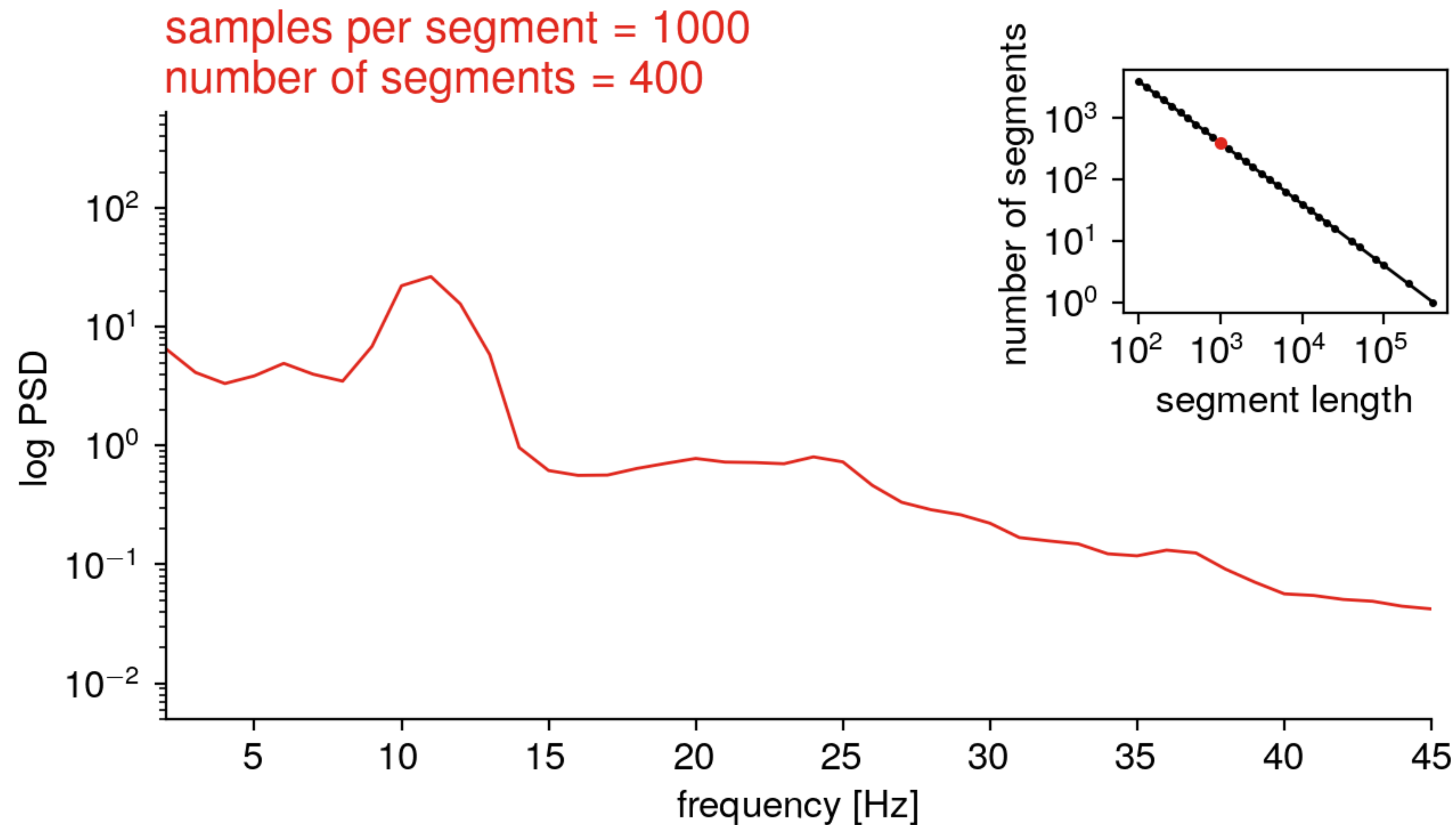
methods: frequency resolution

- changing the settings how many samples per segment are used determines frequency resolution.



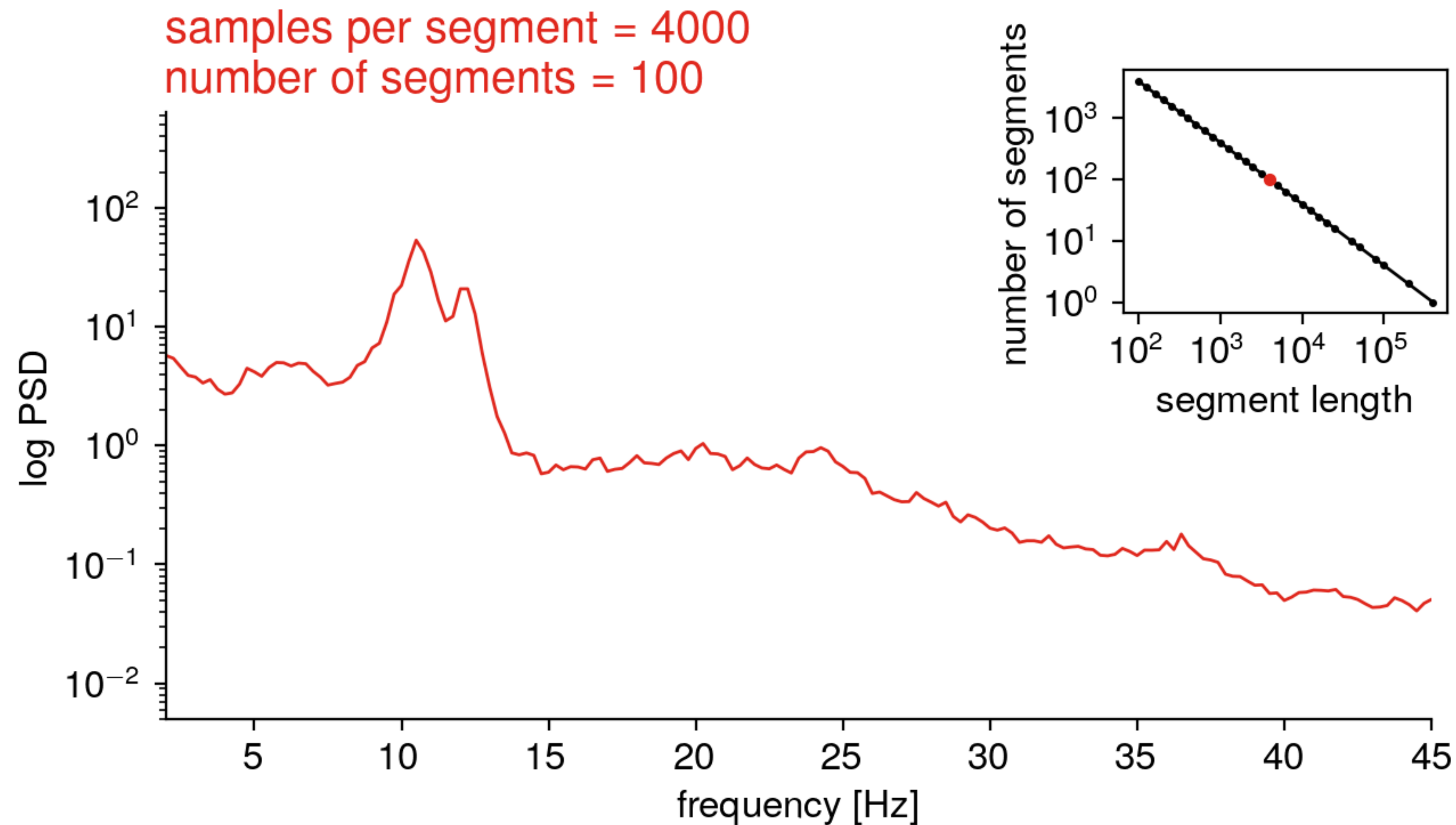
methods: frequency resolution

- changing the settings how many samples per segment are used determines frequency resolution.



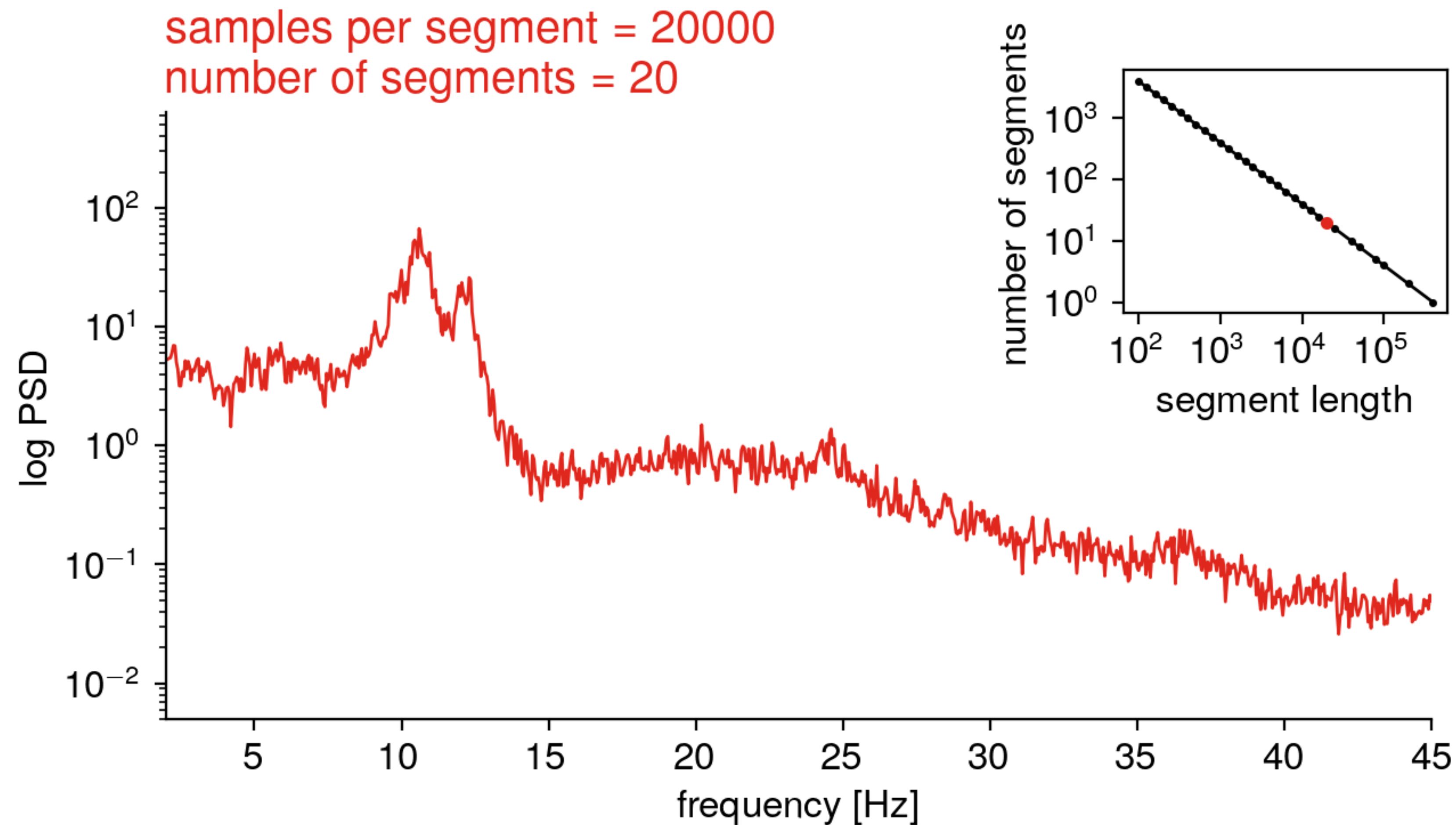
methods: frequency resolution

- changing the settings how many samples per segment are used determines frequency resolution.



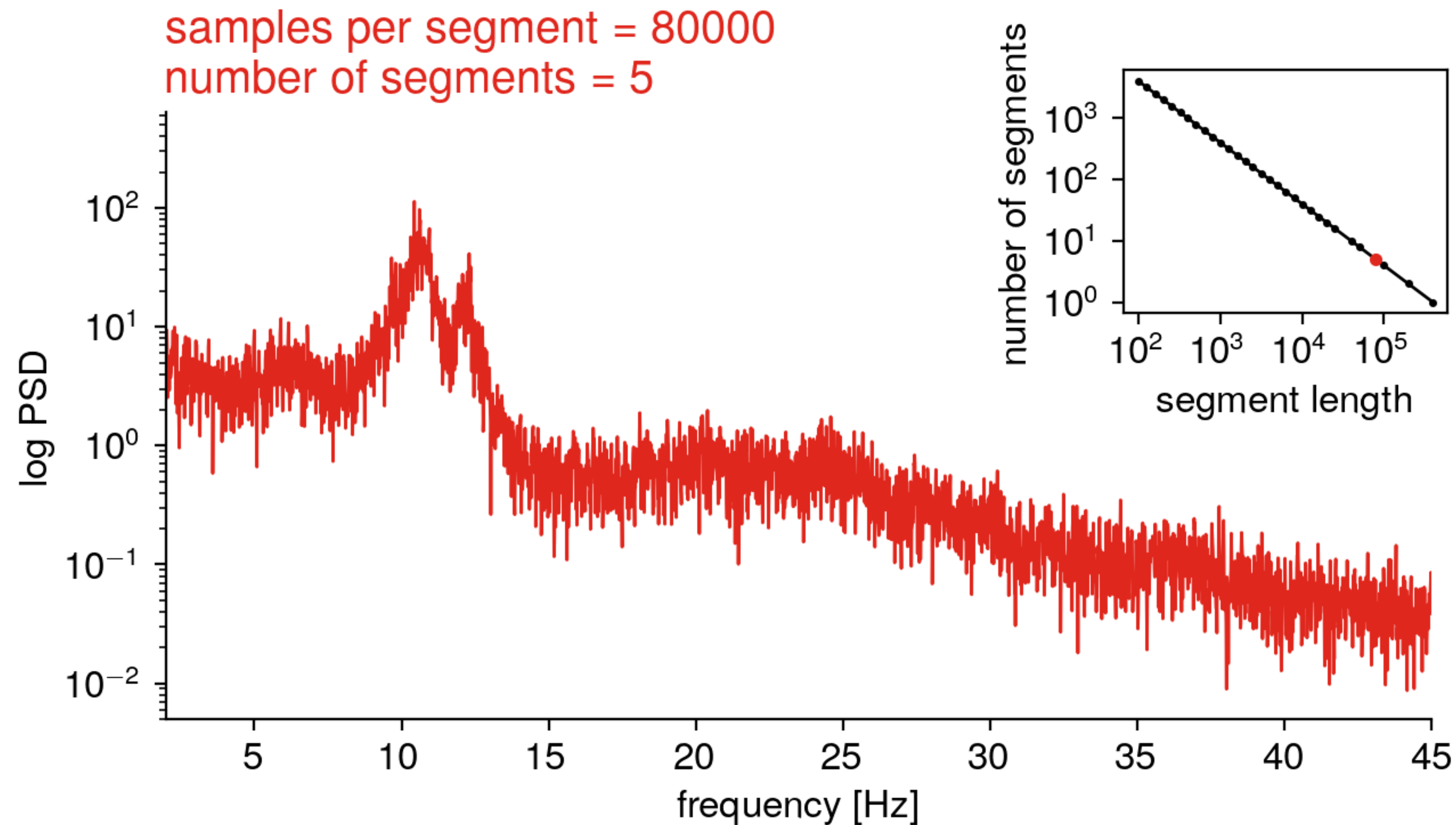
methods: frequency resolution

- changing the settings how many samples per segment are used determines frequency resolution.



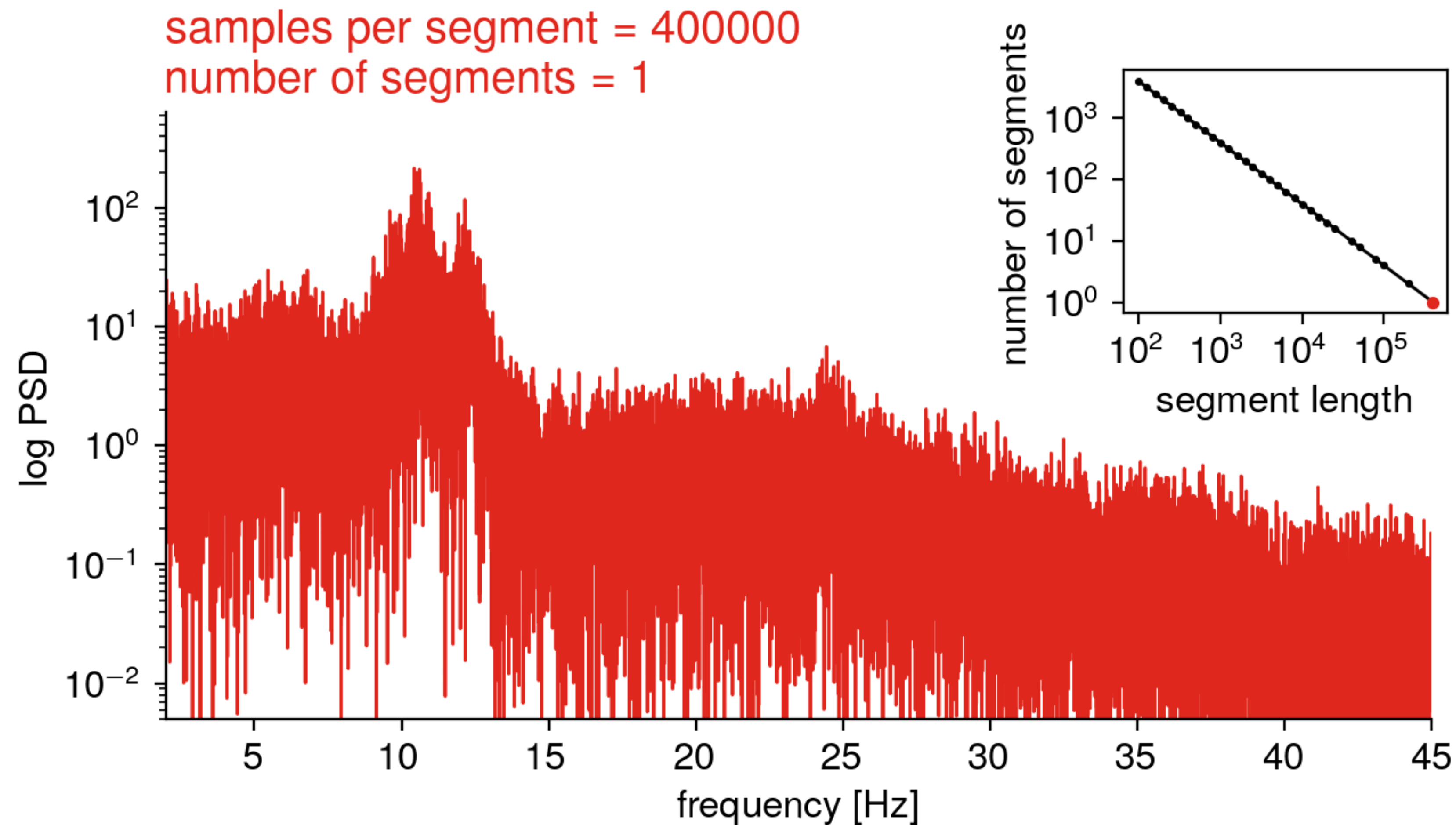
methods: frequency resolution

- changing the settings how many samples per segment are used determines frequency resolution.



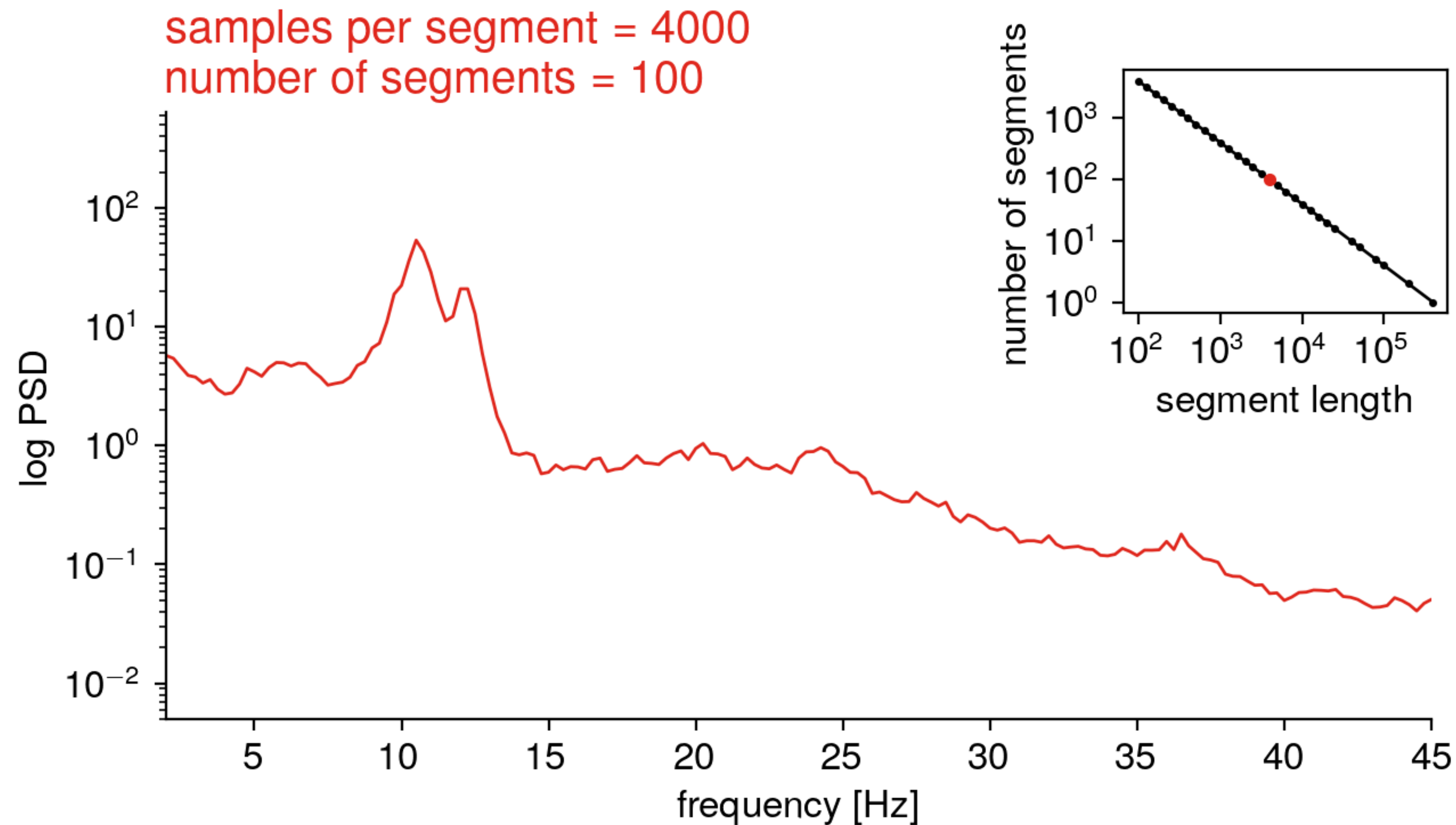
methods: frequency resolution

- changing the settings how many samples per segment are used determines frequency resolution.

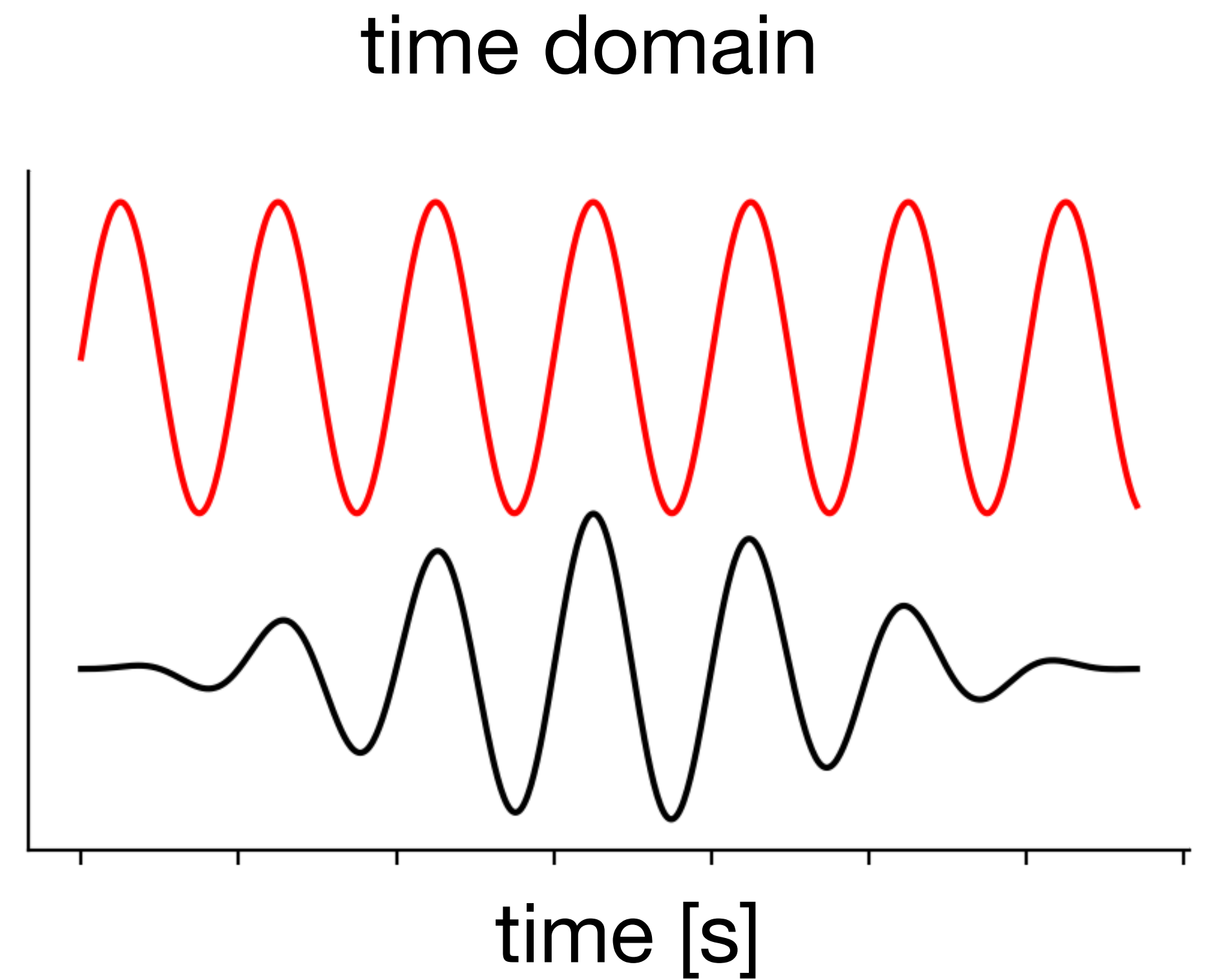
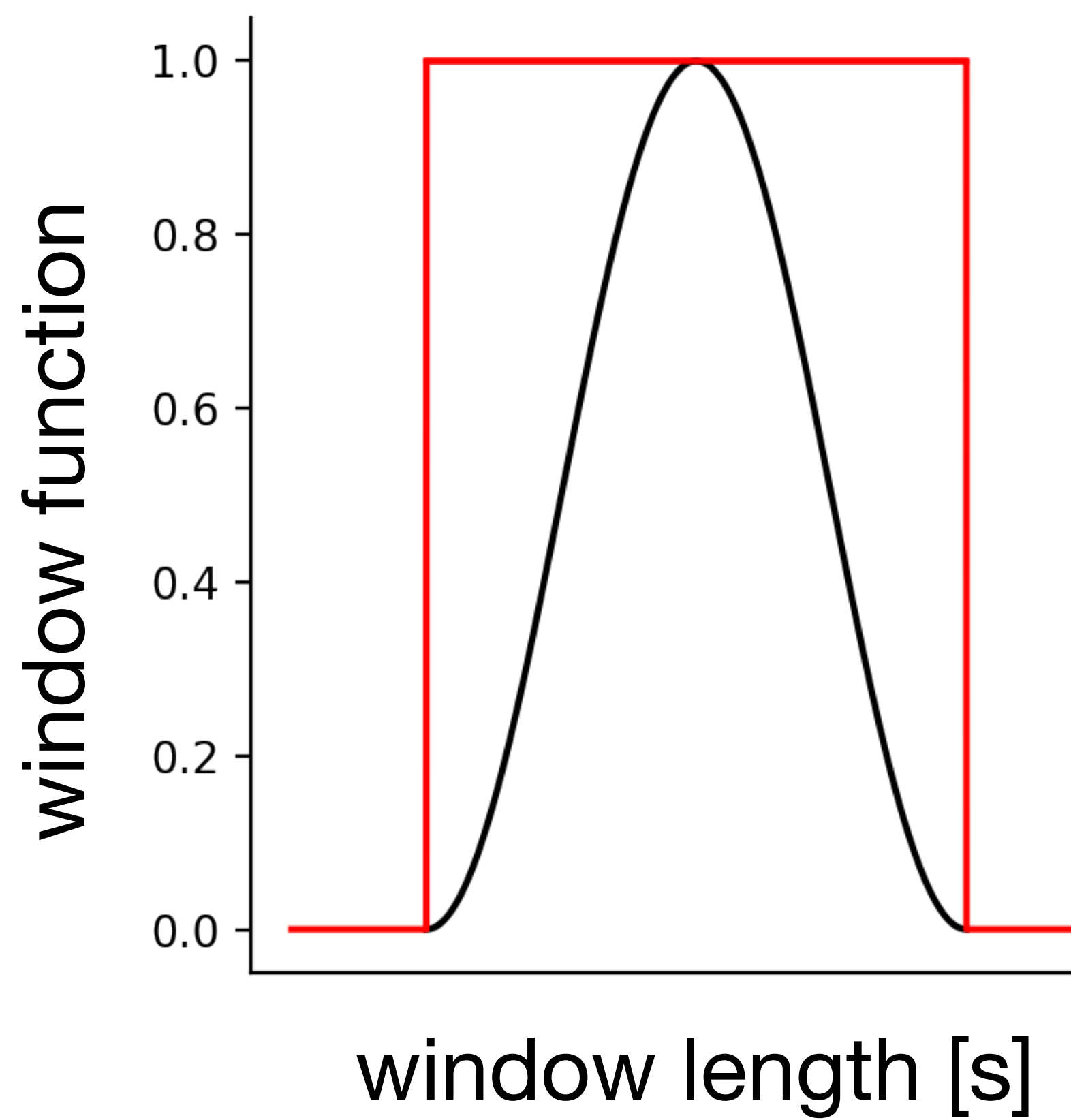


methods: frequency resolution

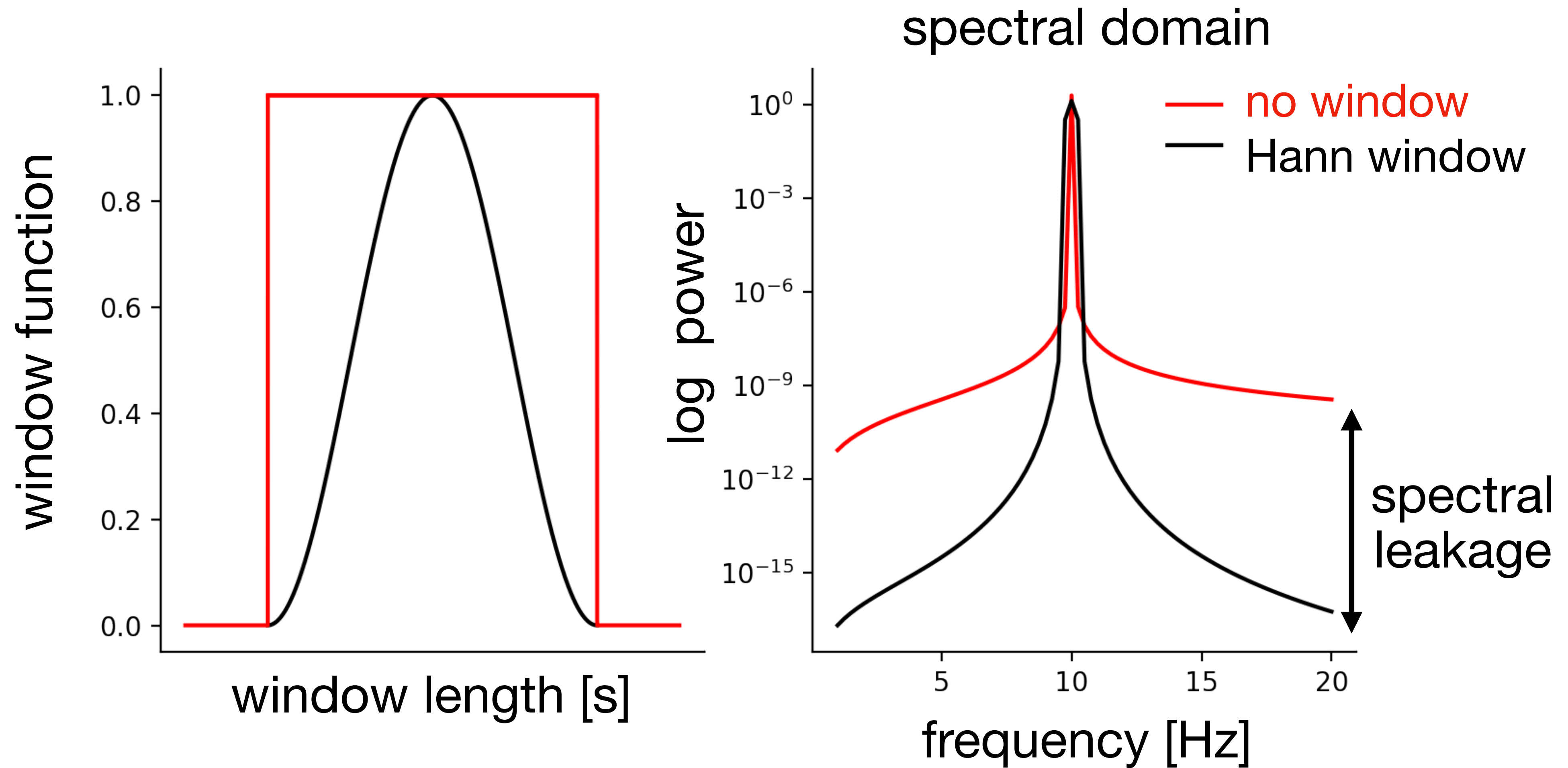
- changing the settings how many samples per segment are used determines frequency resolution.



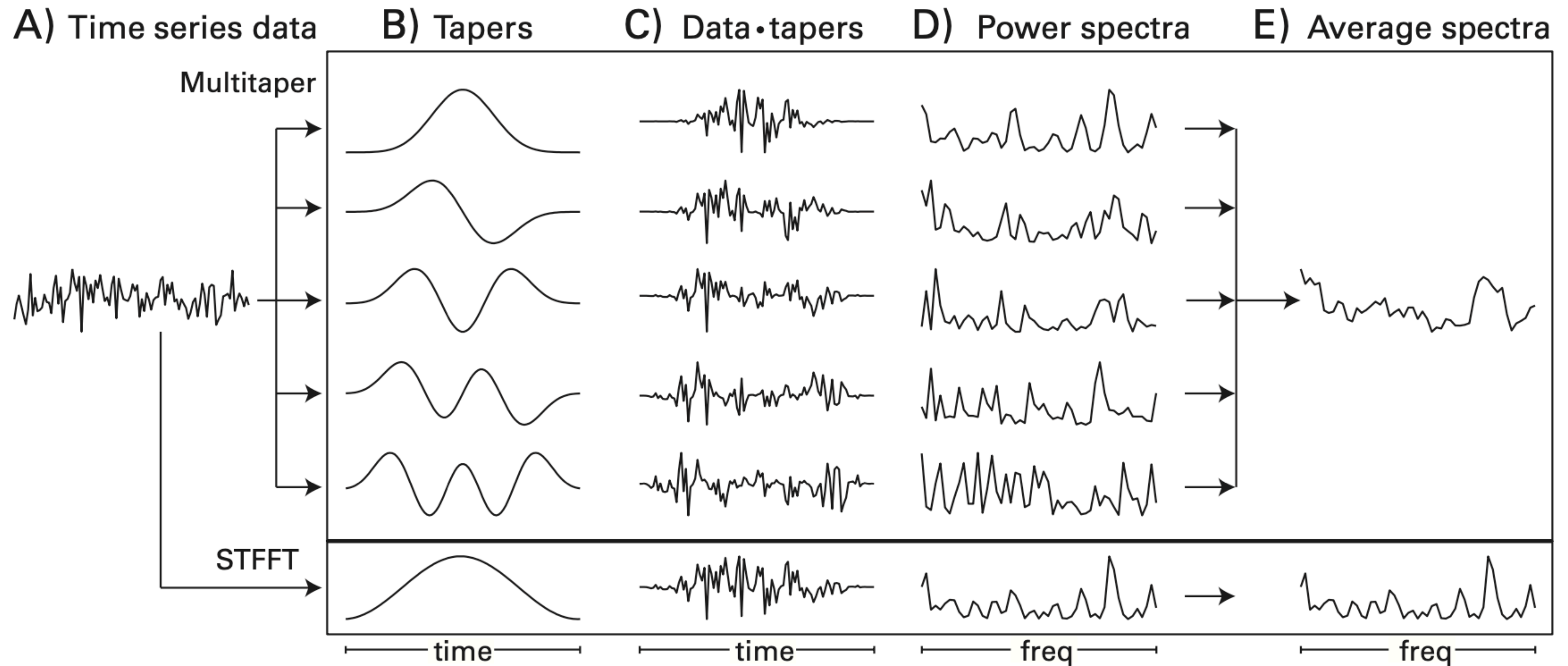
methods: taper / window function



methods: taper / window function

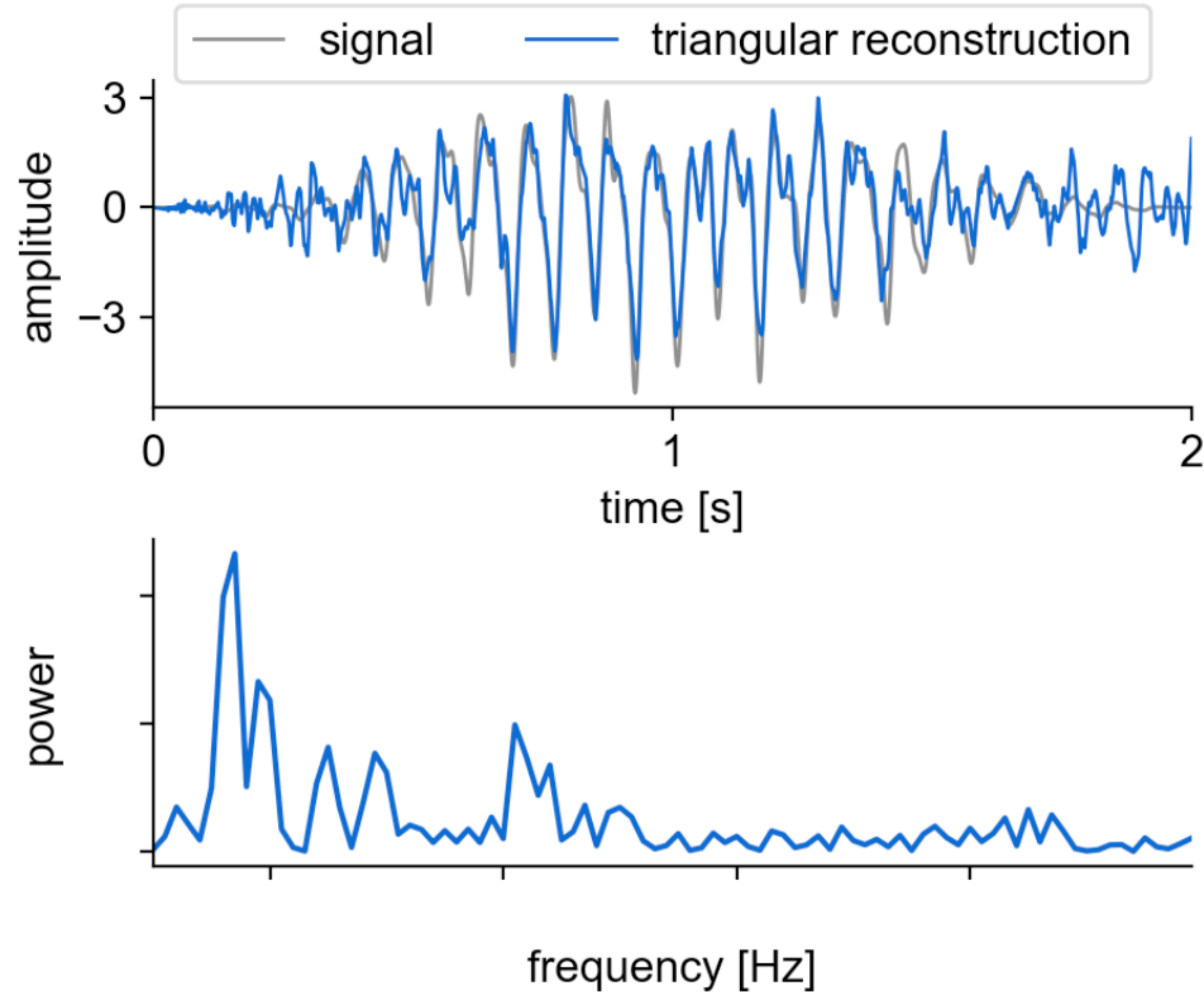
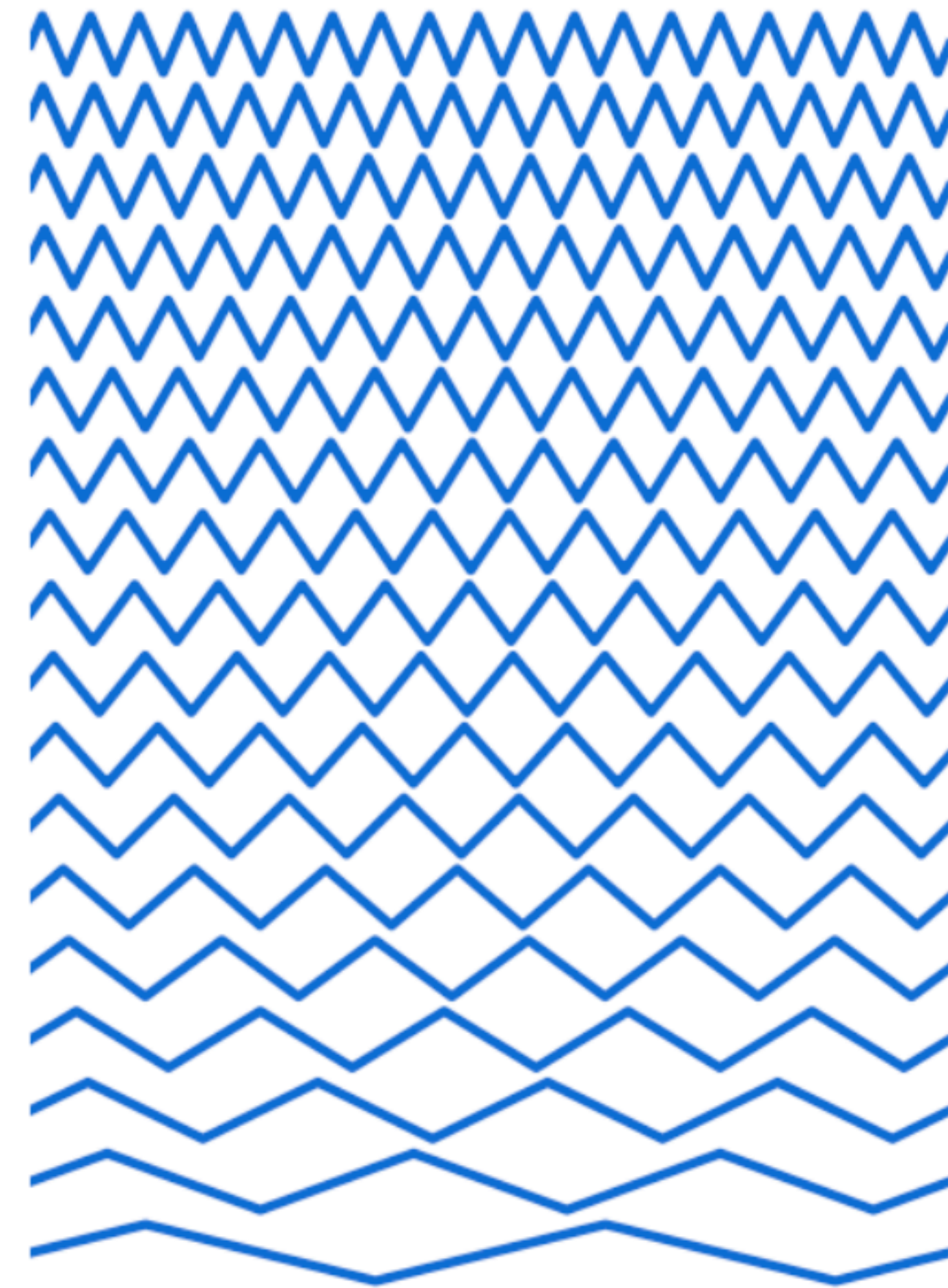


methods: multitaper, goal: increase SNR



other functions as factors?

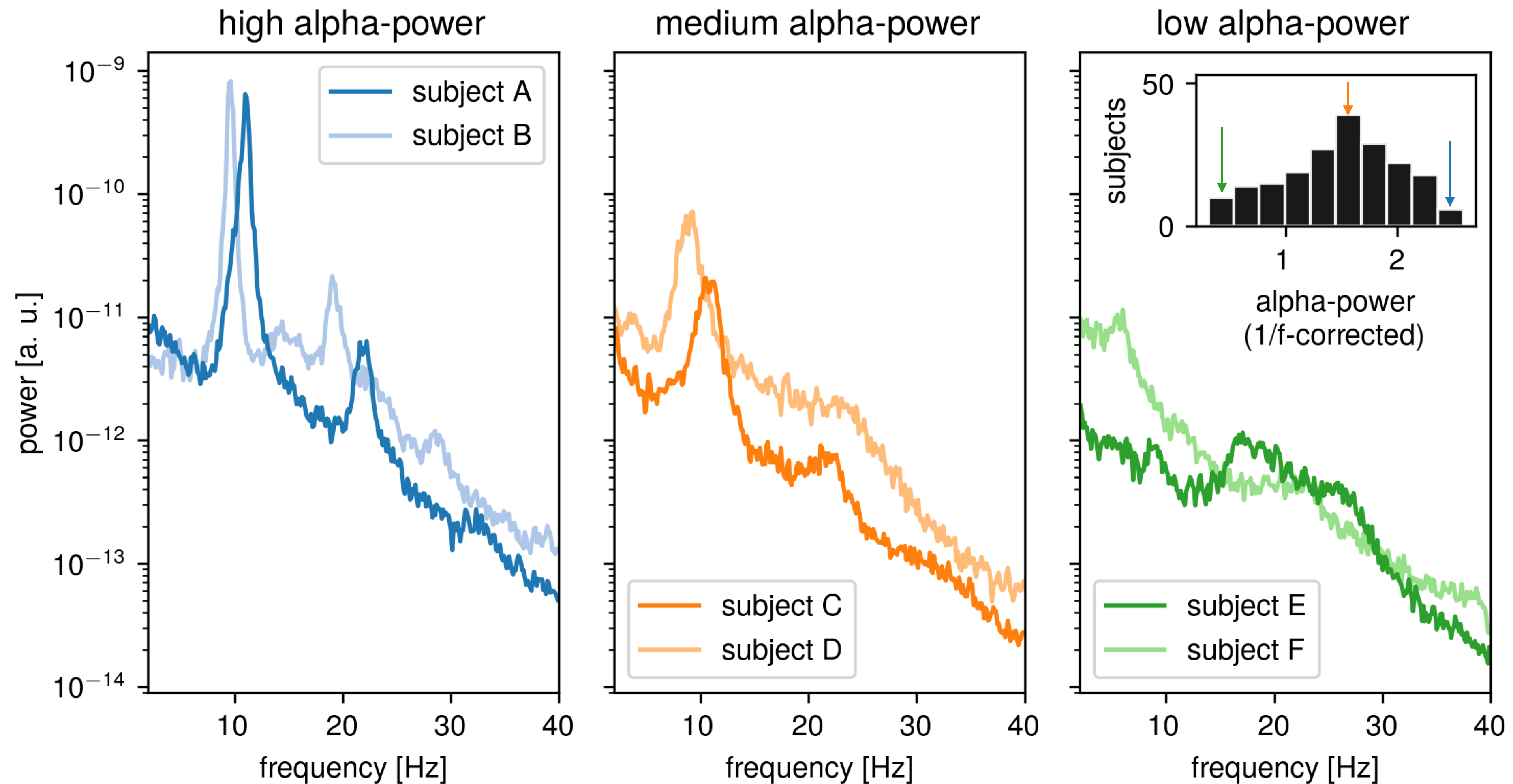
triangular
basis functions



spectral
analysis does
not explain
neuro-
physiological
generative
mechanisms

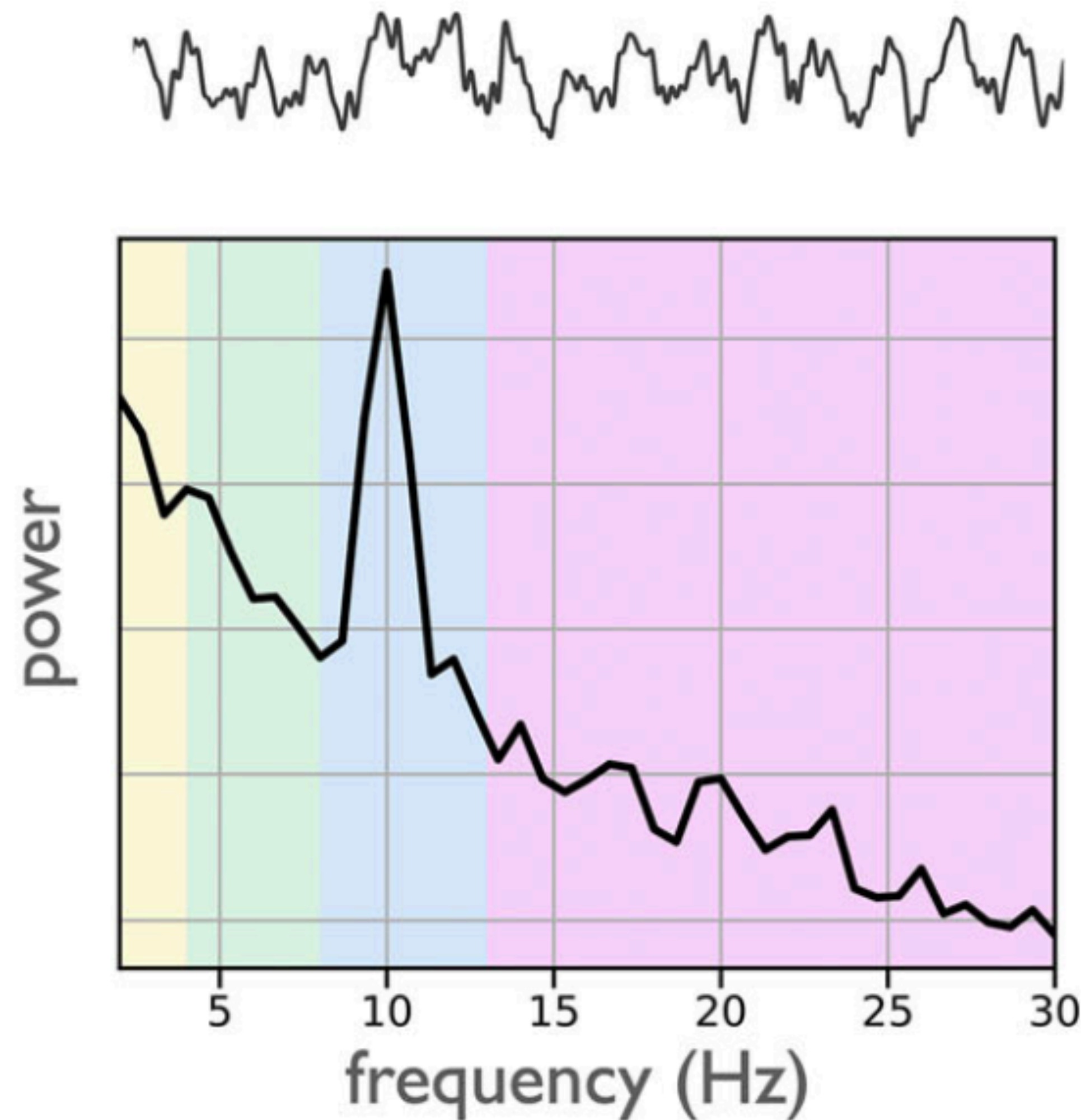
spectral analysis interpretation

variability & oscillation power, example: EEG



Oscillations are variable across participants.

measure: oscillation frequency & power



Frequency (Hz)	IFCN-2017 Glossary
Delta	0.1–<4
Theta	4–<8
Alpha	8–13
Beta	14–30

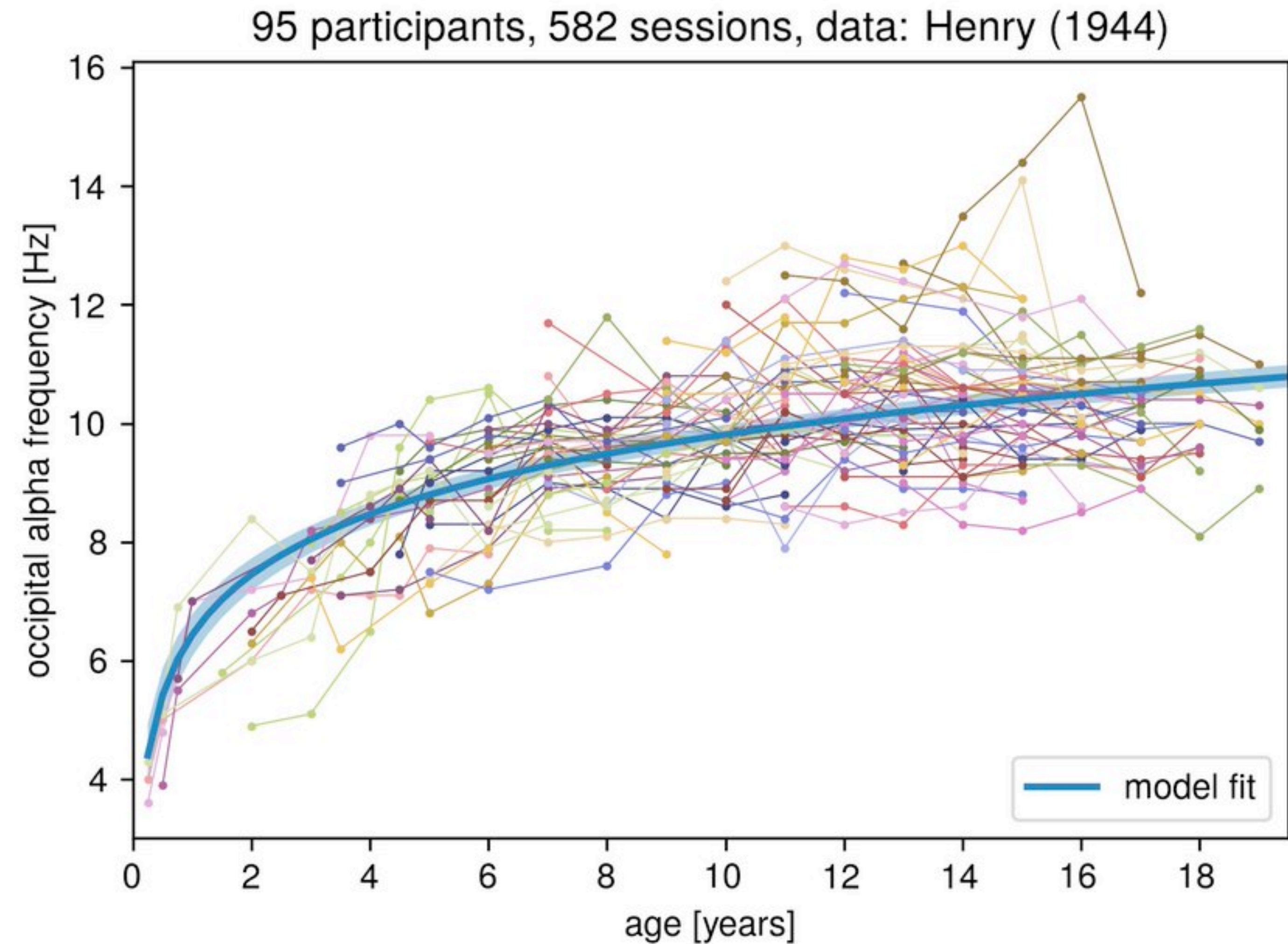
measure:
“alpha-frequency”



phenomenon:
“alpha-rhythm”

pitfalls: frequency changes across frequency boundaries

- observation:
oscillation frequency
changes drastically
over the course of
development
- here posterior
dominant rhythm,
human EEG



pitfalls: frequency changes across frequency boundaries

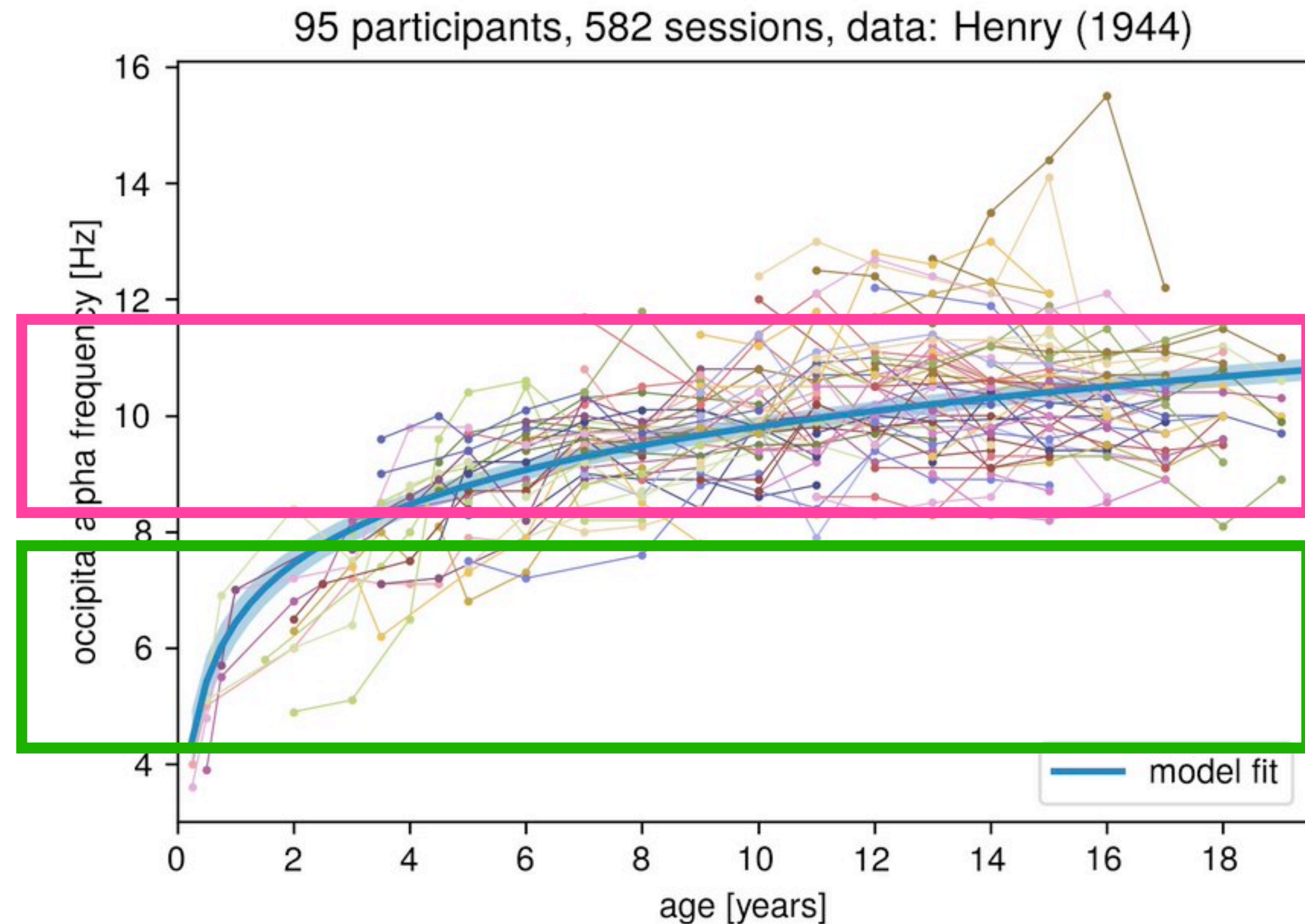
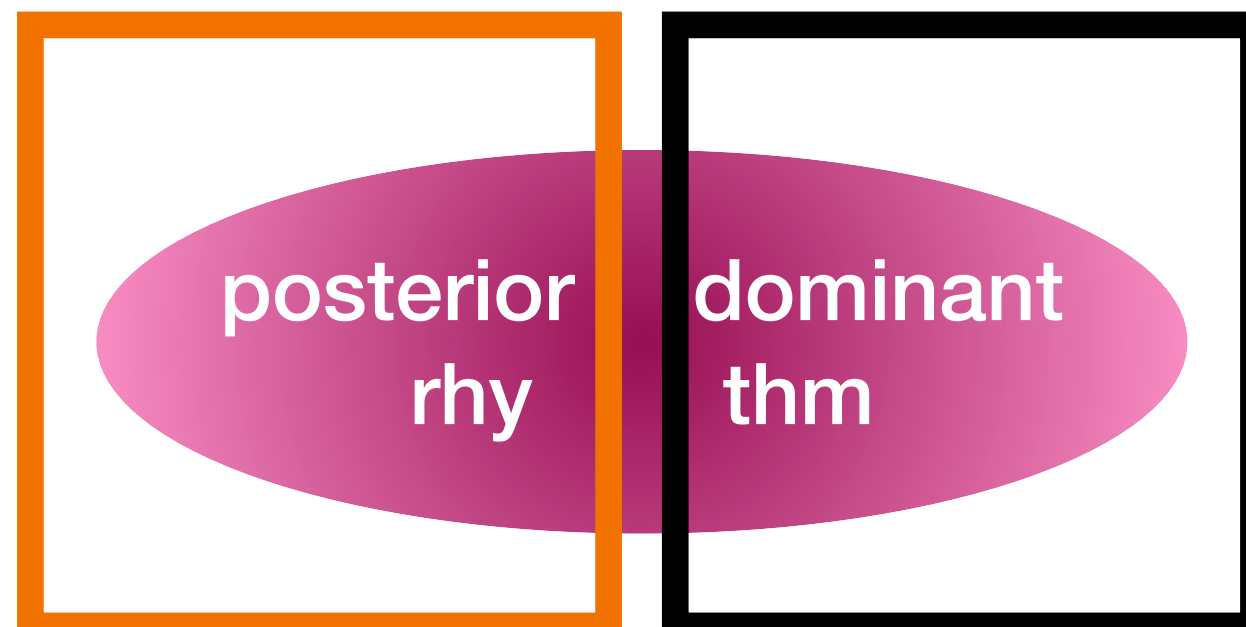
- observation:
oscillation frequency
changes drastically
over the course of
development
- here posterior
dominant rhythm,
human EEG

alpha-rhythm?

theta-rhythm?

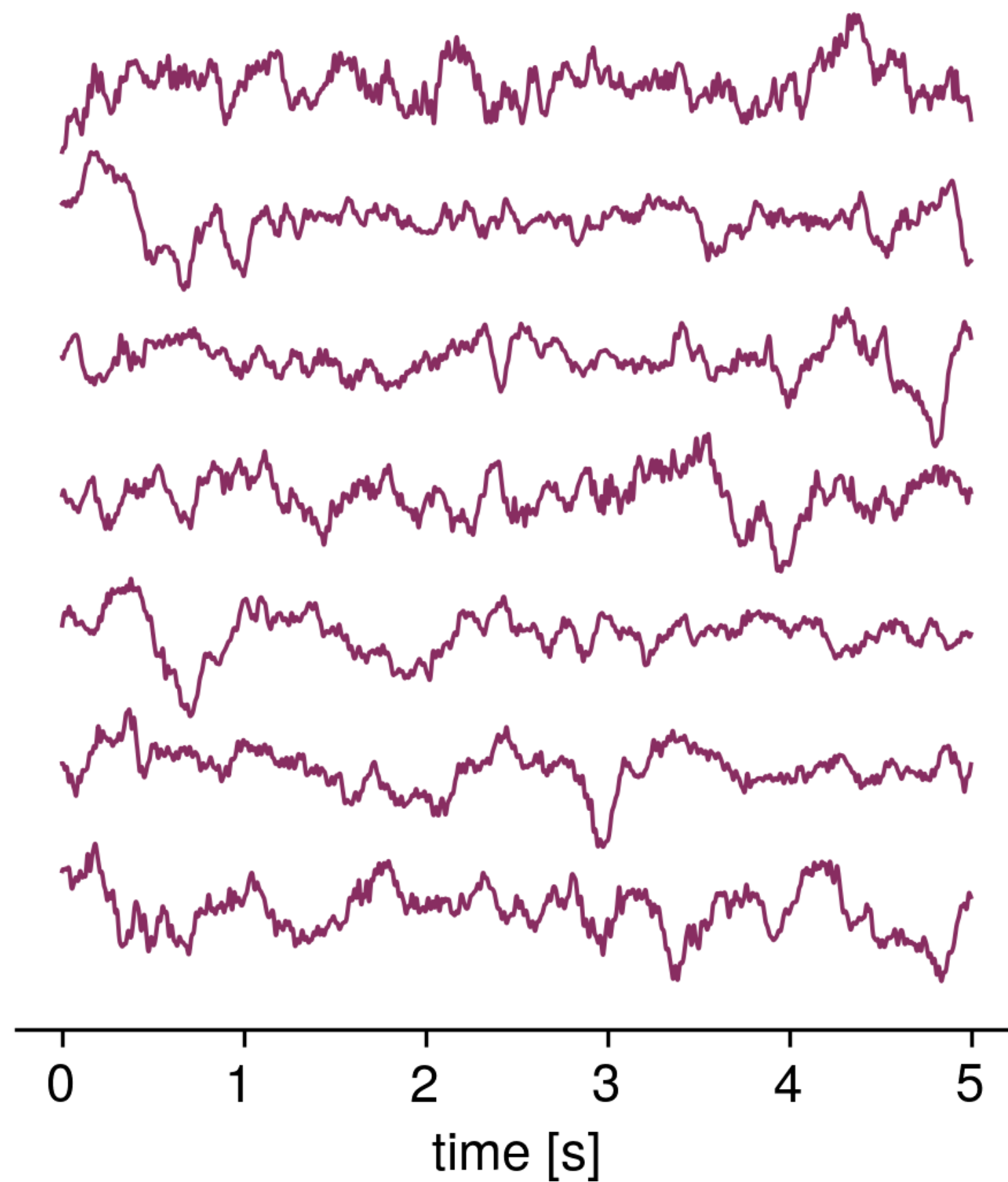
measure: “theta-
frequency”

measure: “alpha-
frequency”

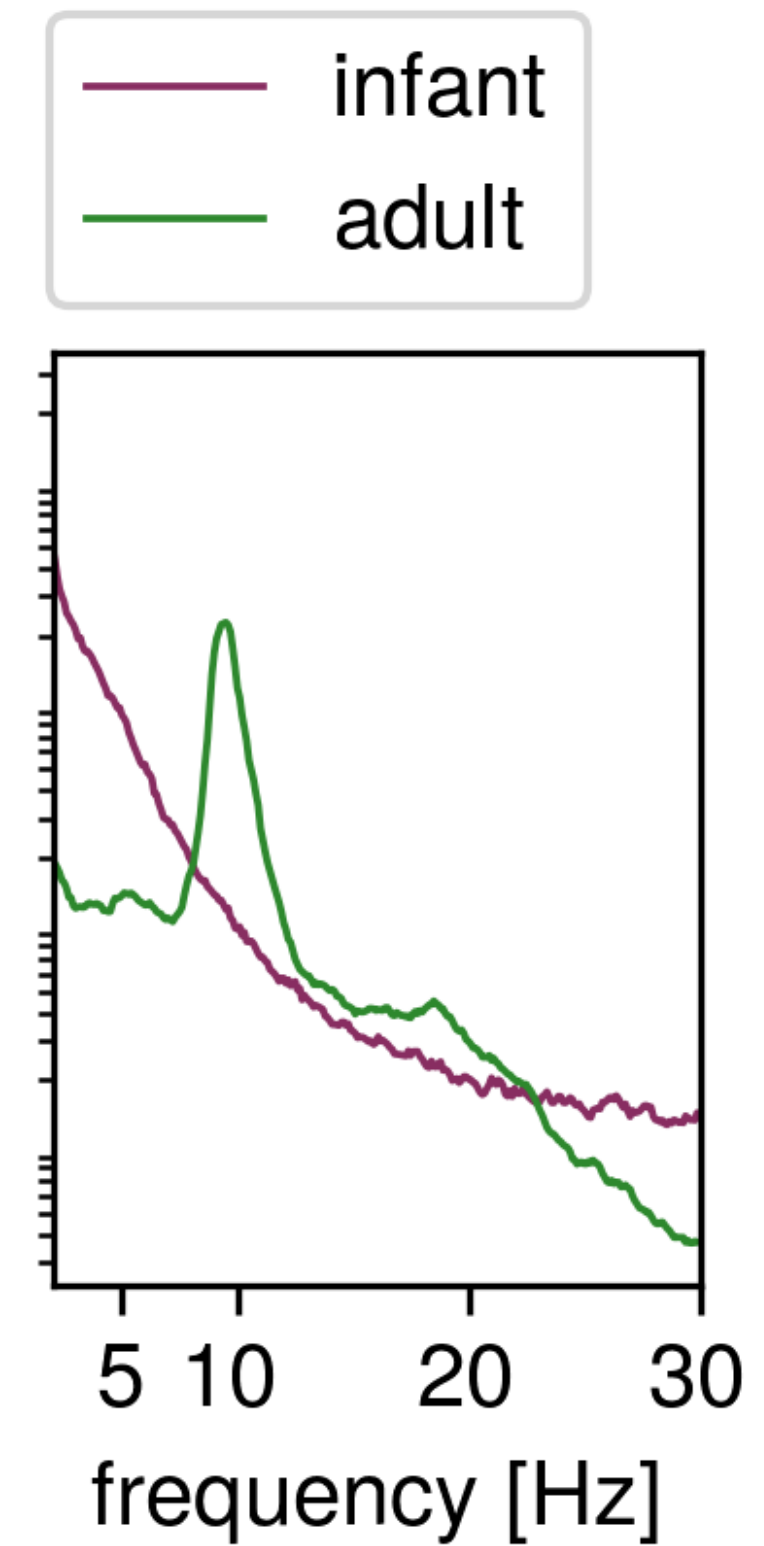
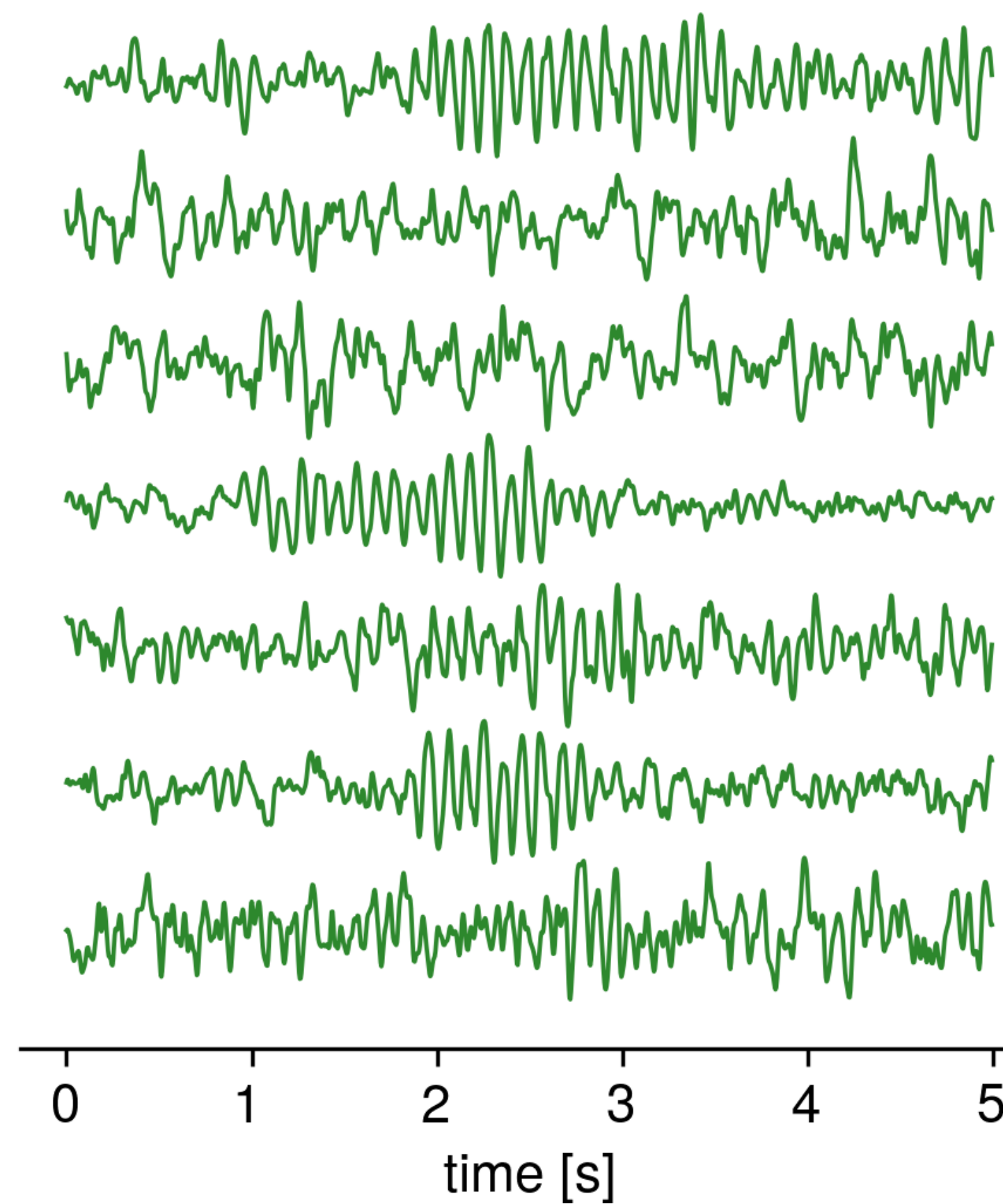


non-rhythmic contributions, 1/f-activity

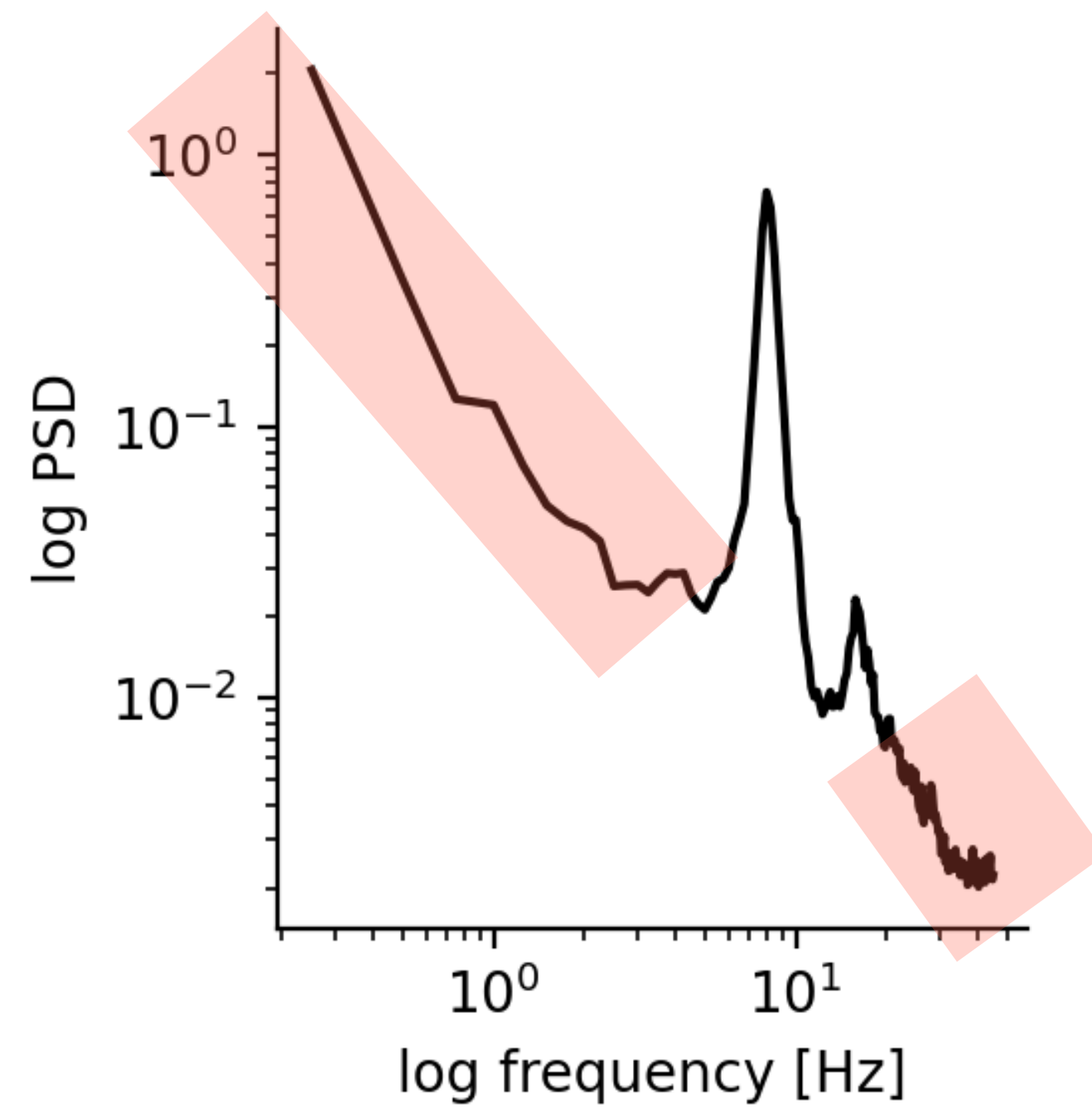
infant EEG activity (age = 2 months)
channel PO3



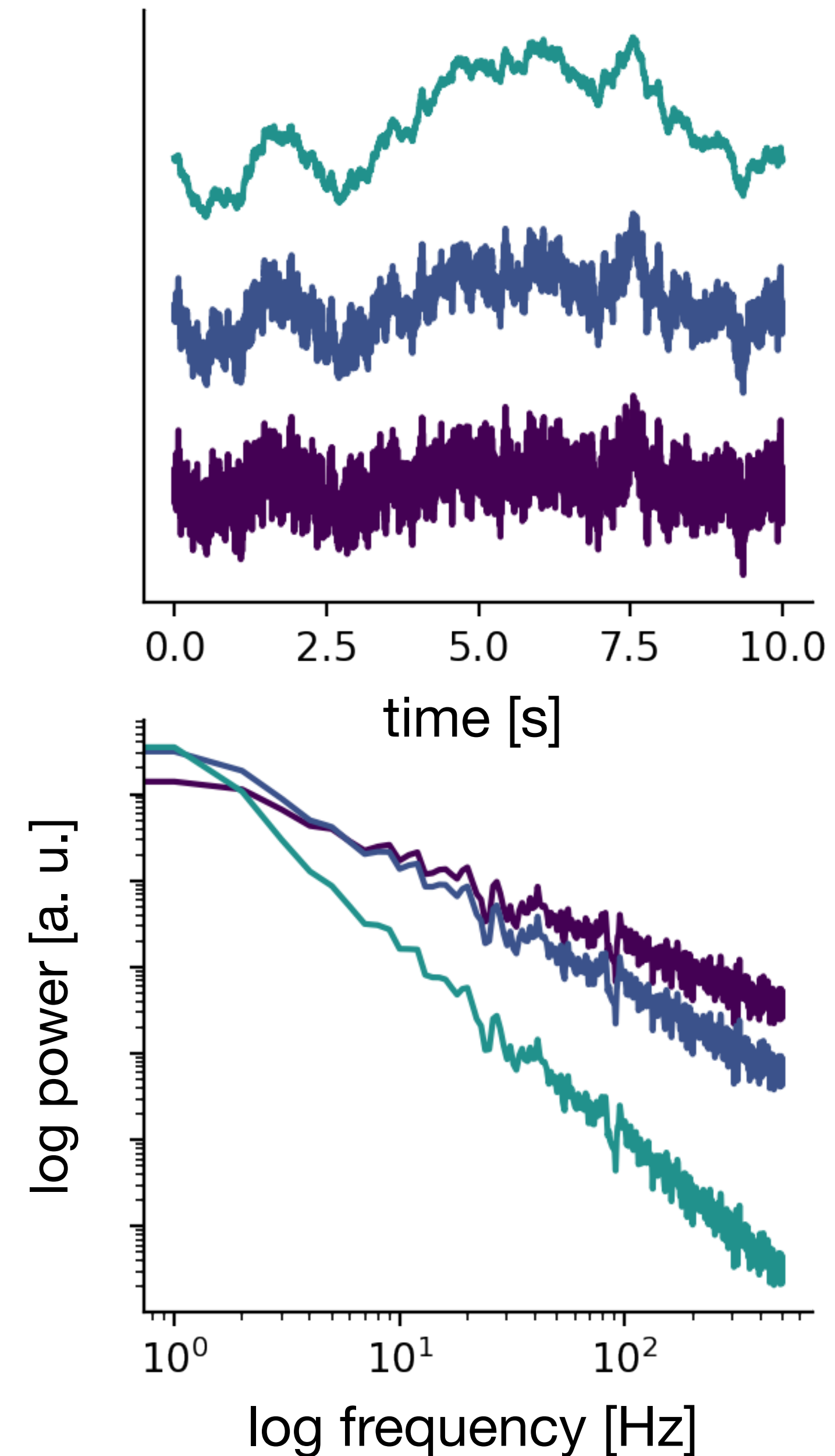
adult EEG activity
channel PO3



non-rhythmic contributions, 1/f-activity



- 1/f-activity:
power scales with frequency
scale free dynamics



pitfalls: not only rhythmic changes + rhythms can be absent



“delta-power”



“theta-power”

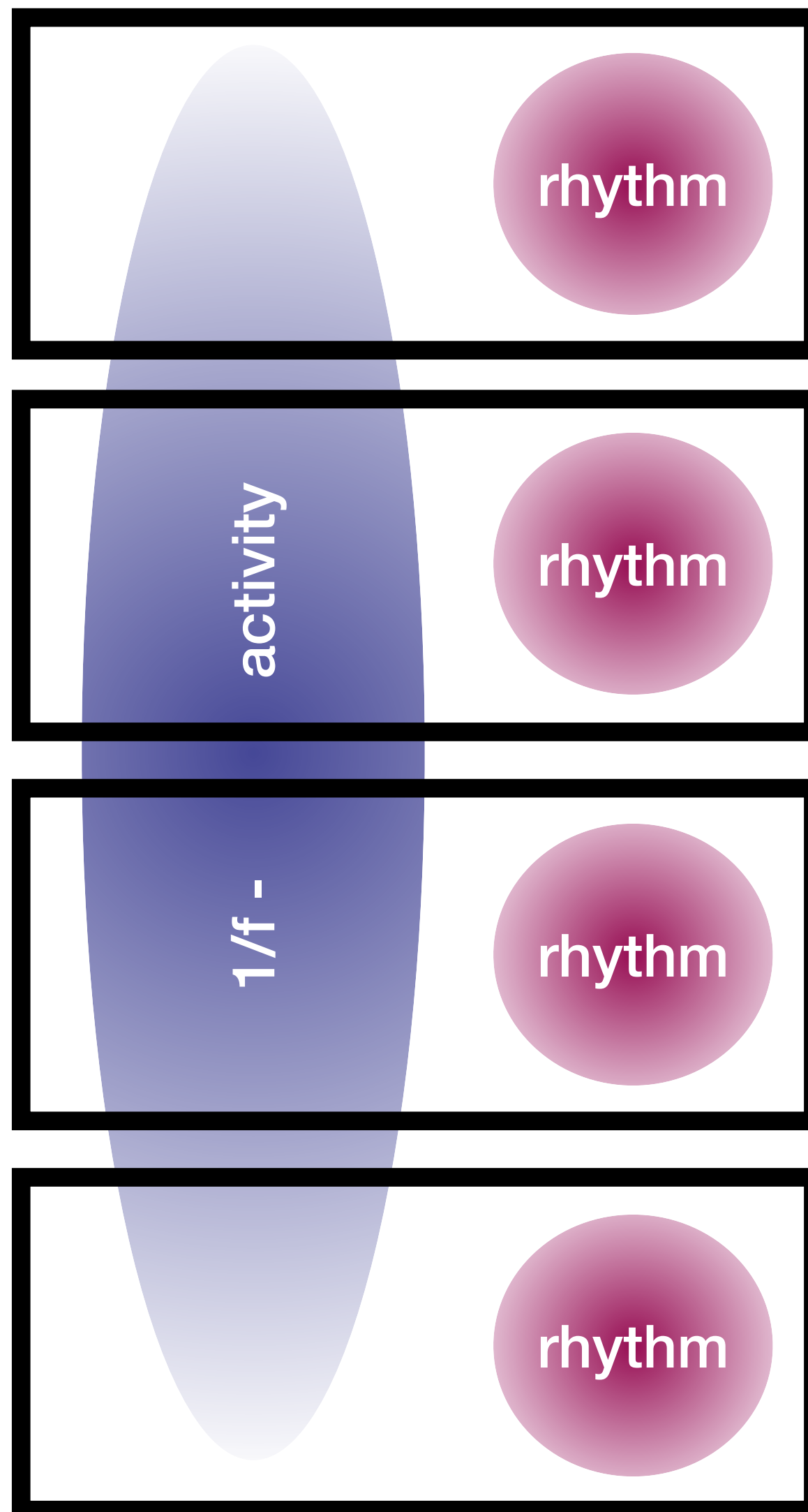


“alpha-power”



“beta-power”

pitfalls: not only rhythmic changes + rhythms can be absent



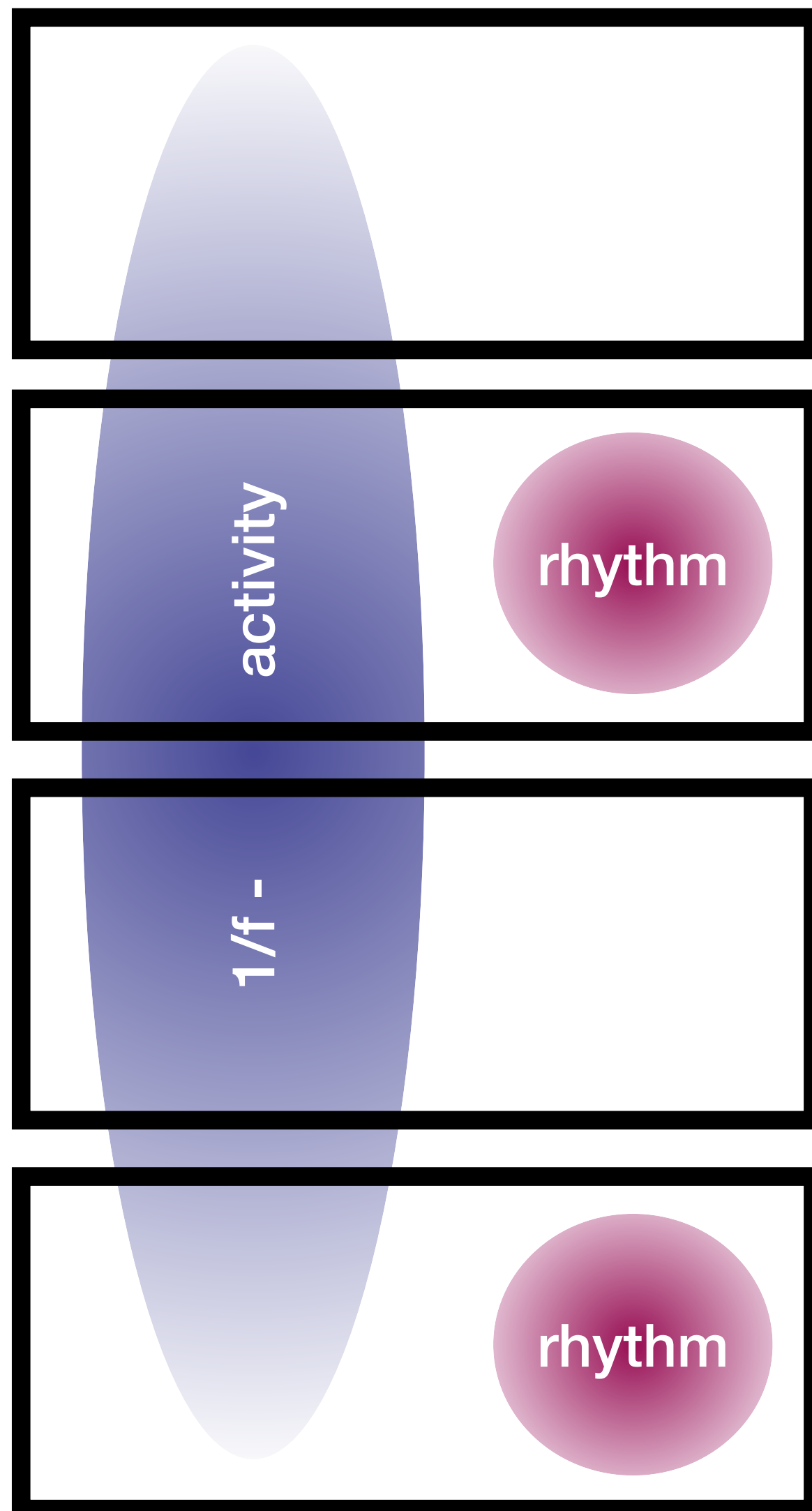
“delta-power”

“theta-power”

“alpha-power”

“beta-power”

pitfalls: not only rhythmic changes + rhythms can be absent



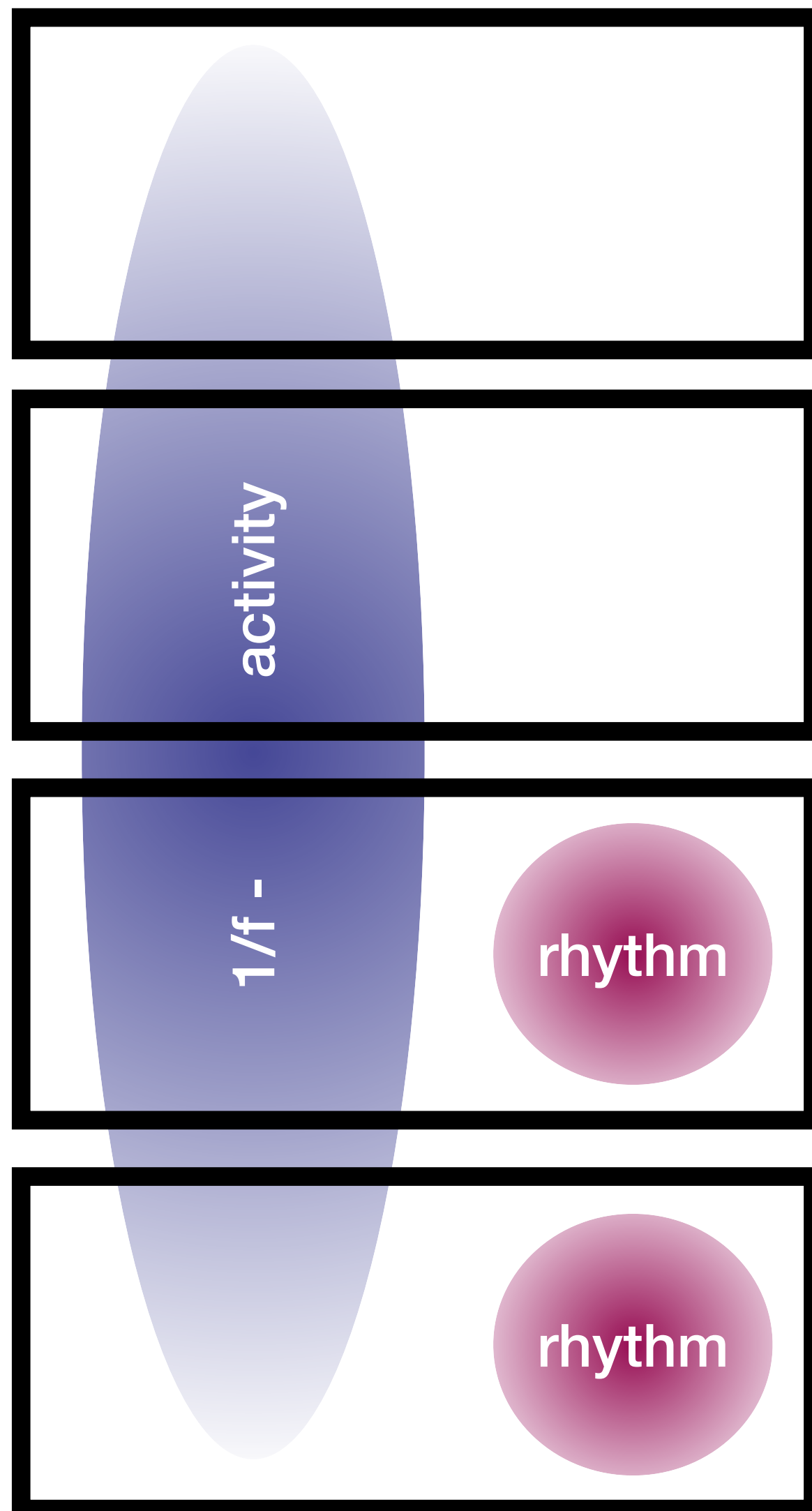
“delta-power”

“theta-power”

“alpha-power”

“beta-power”

pitfalls: not only rhythmic changes + rhythms can be absent



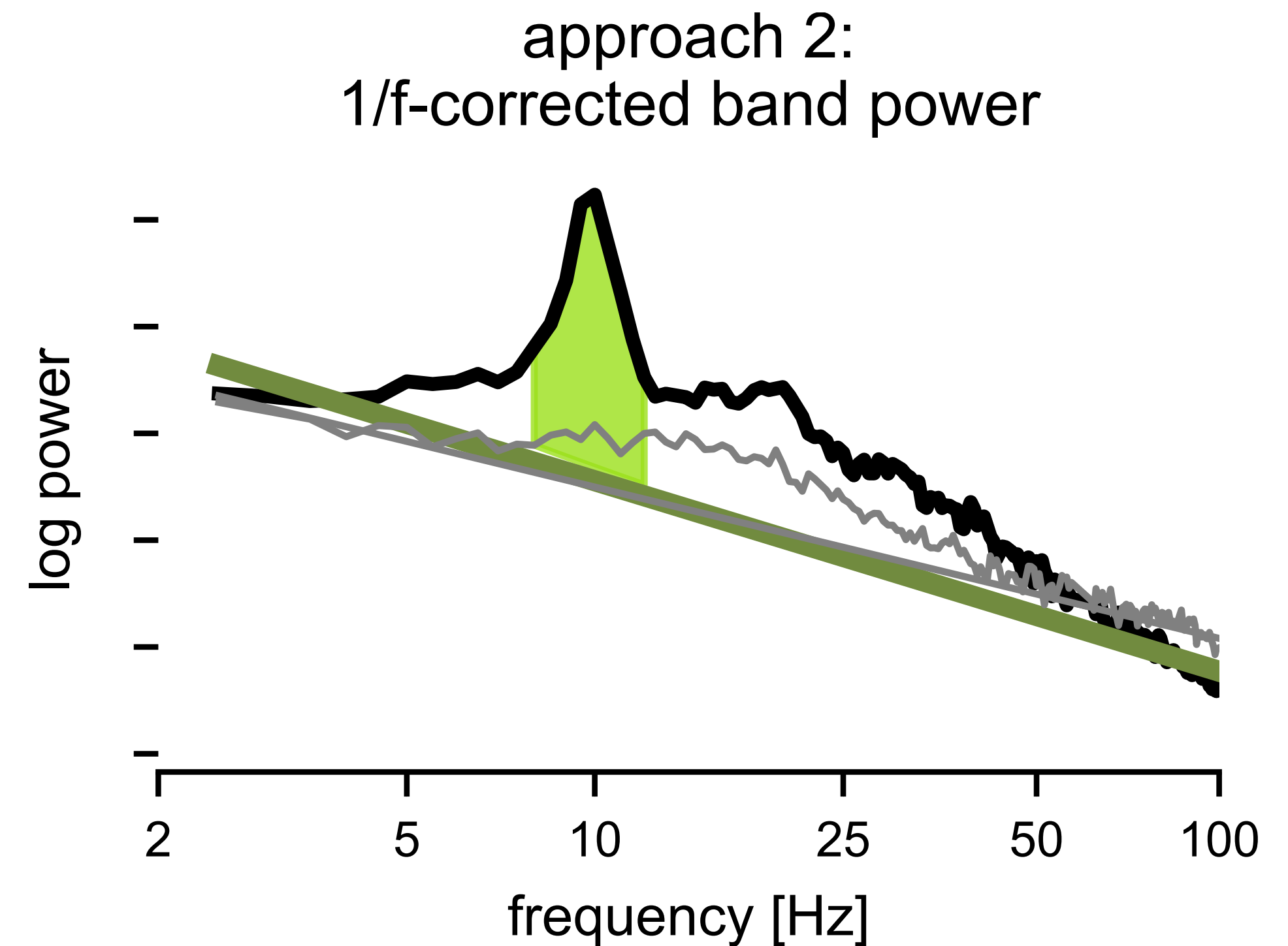
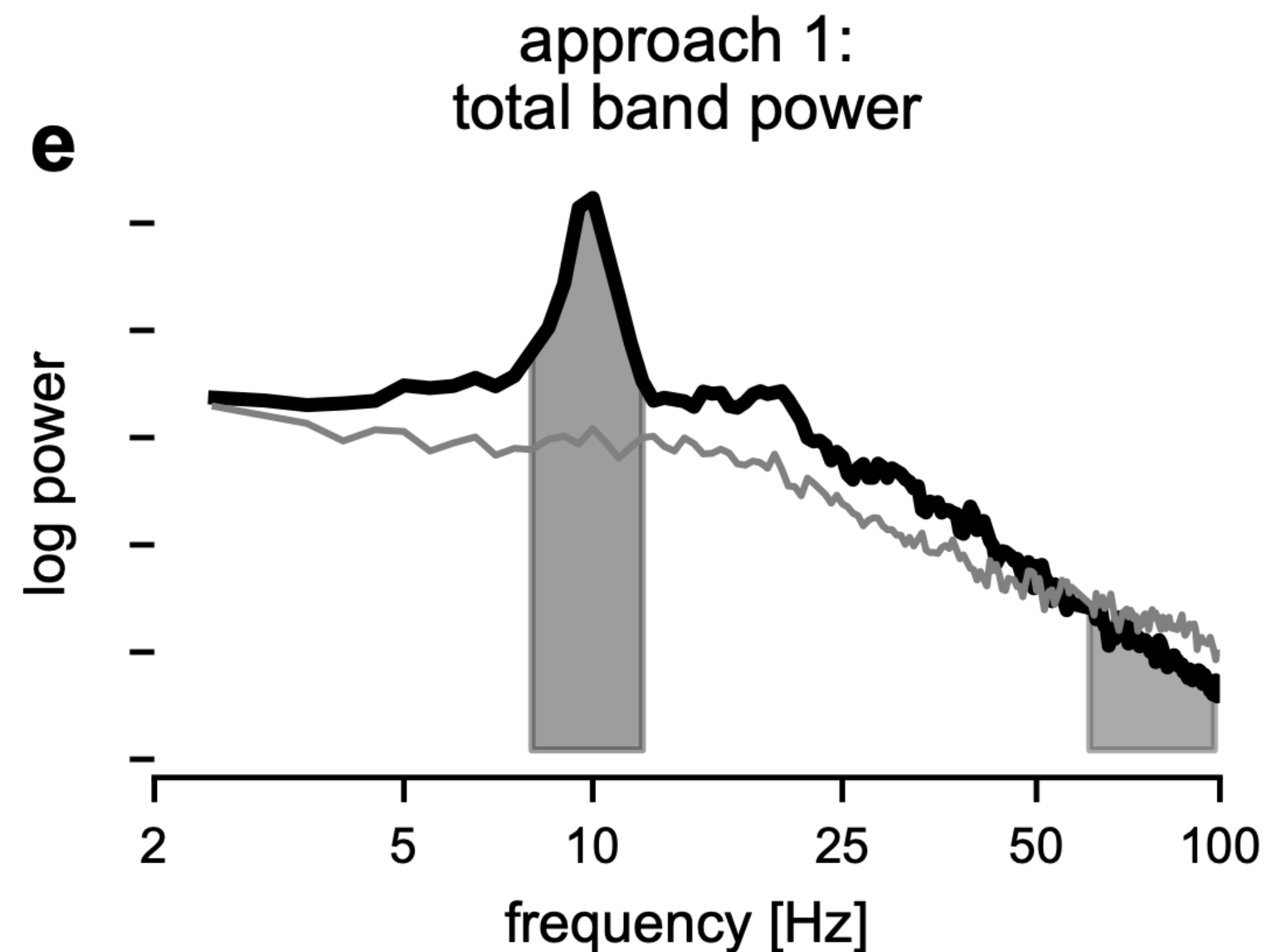
“delta-power”

“theta-power”

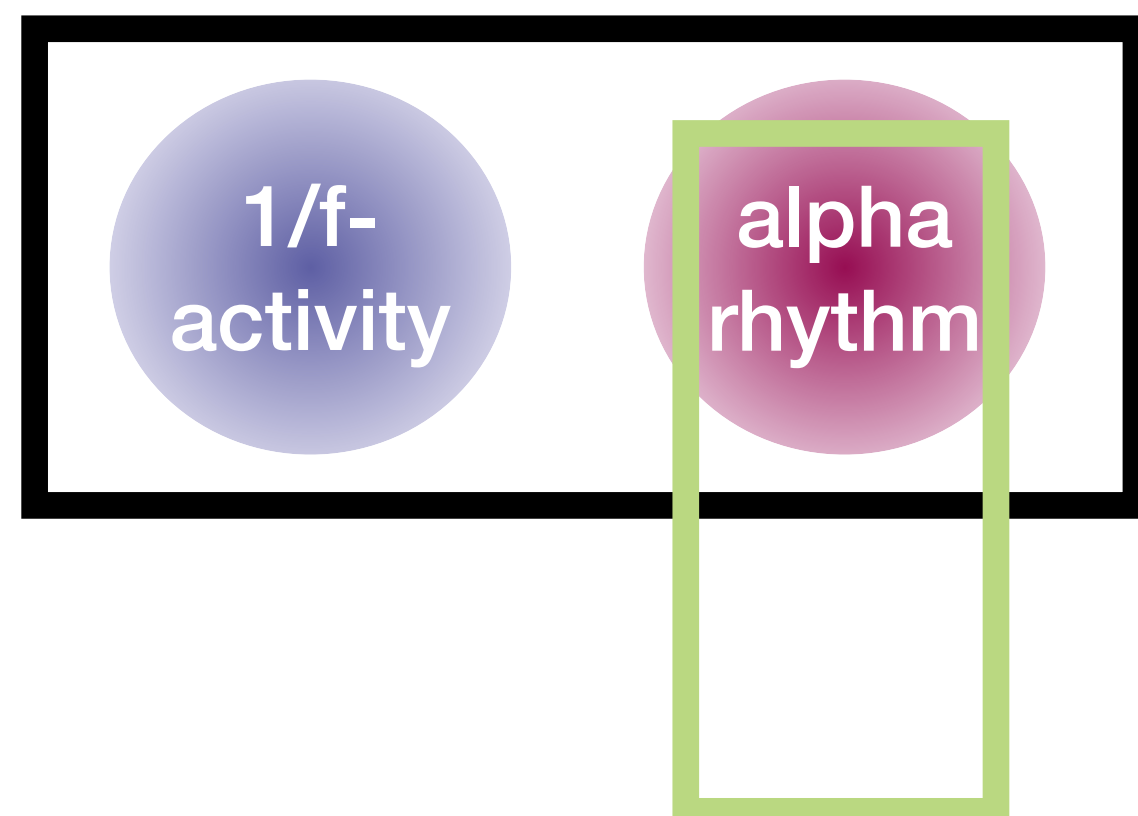
“alpha-power”

“beta-power”

new measures needed?



measure:
“alpha-power”



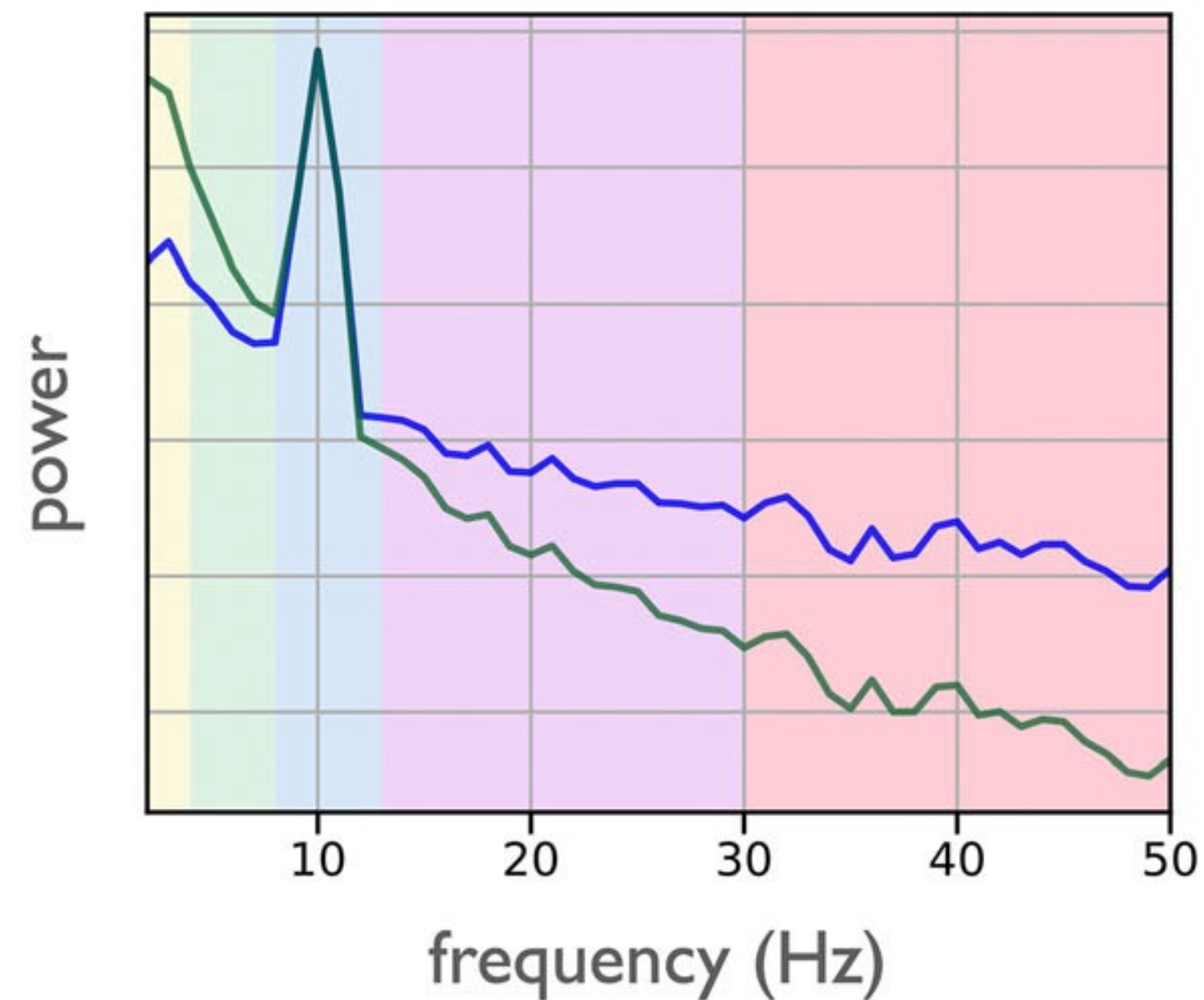
measure:
“1/f-corrected
alpha-power”

1/f-corrected alpha power =
improved way to measure
oscillatory contribution more
specifically?

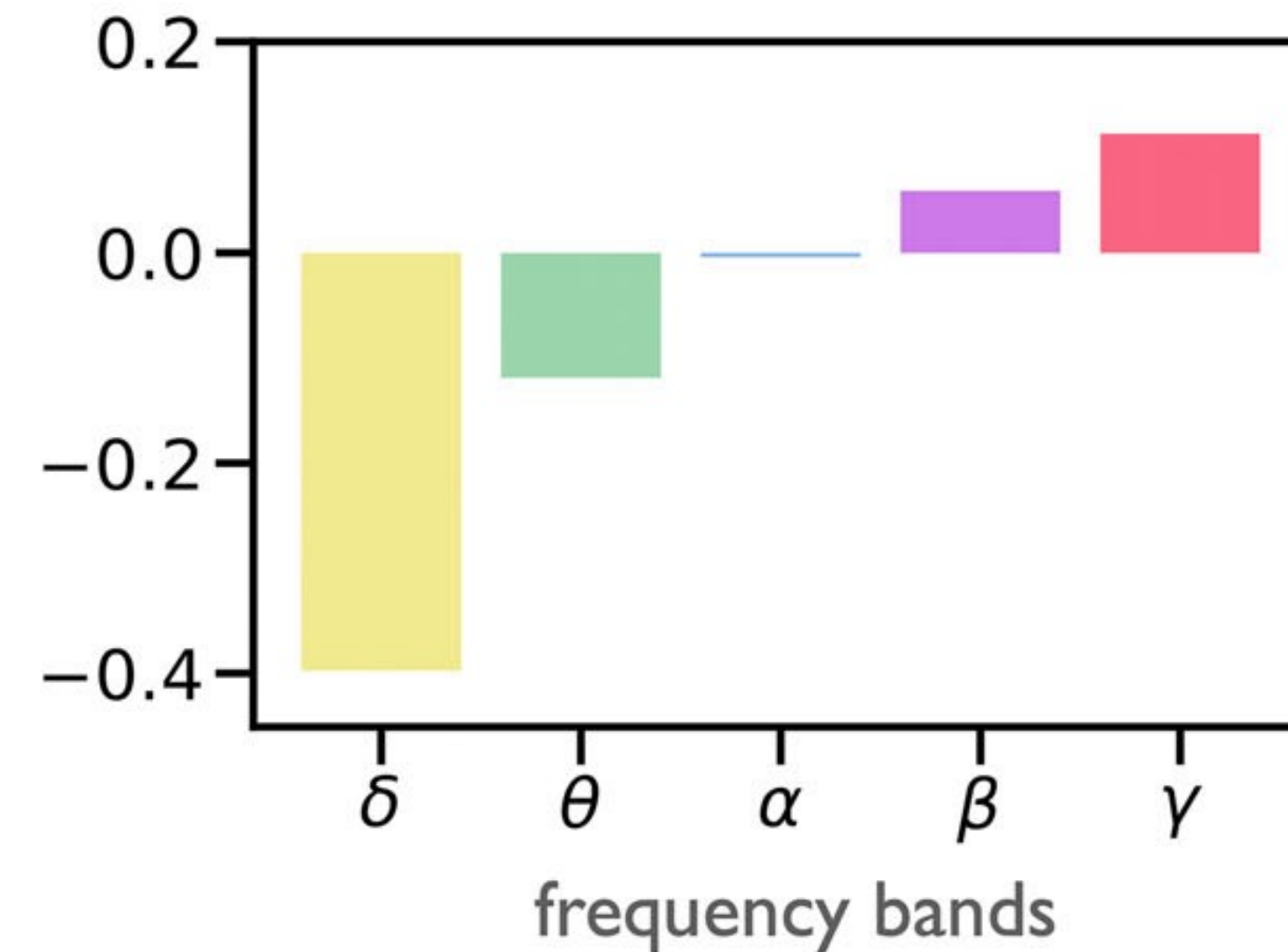
new measures needed?

Two ways to plot the same result:

changes between 2
conditions in terms of 1/f-
exponent



changes between 2
conditions per frequency
band



same summary measures, different signal generation

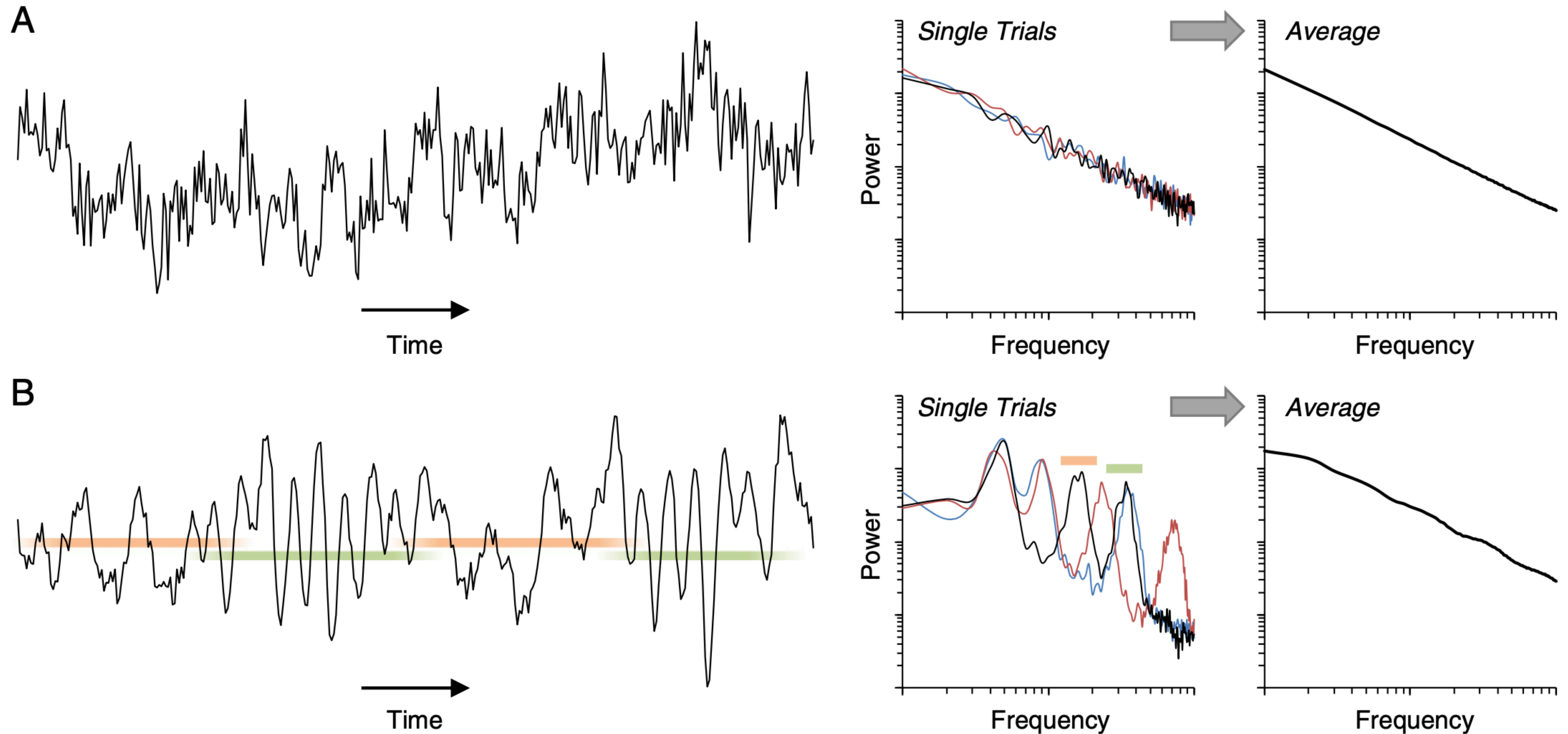
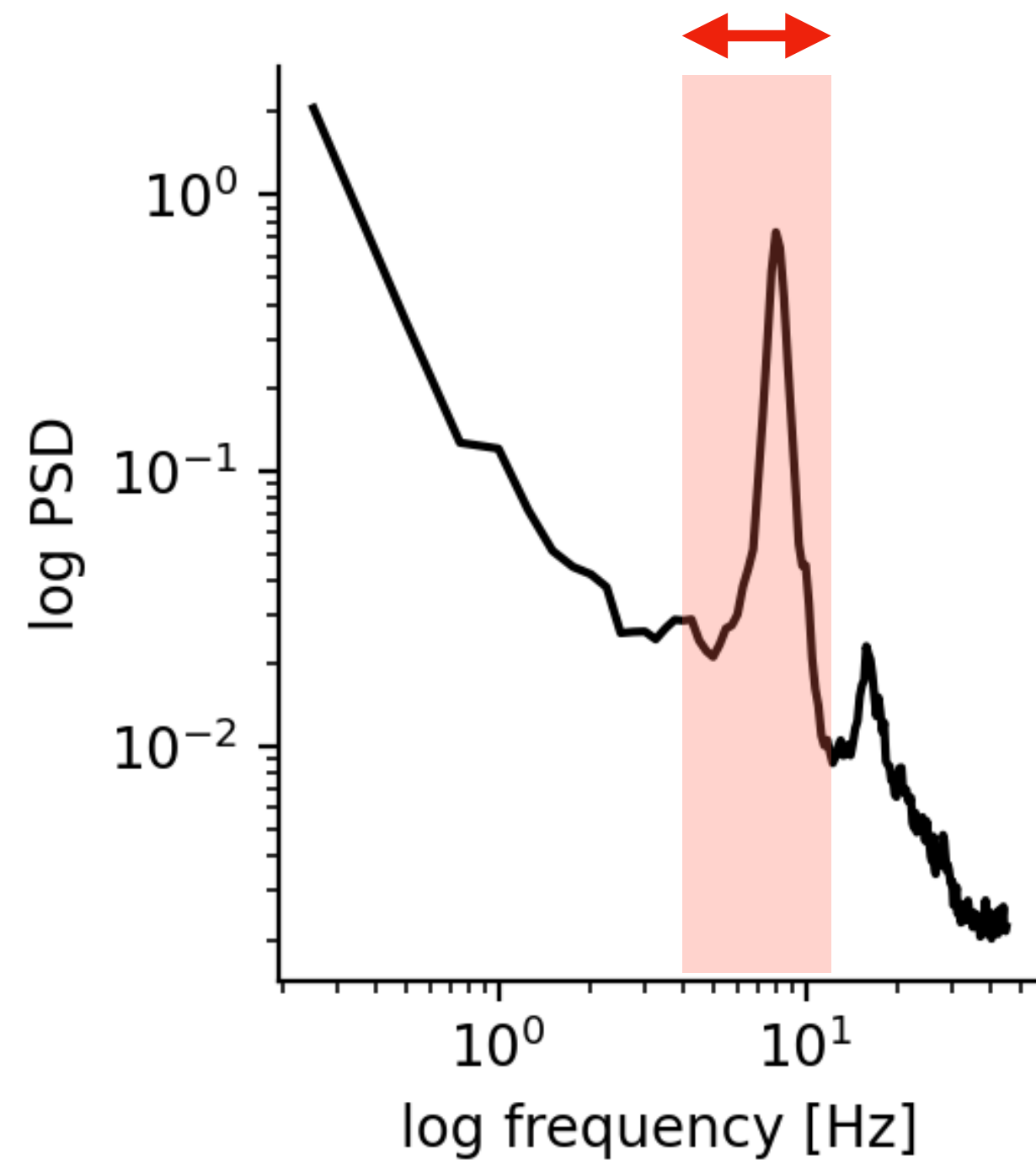
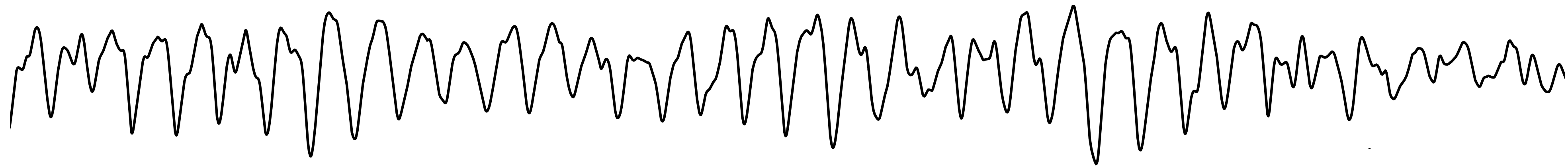


figure from: Palva & Palva
NeuroImage, 2012

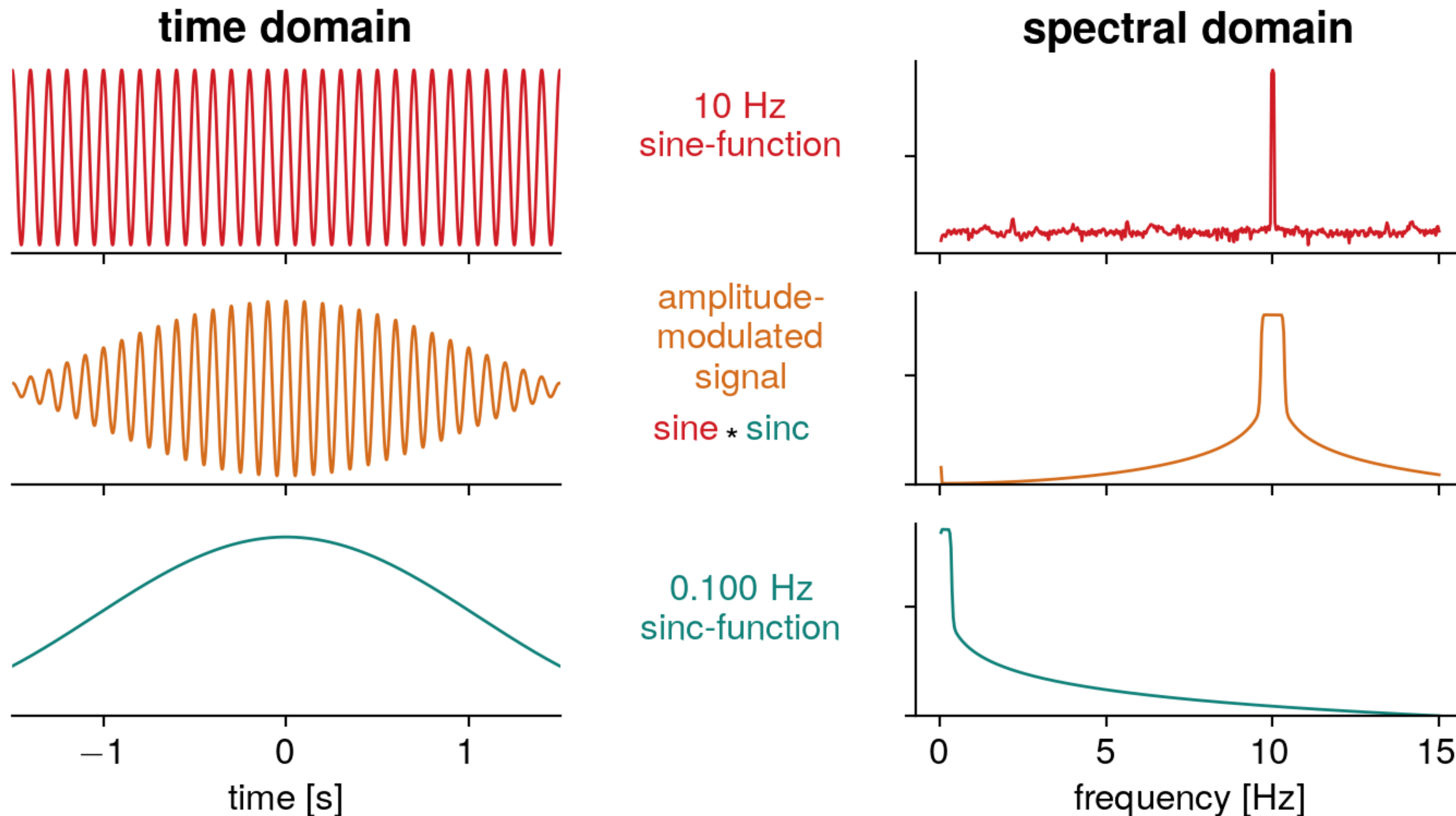
phenomenon: amplitude modulation

- neural rhythms show amplitude modulation.



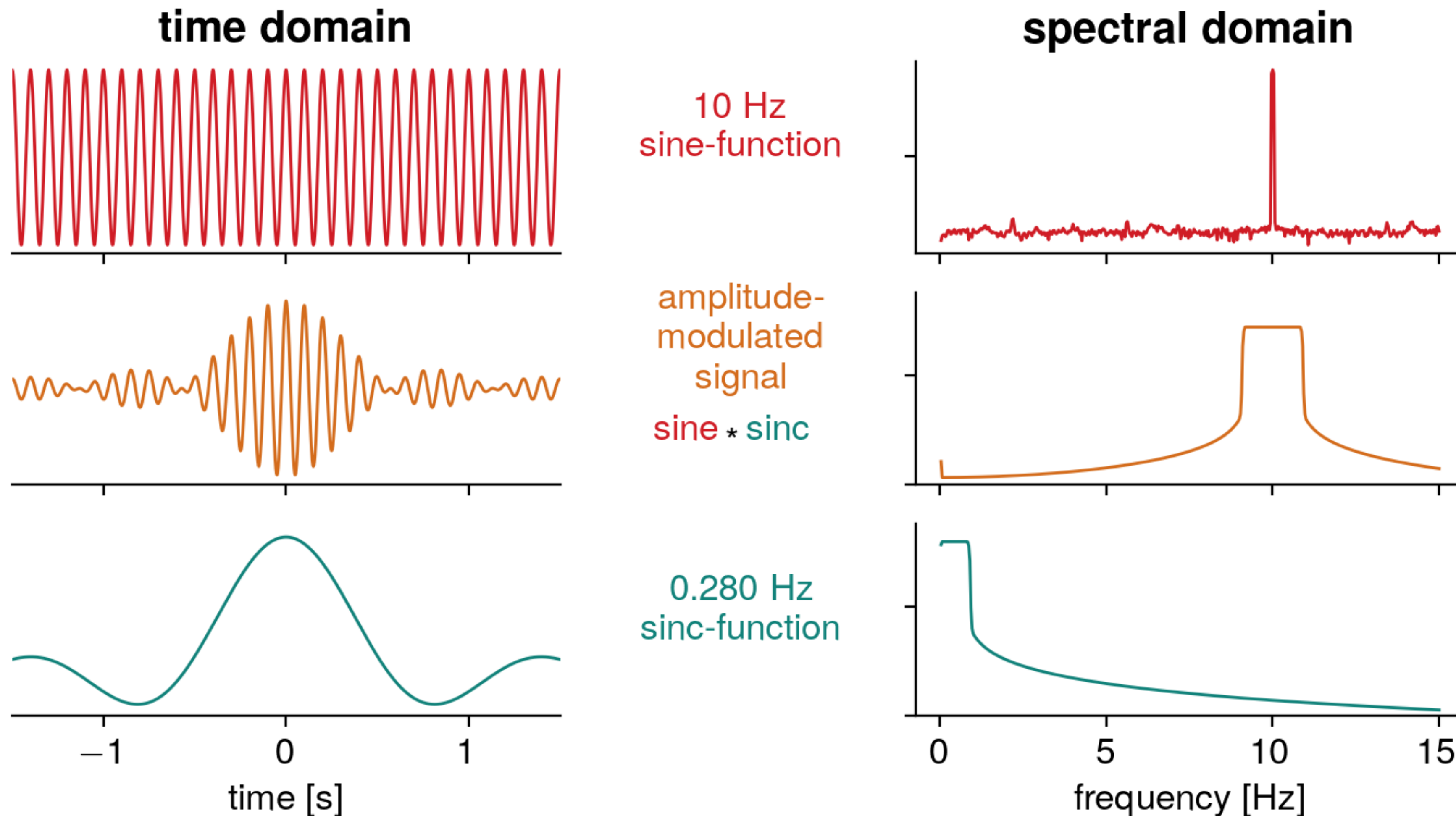
effects of amplitude modulation on spectrum

- amplitude modulation can contribute to a broadened spectral peak.

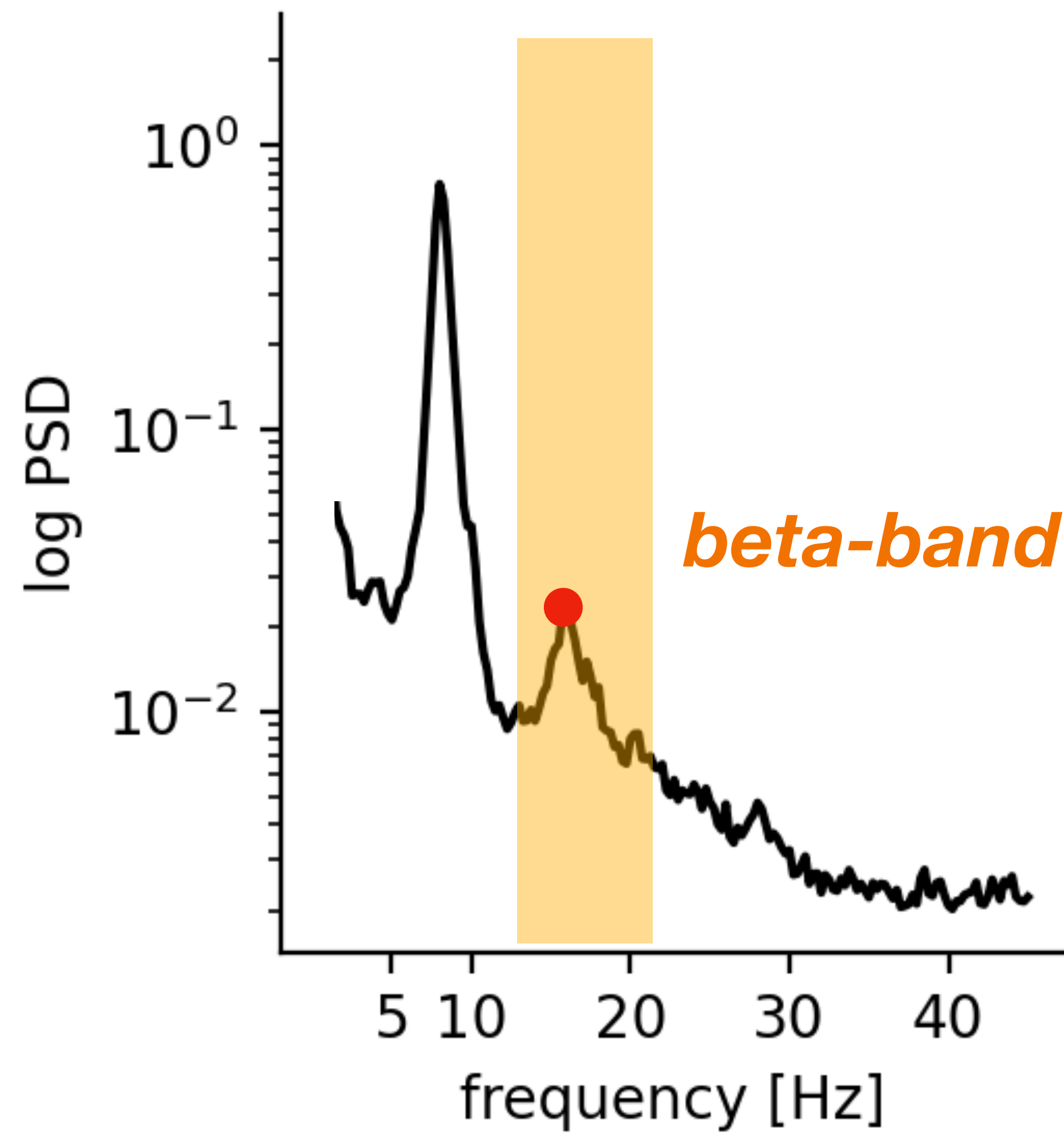


effects of amplitude modulation on spectrum

- amplitude modulation can contribute to a broadened spectral peak.

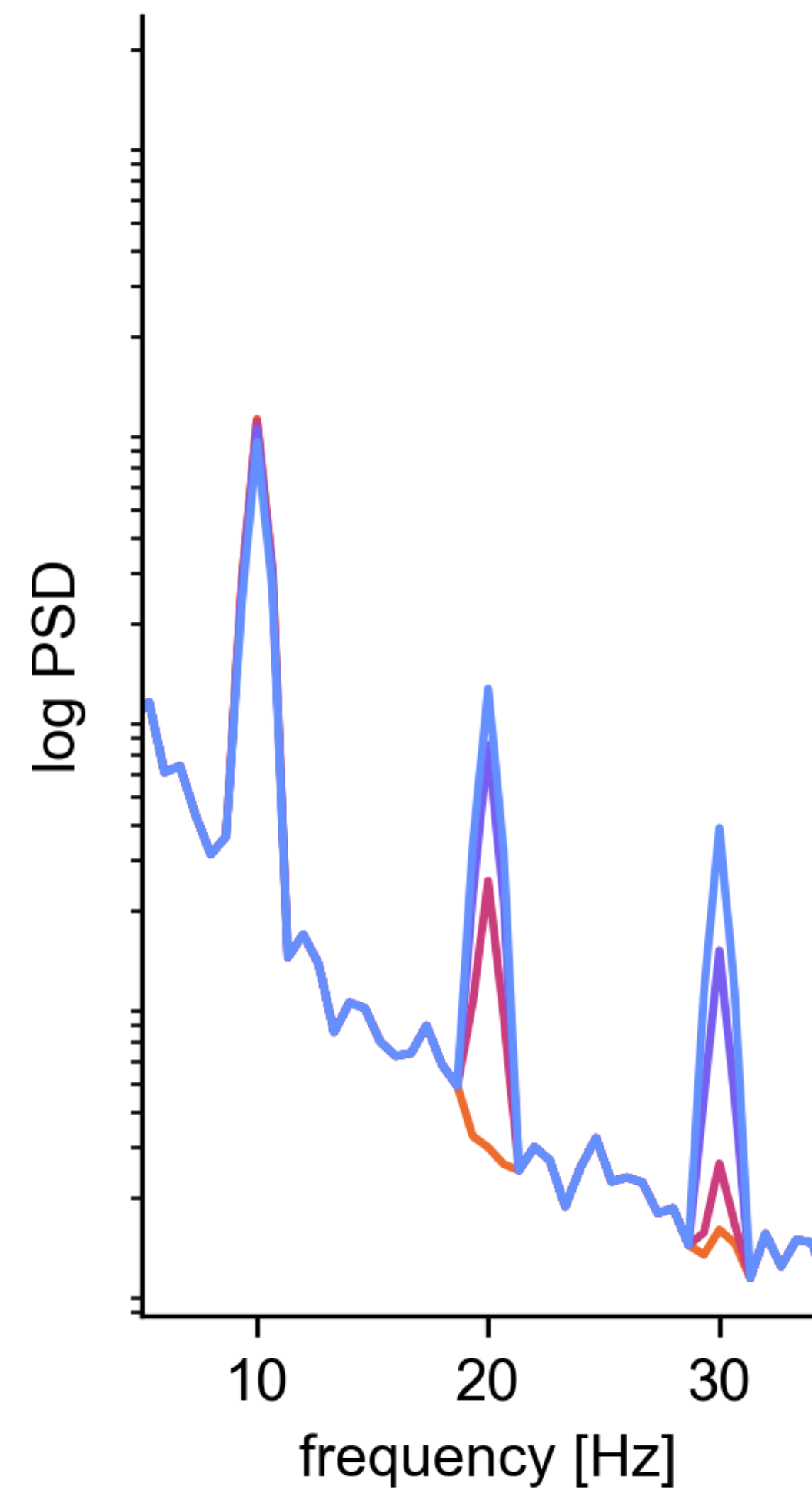
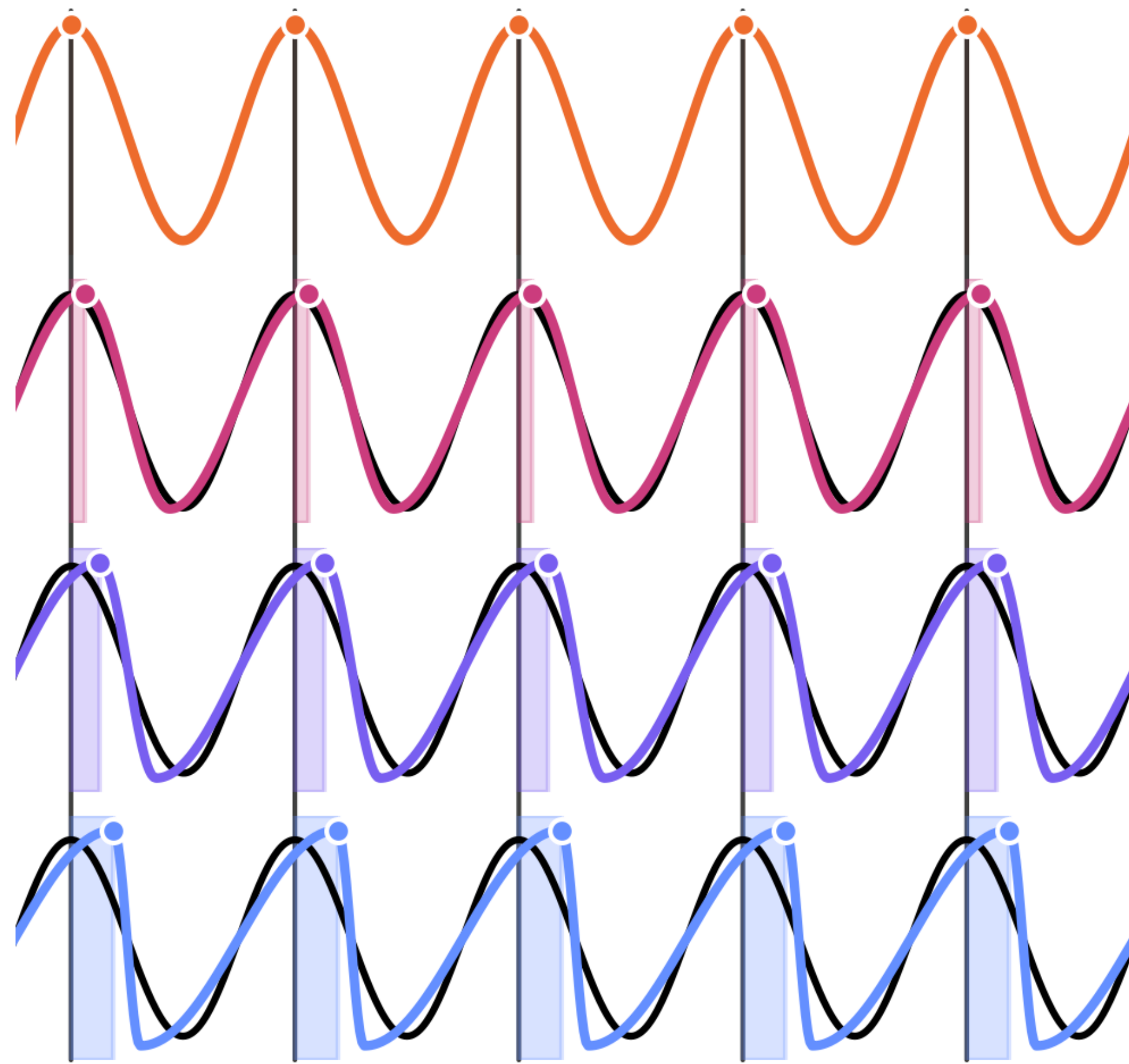


higher frequency spectral peaks



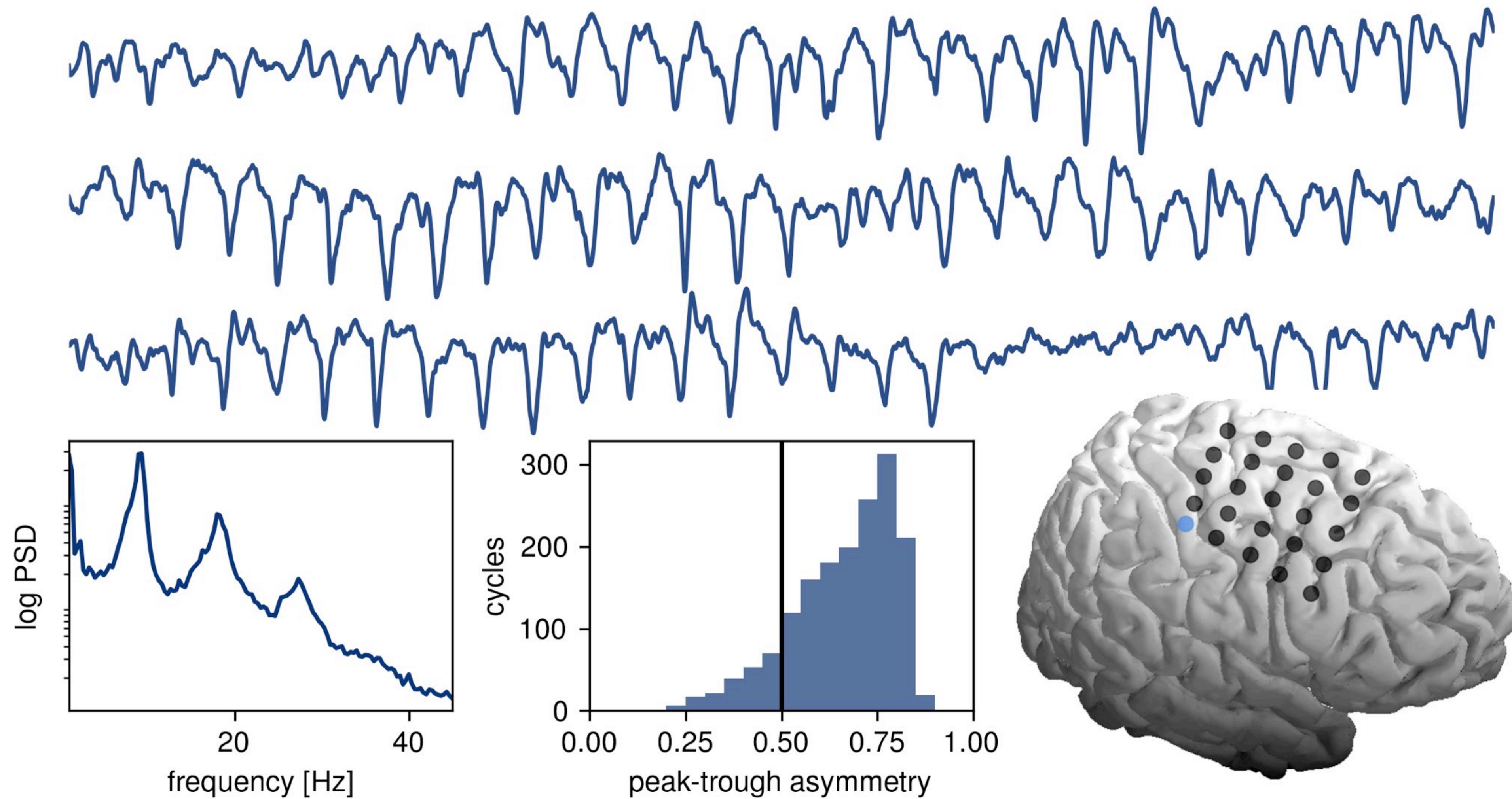
- ✓ verify presence of peak
- ✓ identify frequency of peak in beta-band
- additional spectral peaks in higher frequency bands: genuine rhythms or harmonic contributions?

pitfalls: waveform shape & spectral peaks

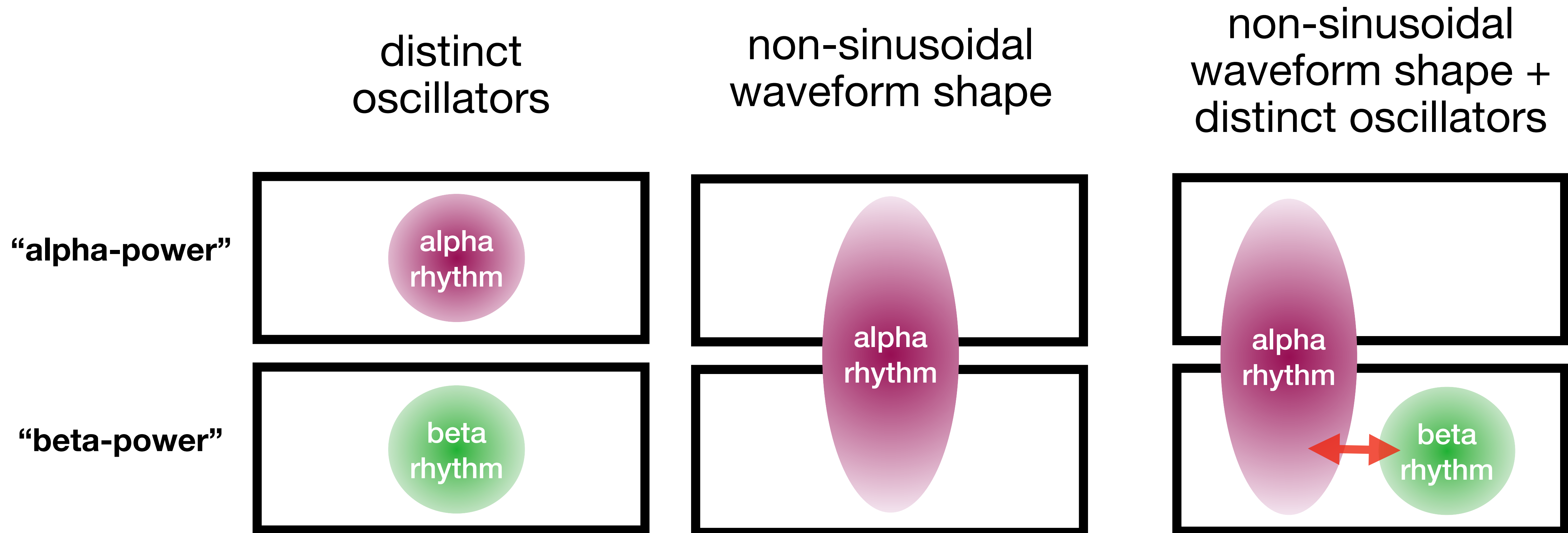


- individual spectral peaks $\neq$ independent rhythms
- non-sinusoidal waveforms $\rightarrow$ harmonic peaks in the spectrum.

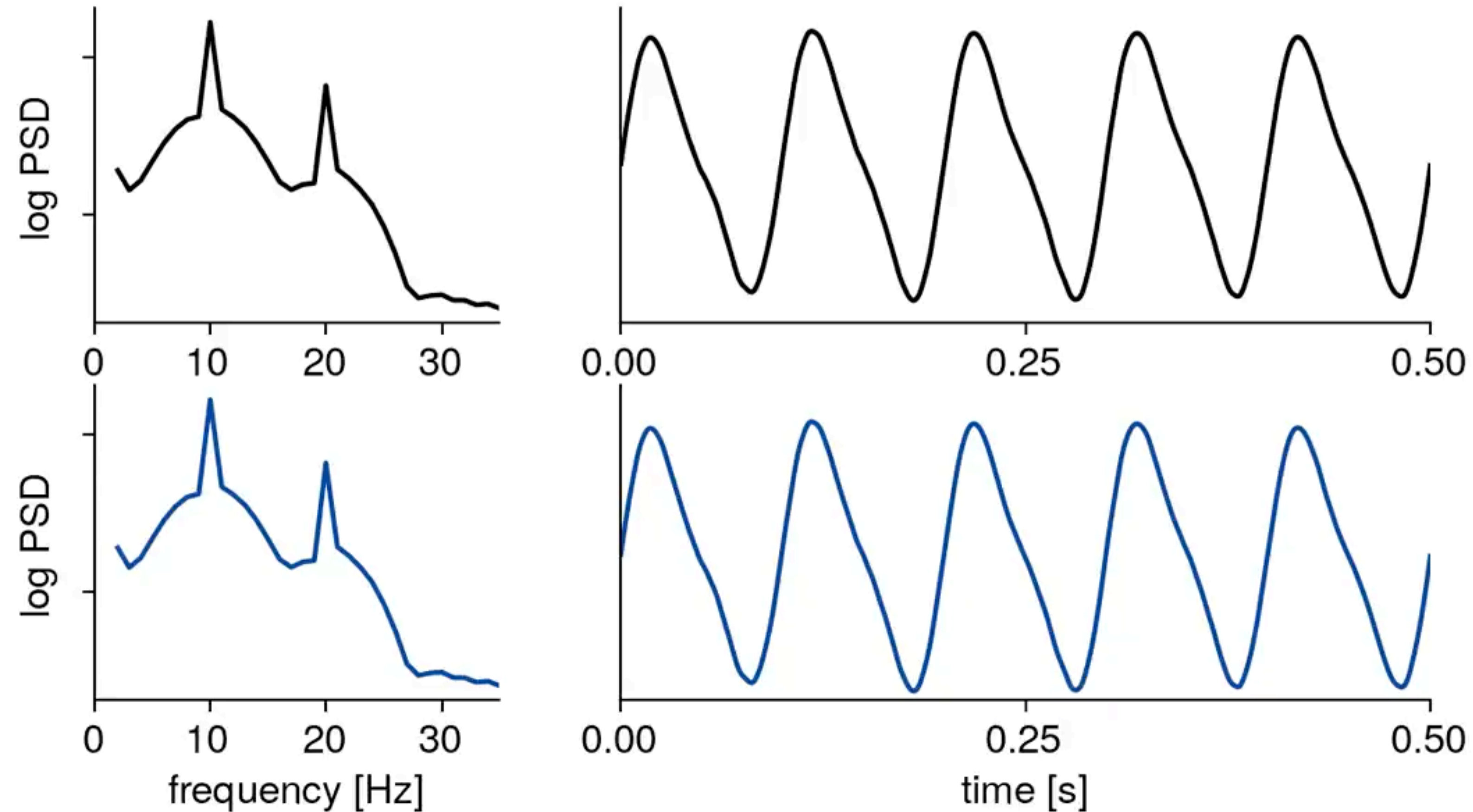
example: non-sinusoidal waveform in ECoG data



waveform shape & spectral peaks: concepts

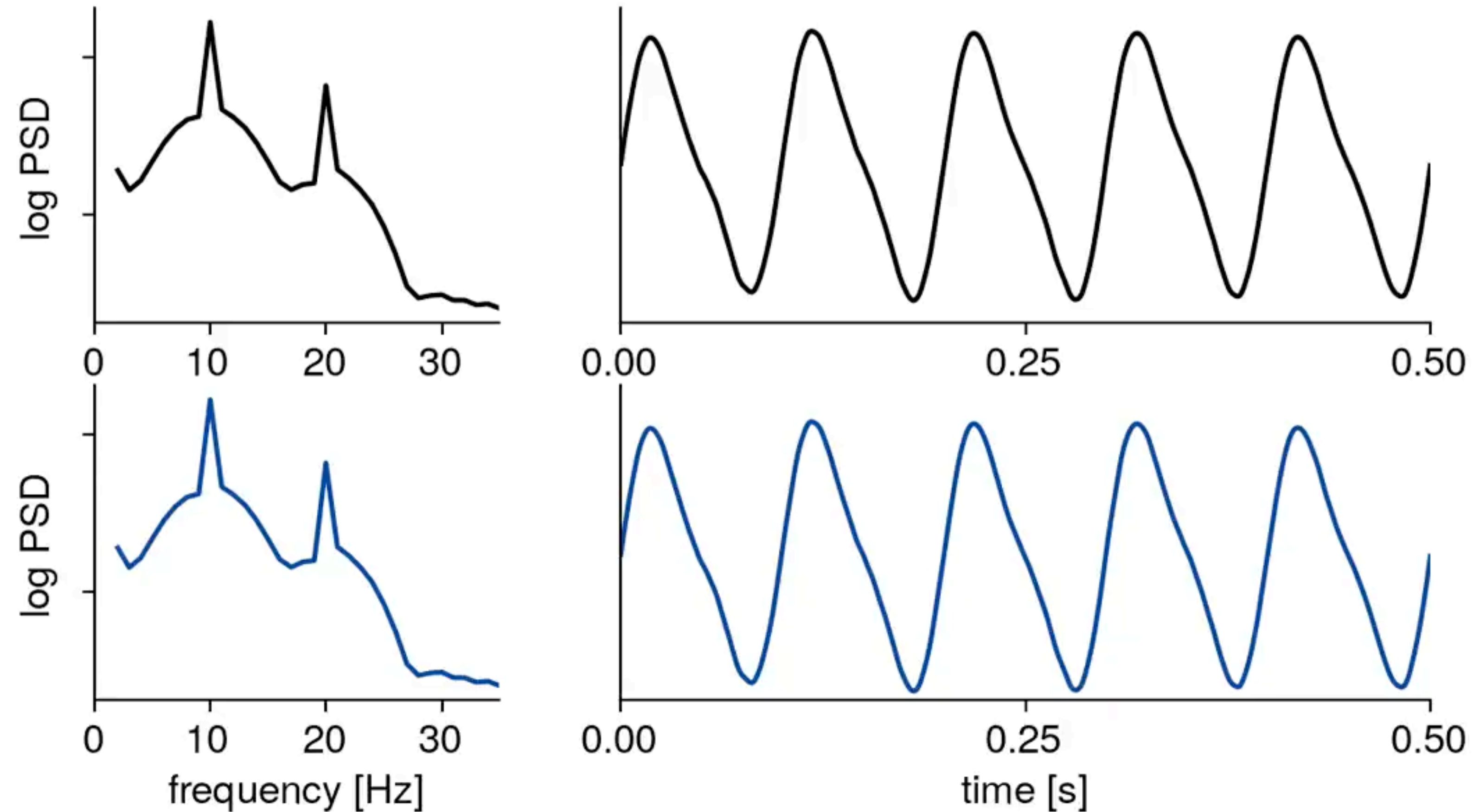


what about phase?



same spectrum – different time domain signals: the power spectrum only captures a part of the available information

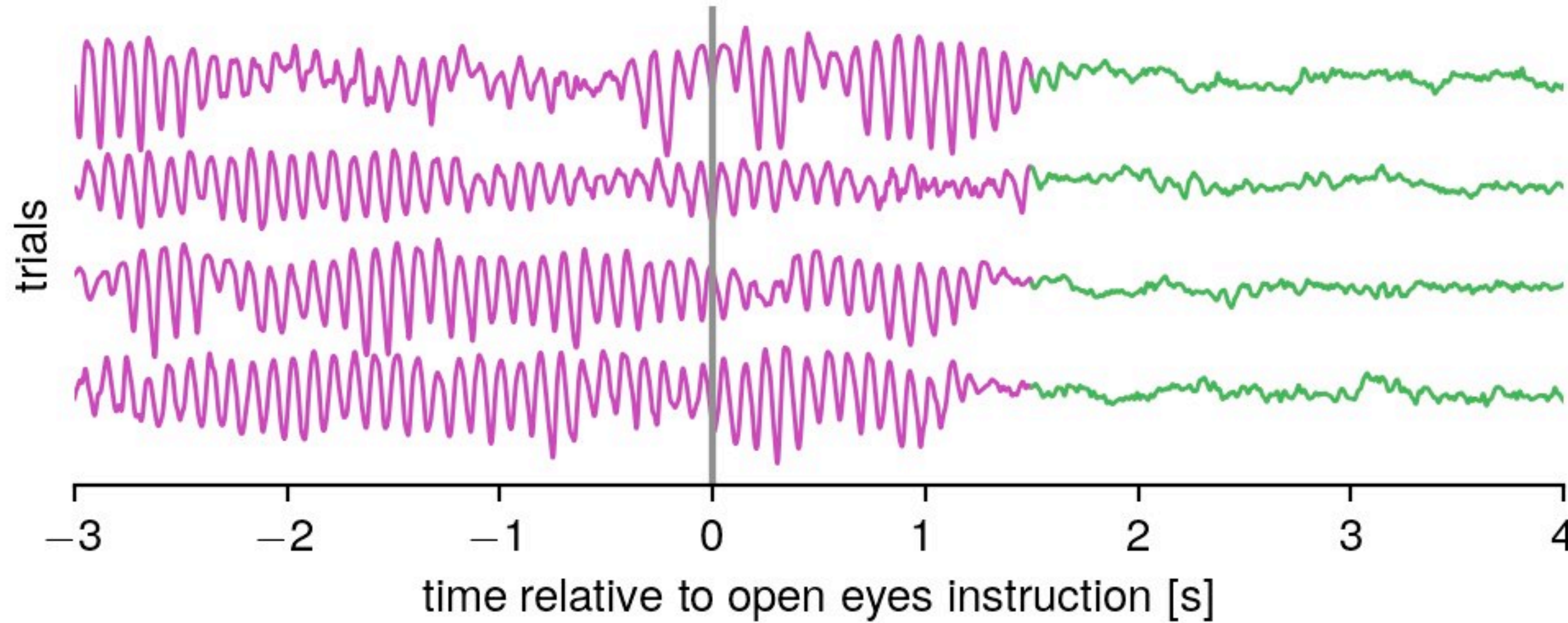
what about phase?



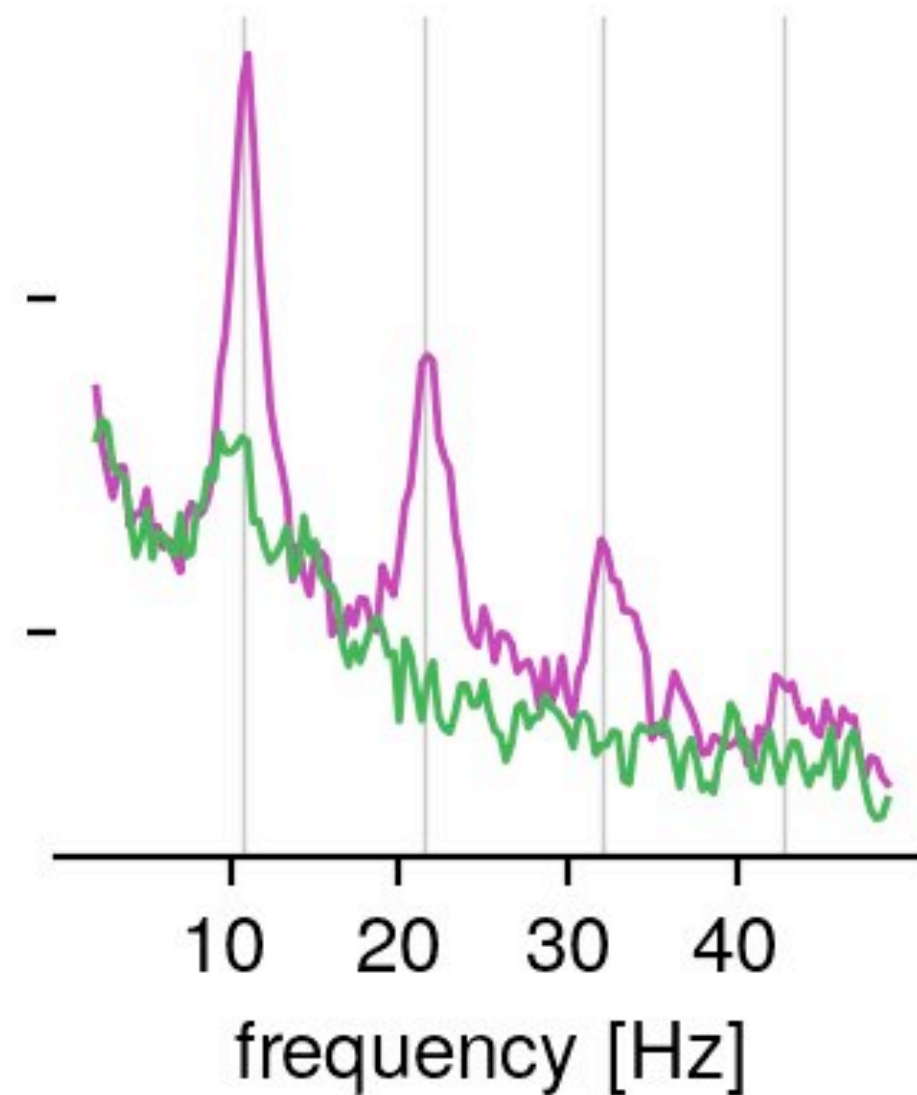
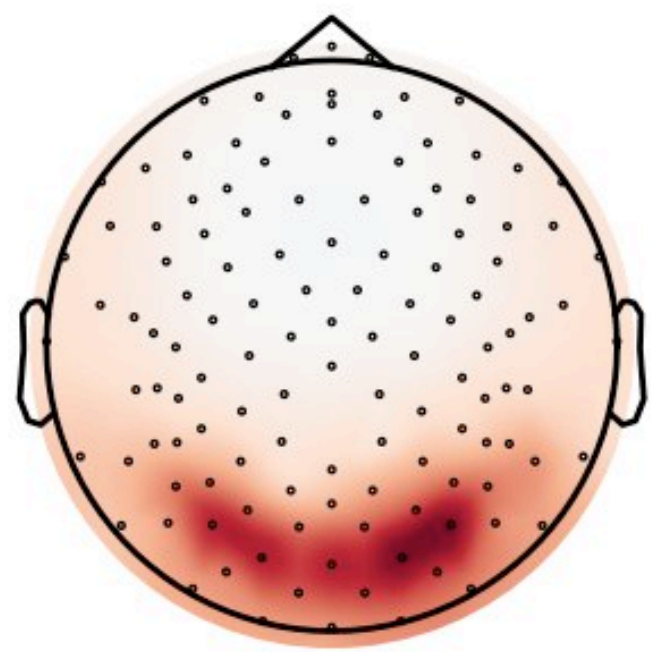
same spectrum – different time domain signals: the power spectrum only captures a part of the available information

time-frequency analysis

motivation



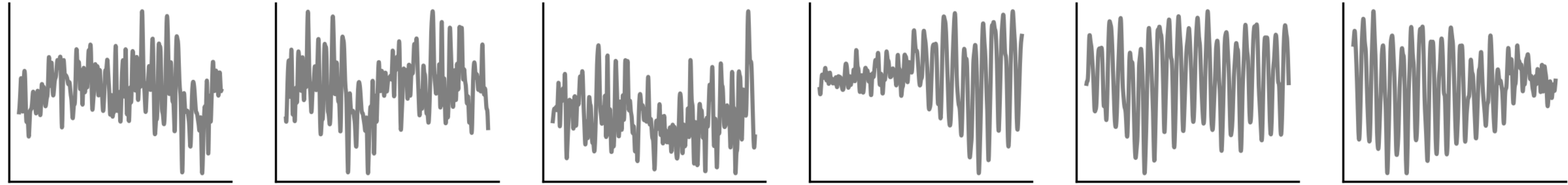
- How to assess temporal dynamics across a trial?



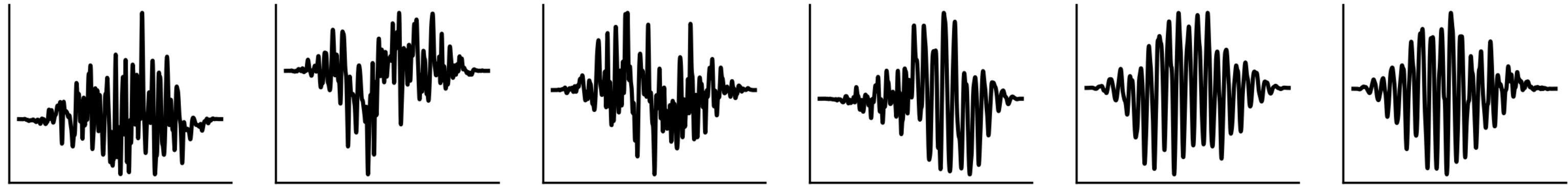
→ **time-frequency representation! (TFR)**

computation

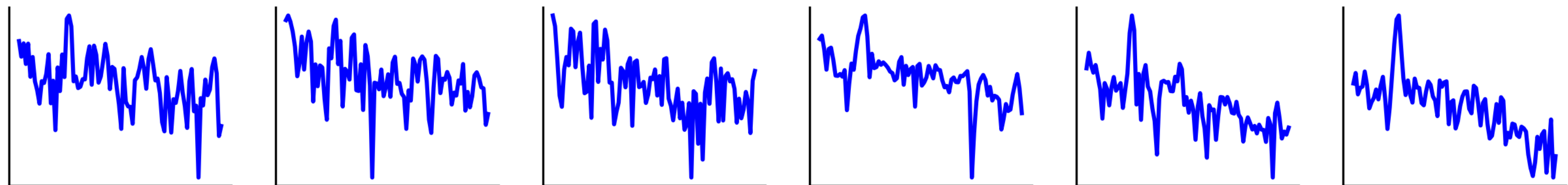
time series, cut into small segments
[nr_segments x nr_samples]



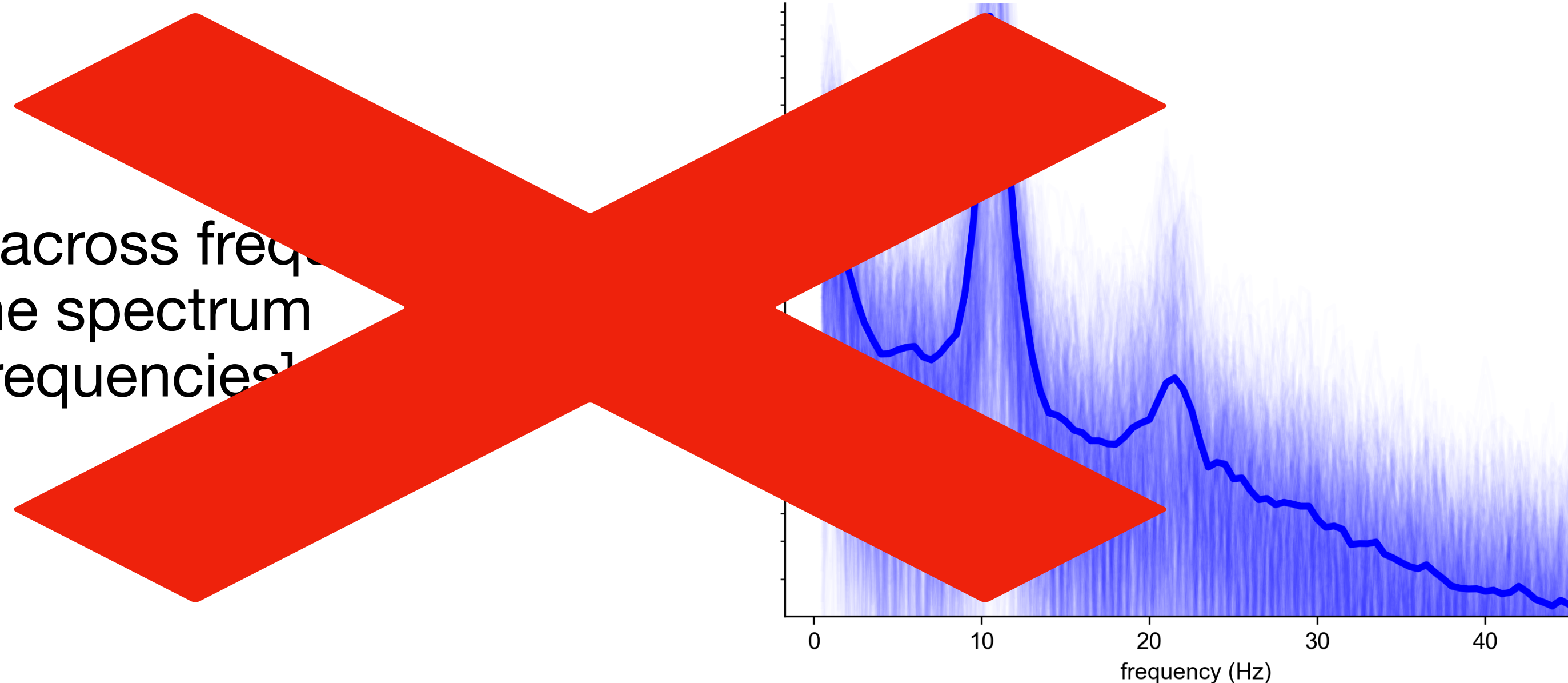
time series, multiplied with a
windowing function
[nr_segments x nr_samples]



spectra for each segment
[nr_segments x nr_frequencies]

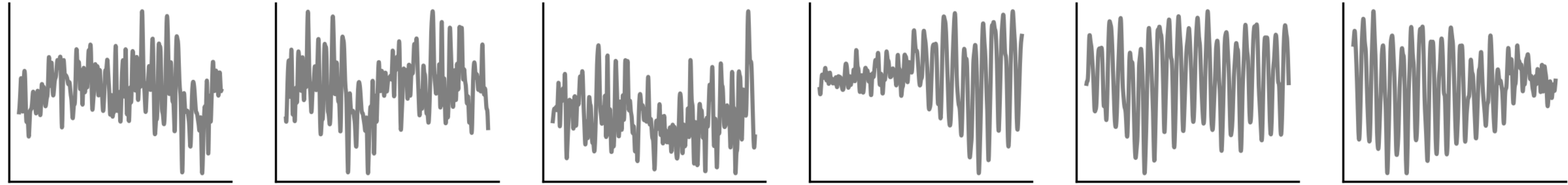


average across frequency
obtain the spectrum
[1 x nr_frequencies]

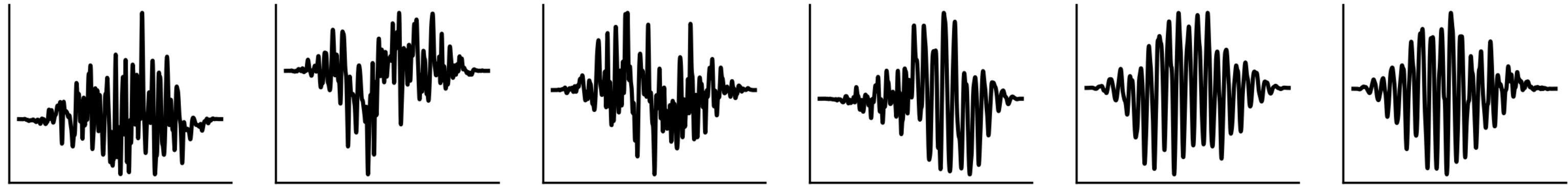


computation

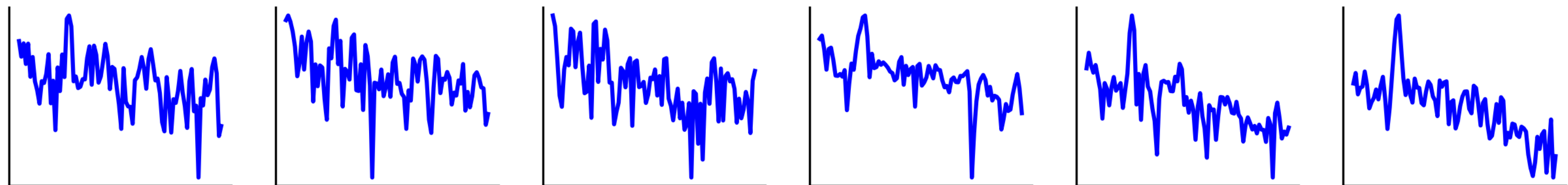
time series, cut into small segments
[nr_segments x nr_samples]



time series, multiplied with a
windowing function
[nr_segments x nr_samples]

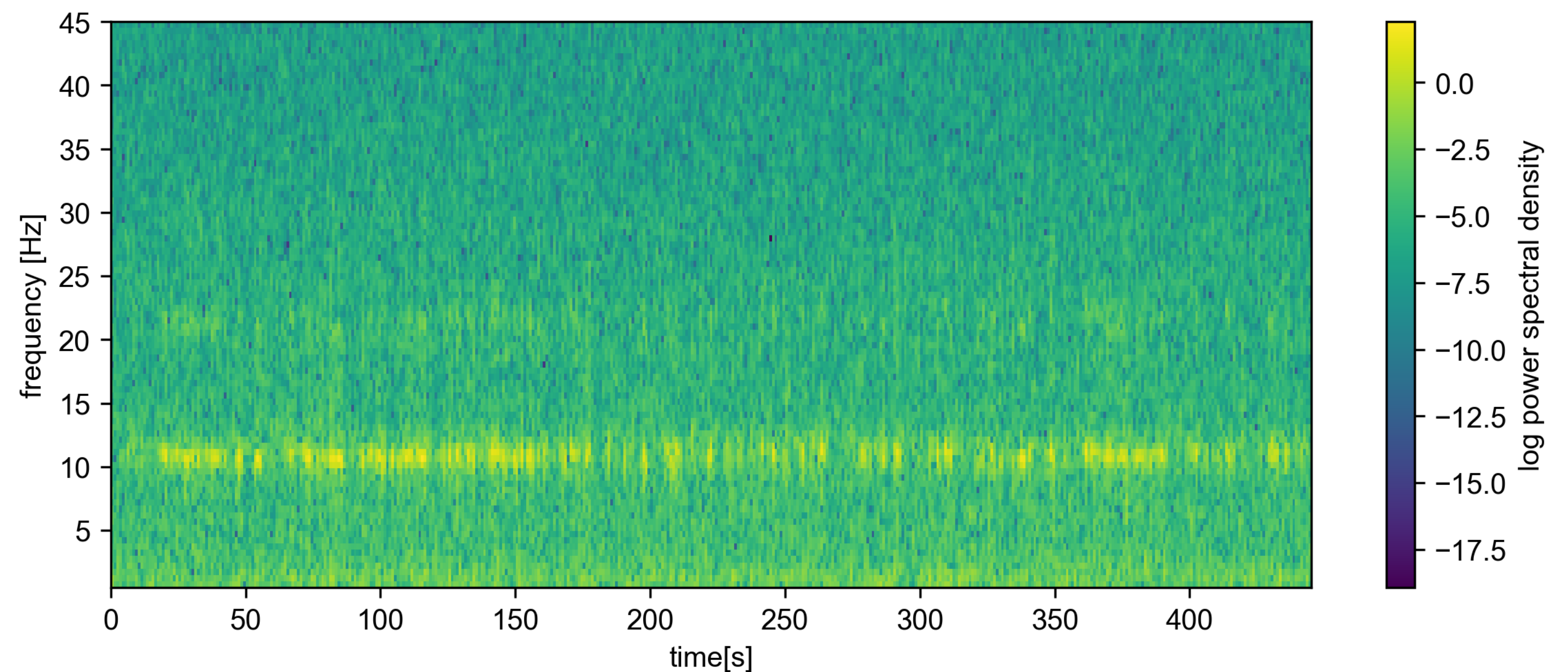


spectra for each segment
[nr_segments x nr_frequencies]

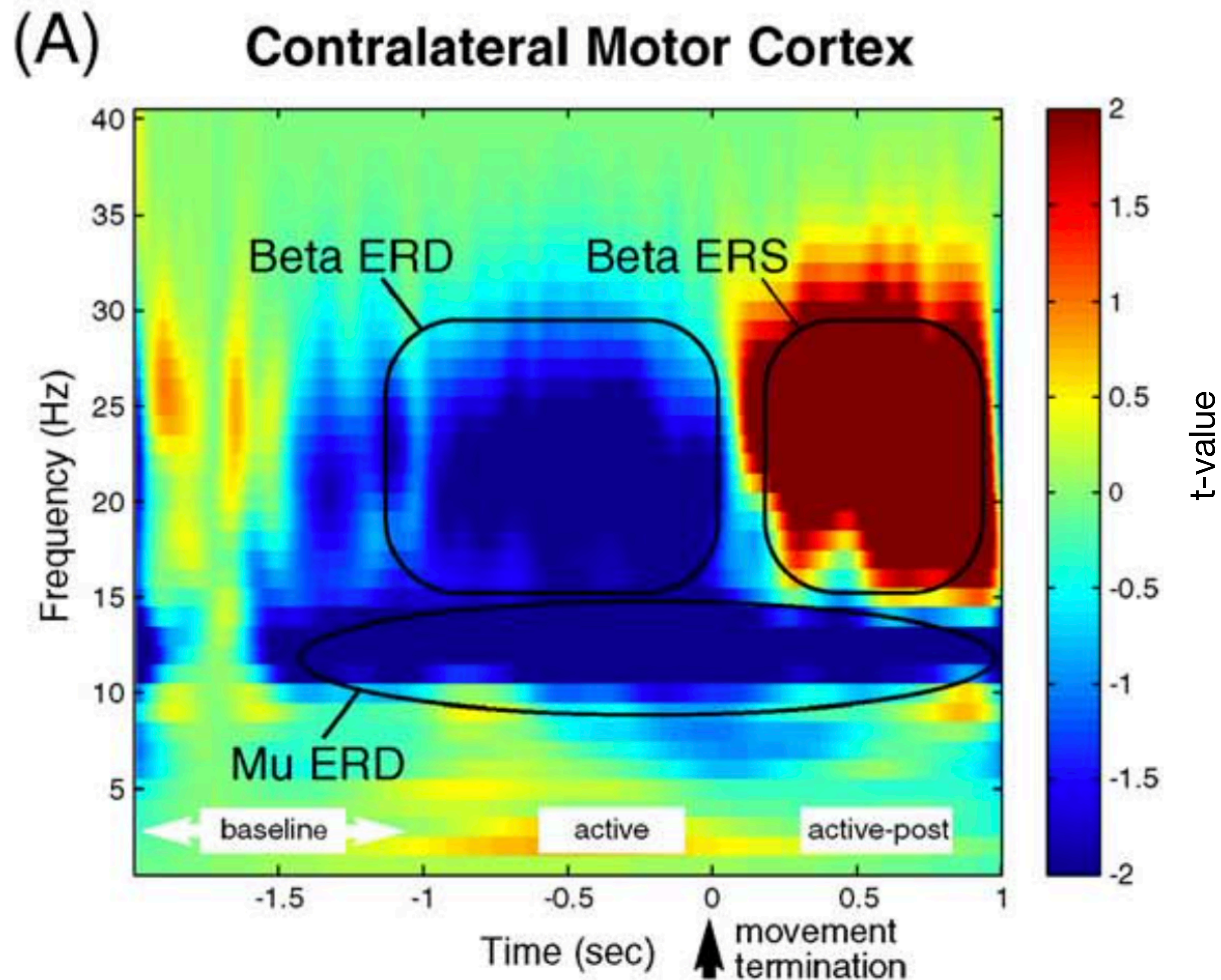


rotate by 90 degrees
stack spectra from segments
& plot in color

→ time-frequency representation



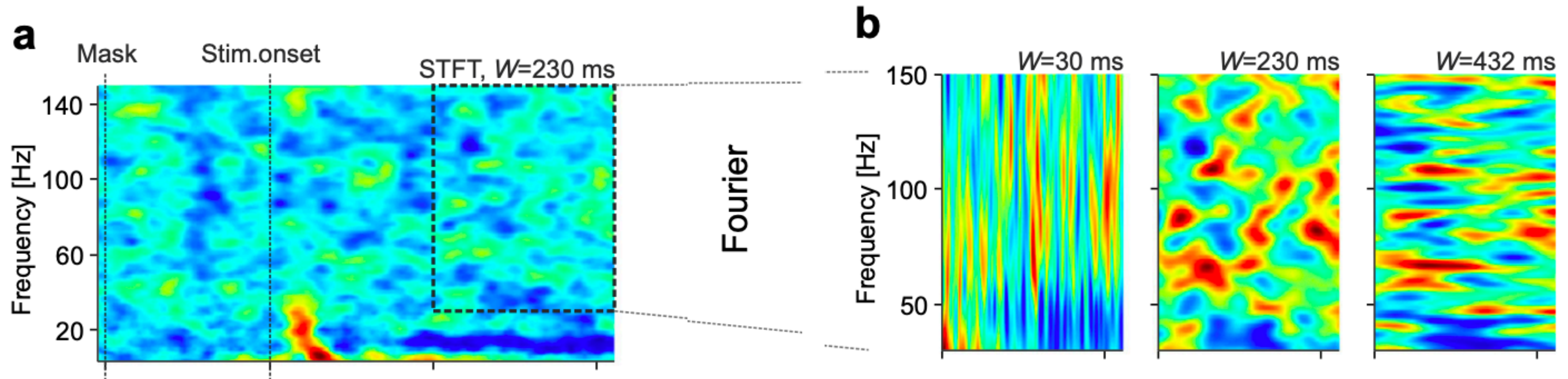
example output for MEG data



- rich spectral power dynamics in different frequency bands
- often, a baseline/normalization procedure or contrast is employed.

methods: parameters

- influence of parameters: window length / number of cycles



methods: parameters

- different approaches for selecting segment length

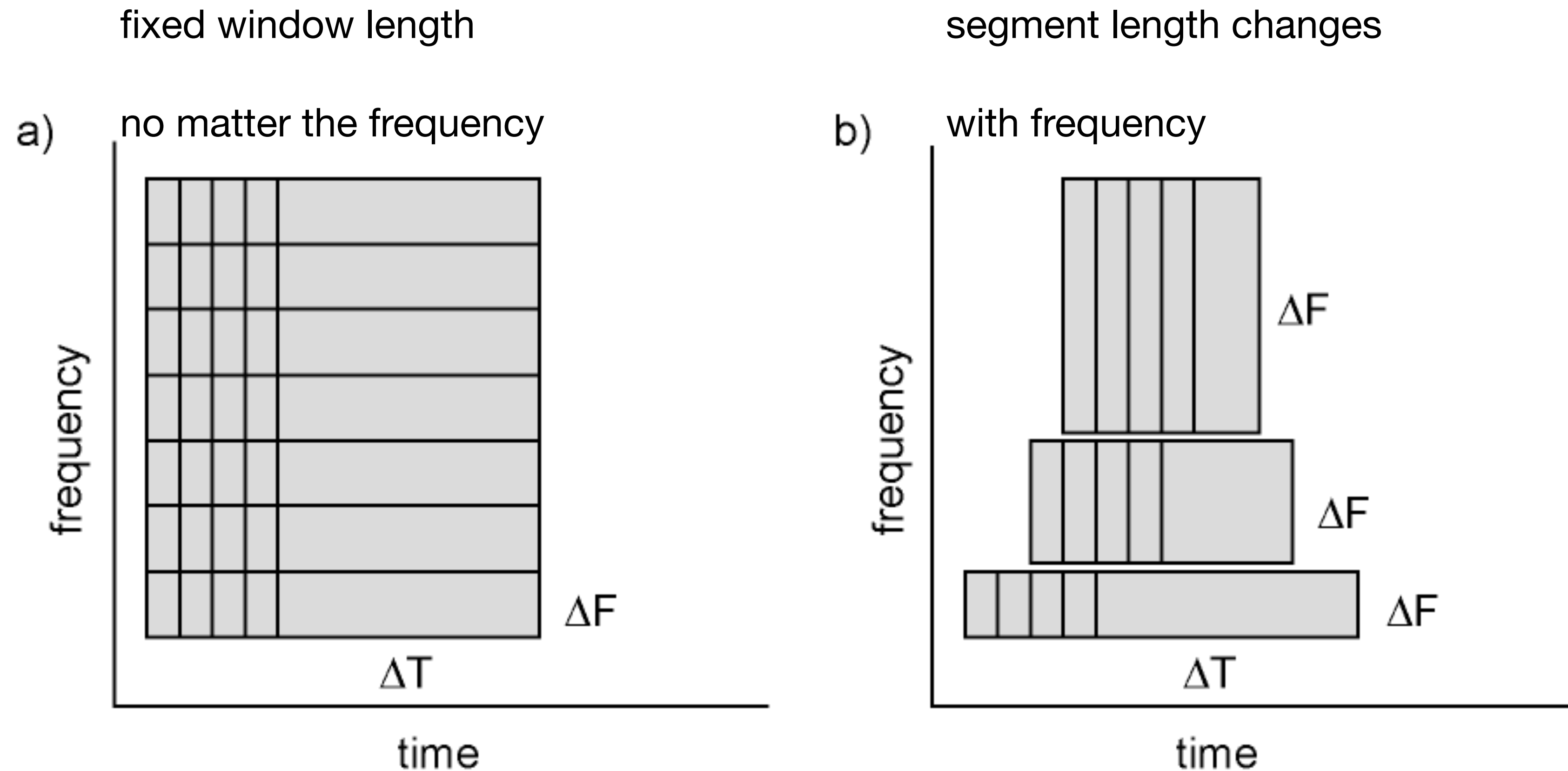
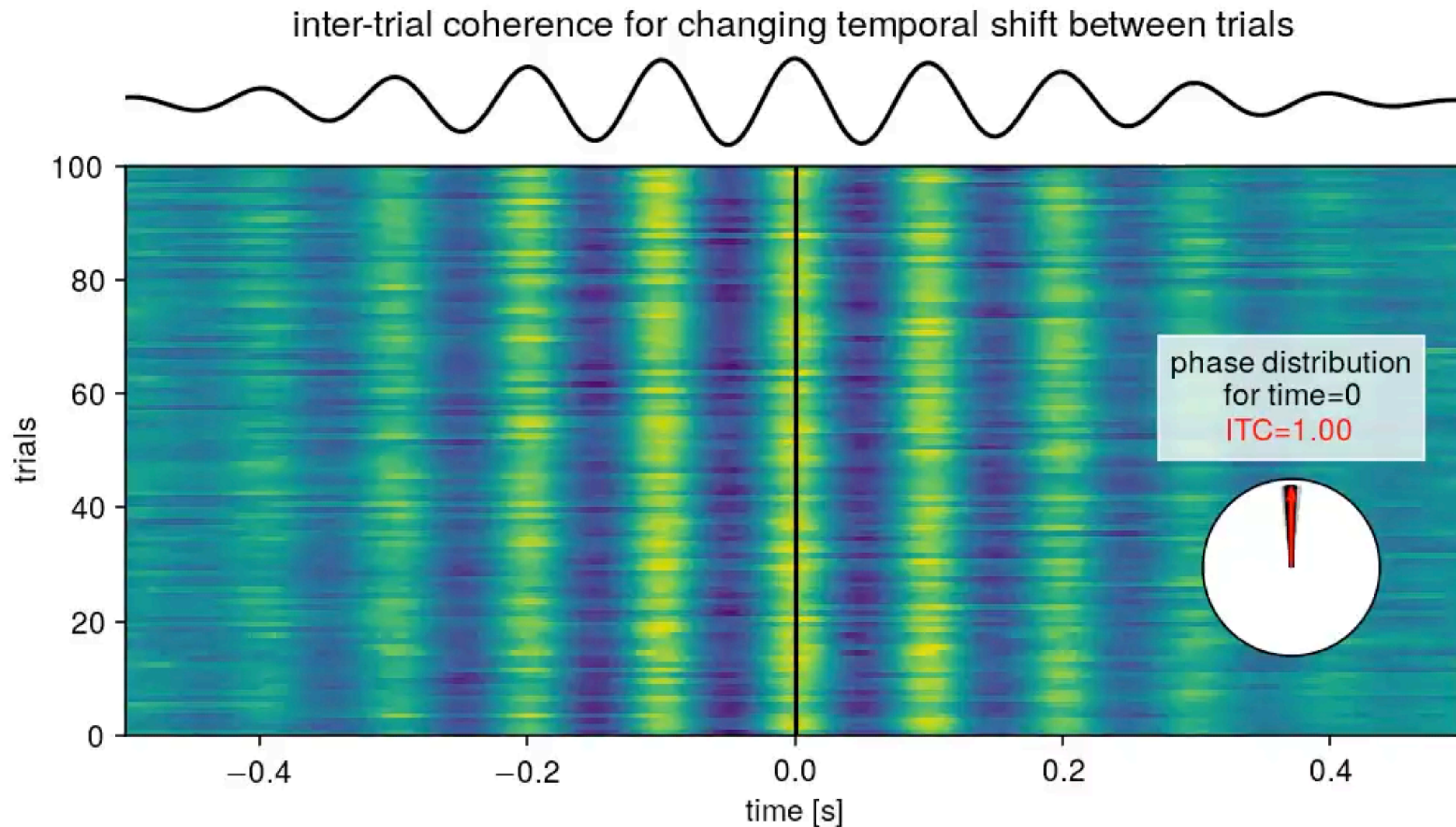


figure from:

methods – inter-trial coherence

- phase information from the time-frequency representation can be used to investigate inter-trial coherence (ITC)



methods – inter-trial coherence

- comparing ITCs of two different trial groups
- research question: does oscillation phase matter for perception of phosphenes?
“optimal phase”
 - two trial groups: phosphenes perceived vs phosphenes not perceived
 - compute ITC for both conditions
 - check if statistically different
- inference: oscillatory phase influences whether participants perceive a phosphene

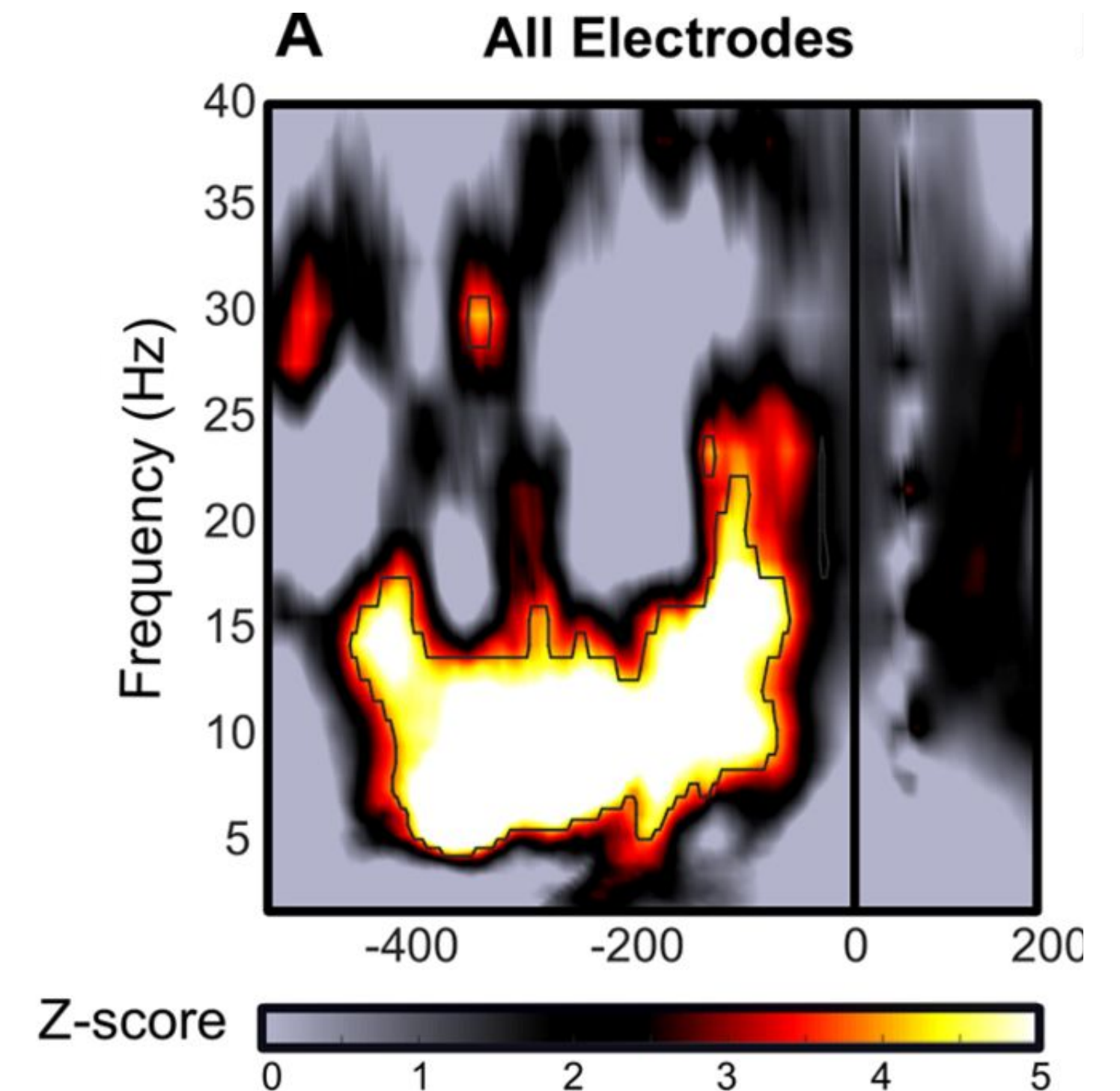
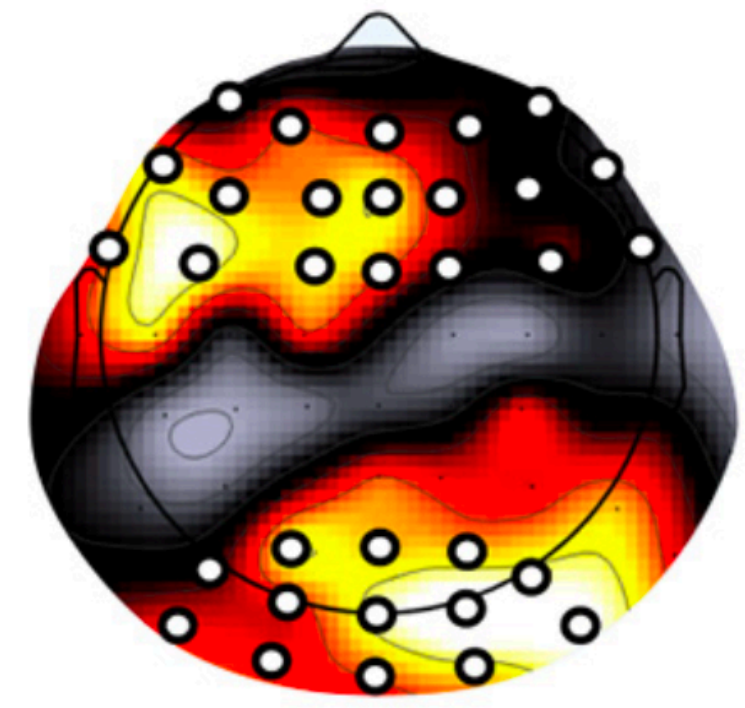


figure from: Fakche et al. (2022)

concepts: evoked vs. induced

- order of operations matters

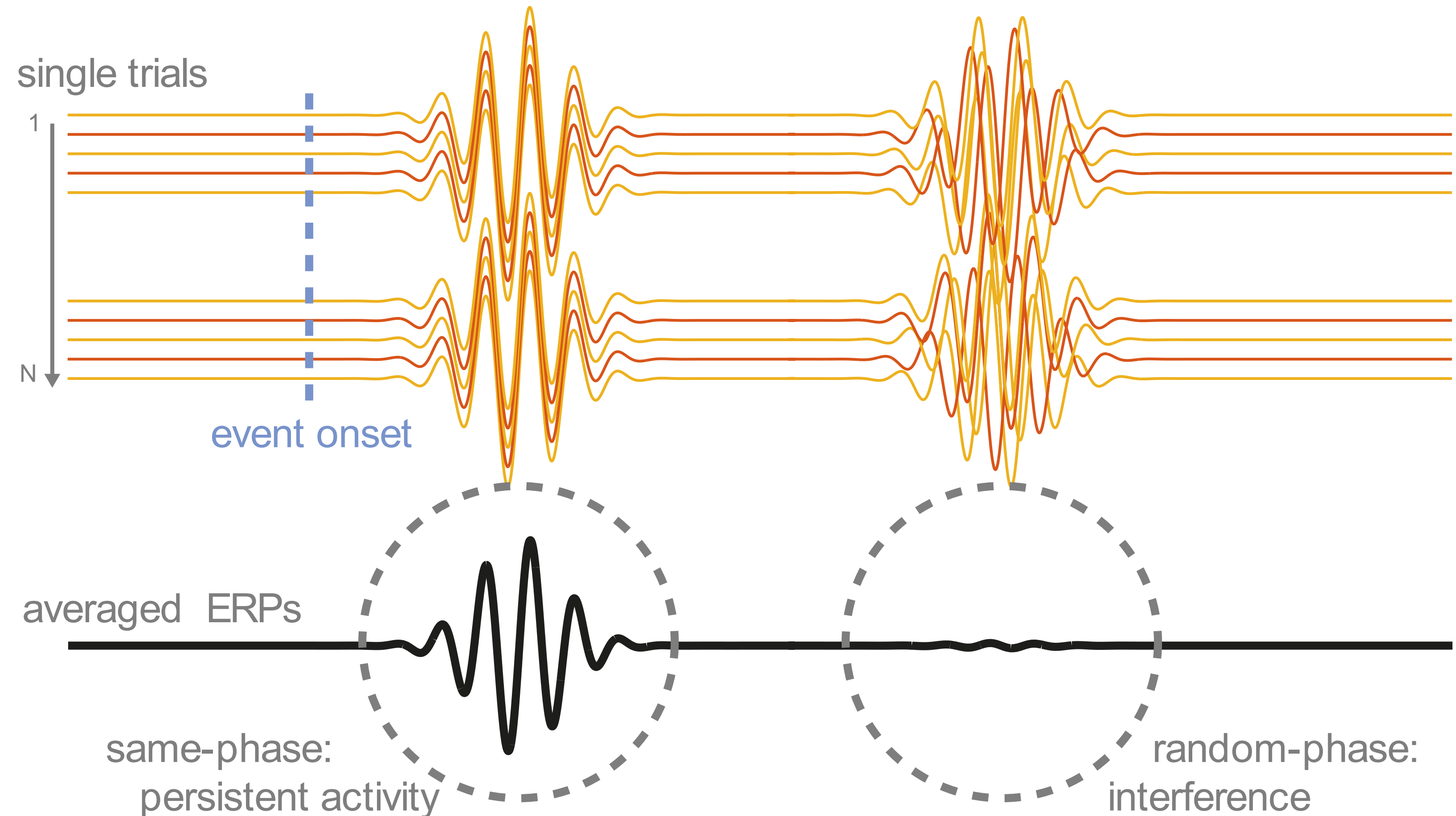
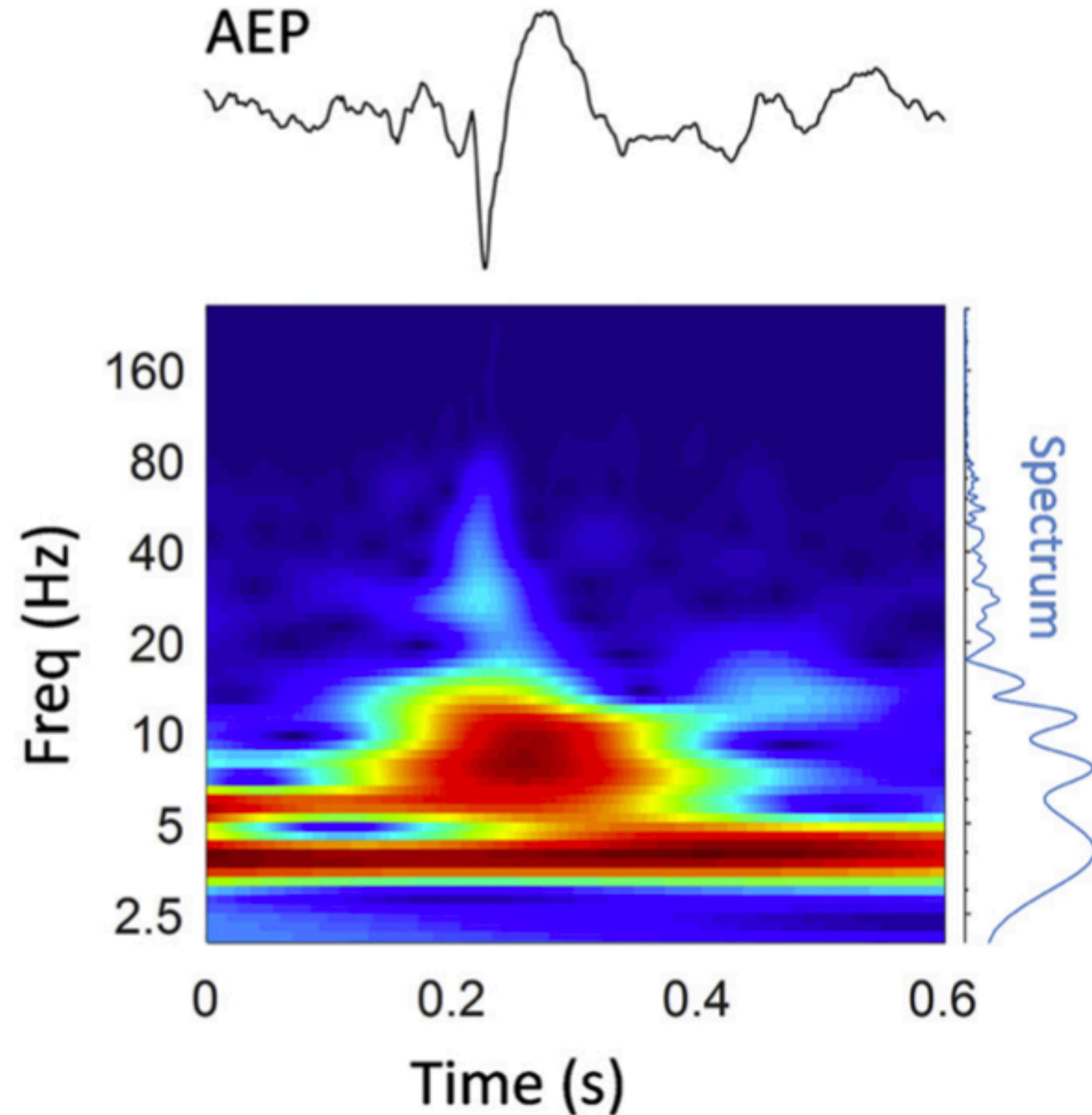


figure from: B. Ehinger:
<https://www.s-ccs.de/teaching-resources/open-teaching-graphics/Induced-Evoked/>

concepts: oscillations vs. evoked responses



- time-frequency representation of an evoked response shows a peak in the theta frequency band $\Leftrightarrow$ genuine rhythms

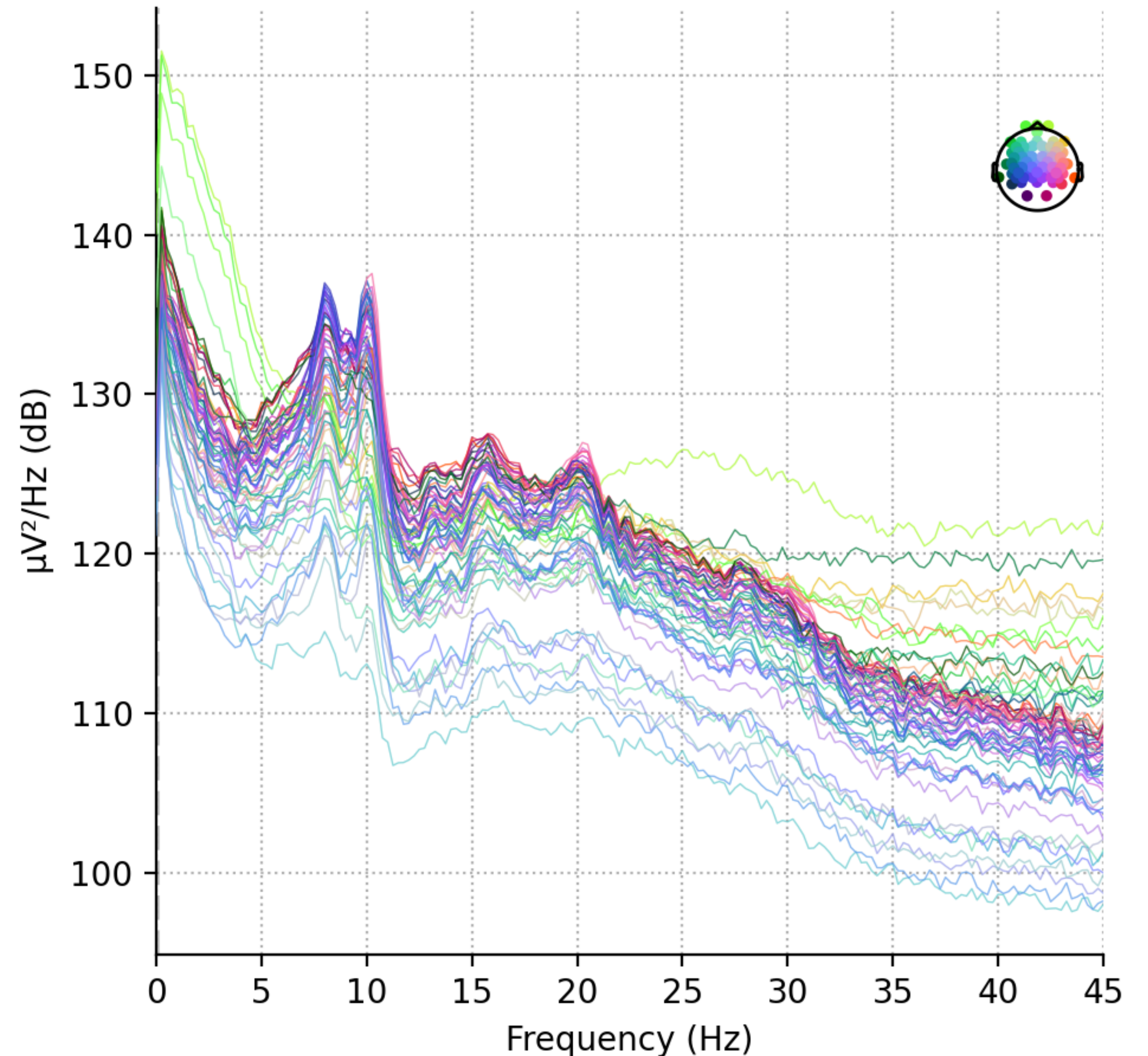
→ TFR on its own is agnostic about generative mechanisms!

figure from: Gourévitch et al.,
Neuroscience and Biobehavioral Reviews (2020)

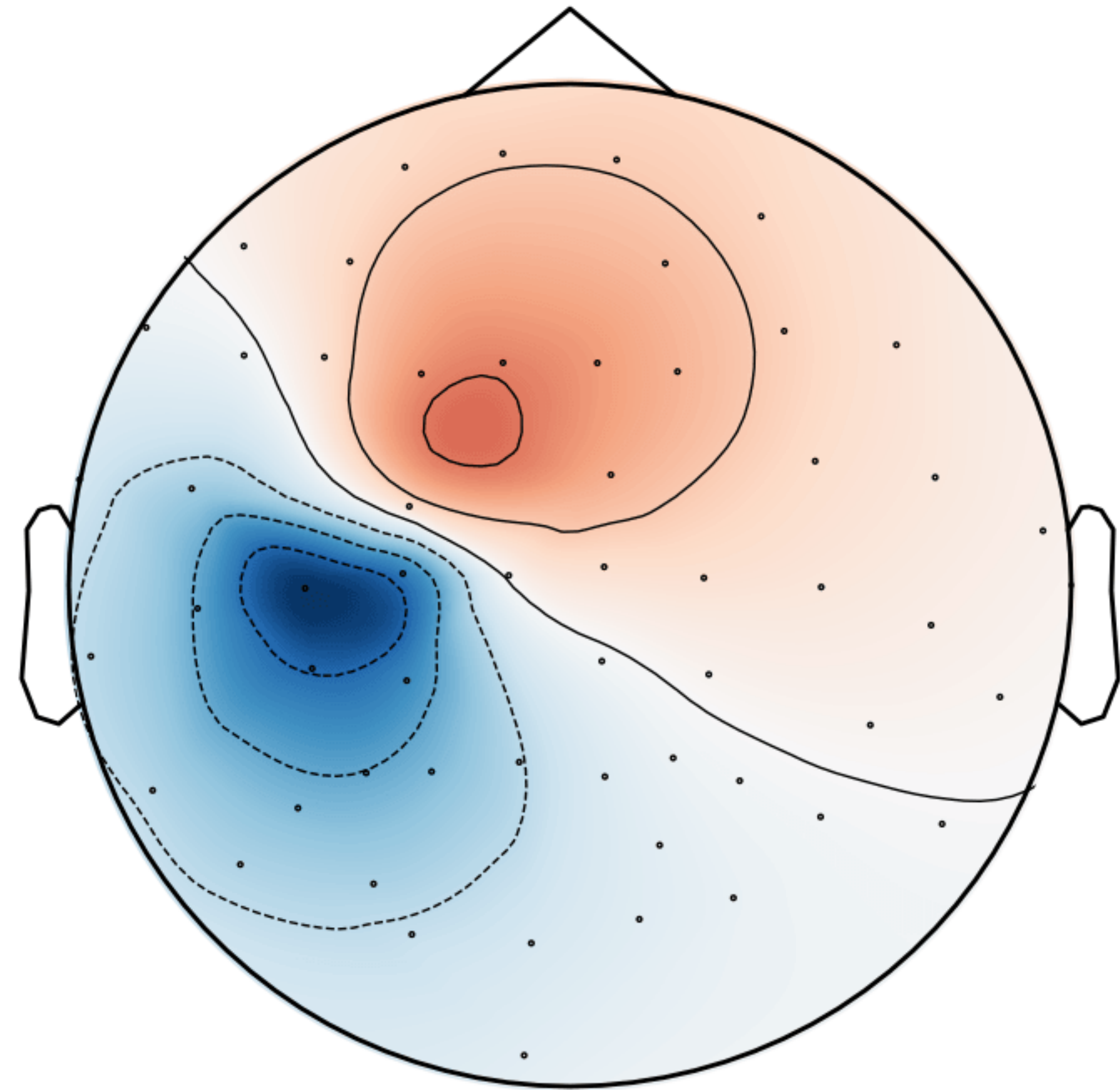
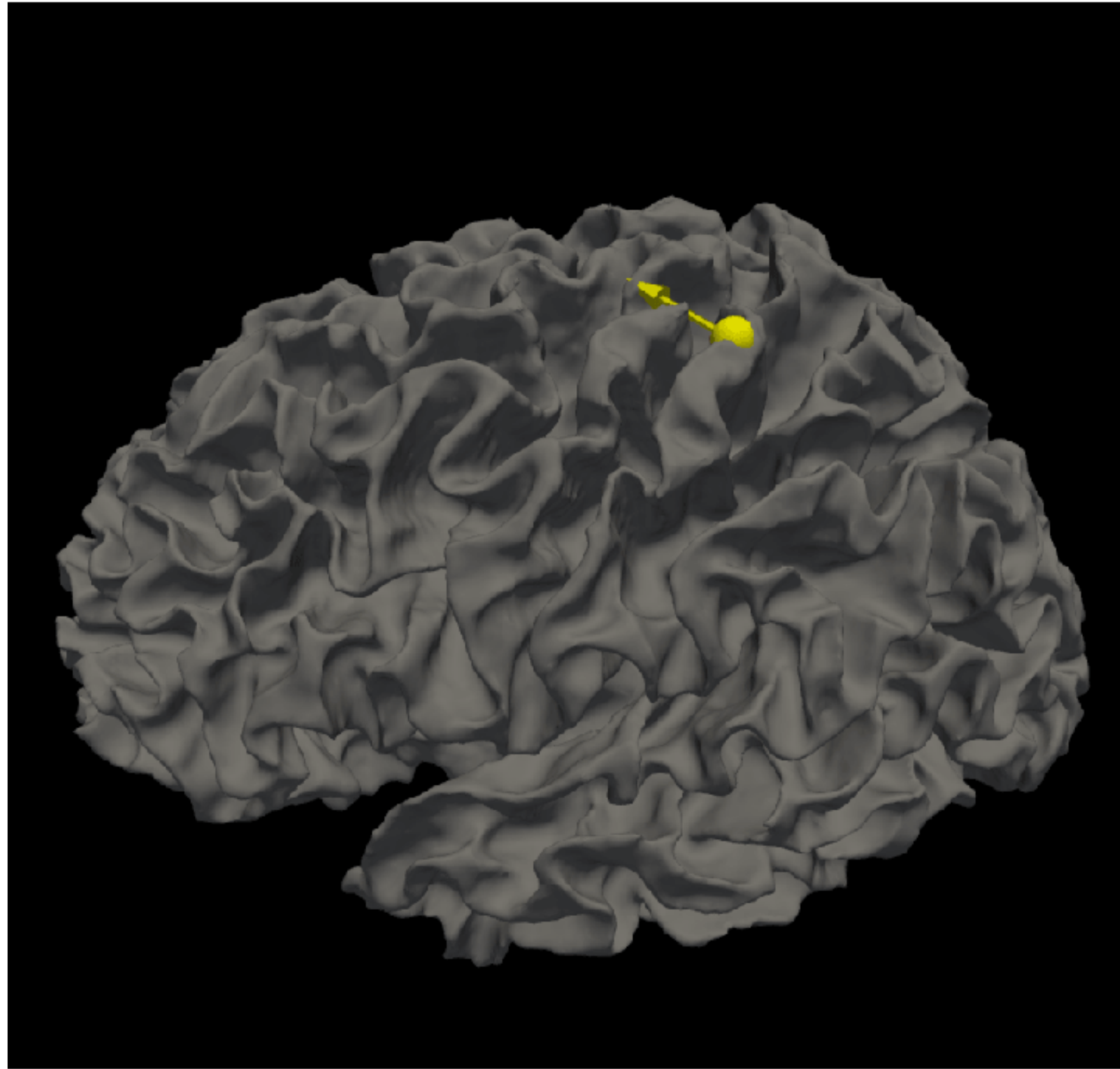
volume conduction

power spectra across channels – data

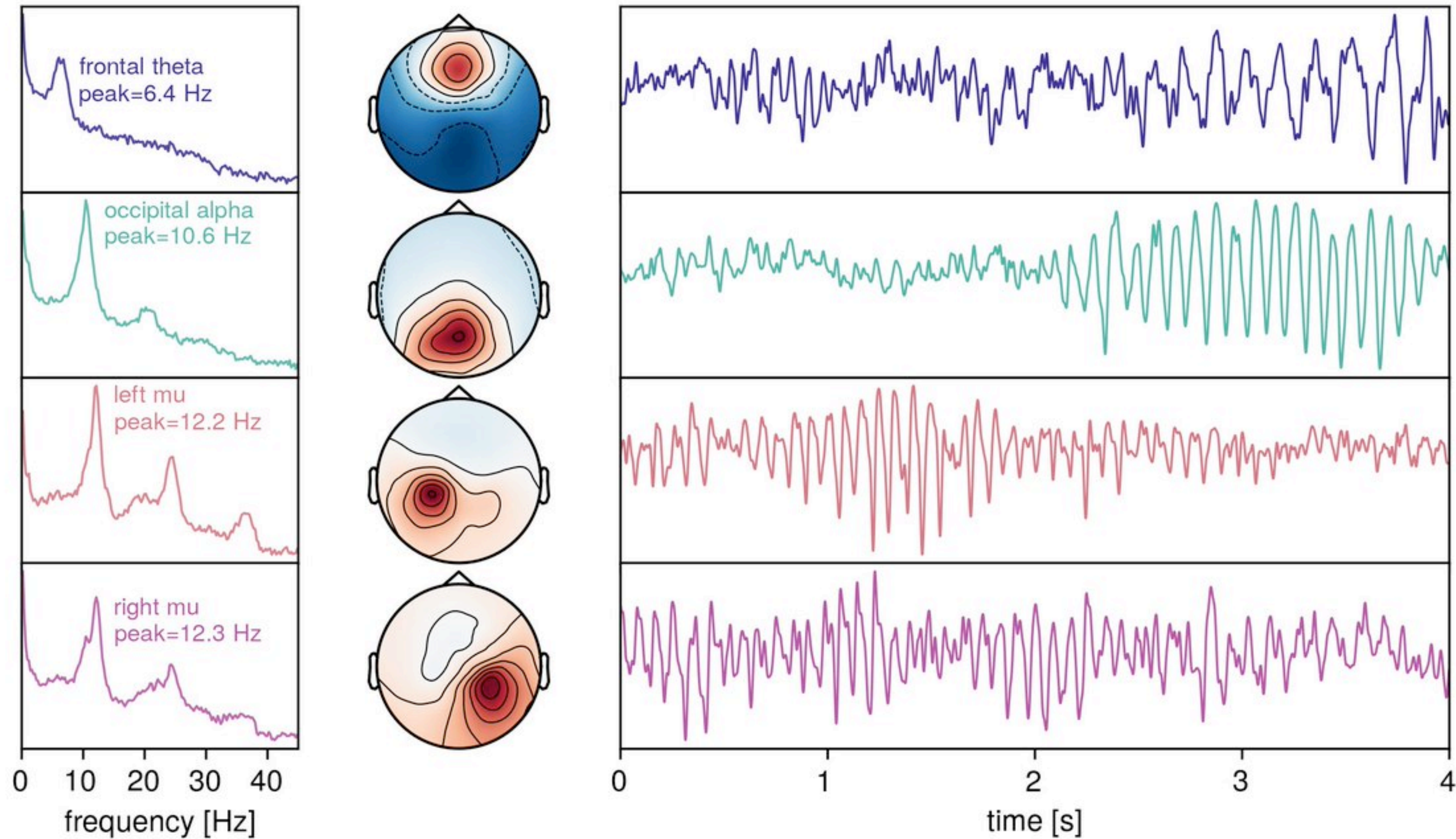
- channels are not independent
- different signal contributions will overlap and result in multiple spectral peaks



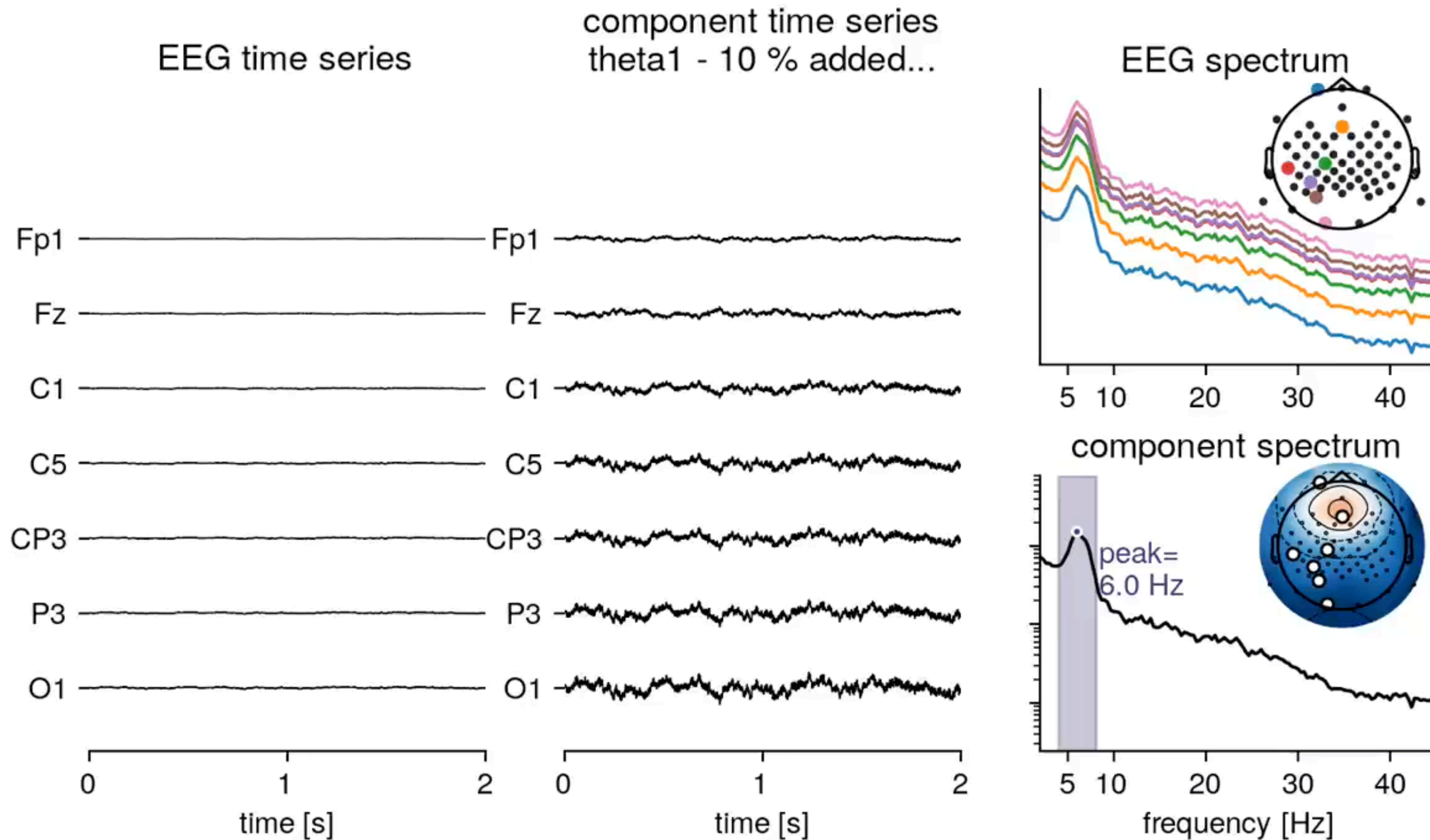
volume conduction – simulation



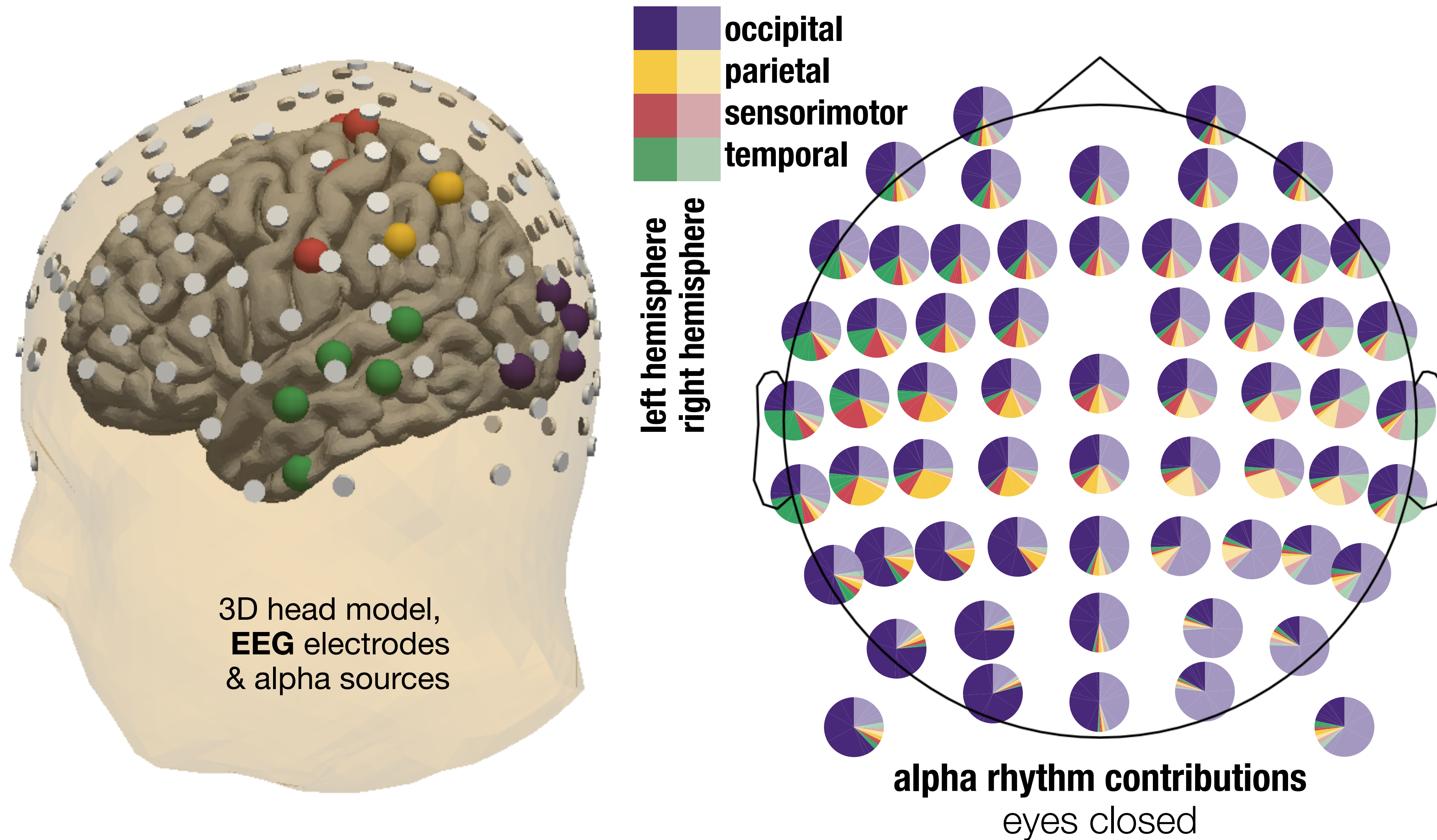
EEG is a mixture of different signals – data



EEG is a mixture of different signals – data

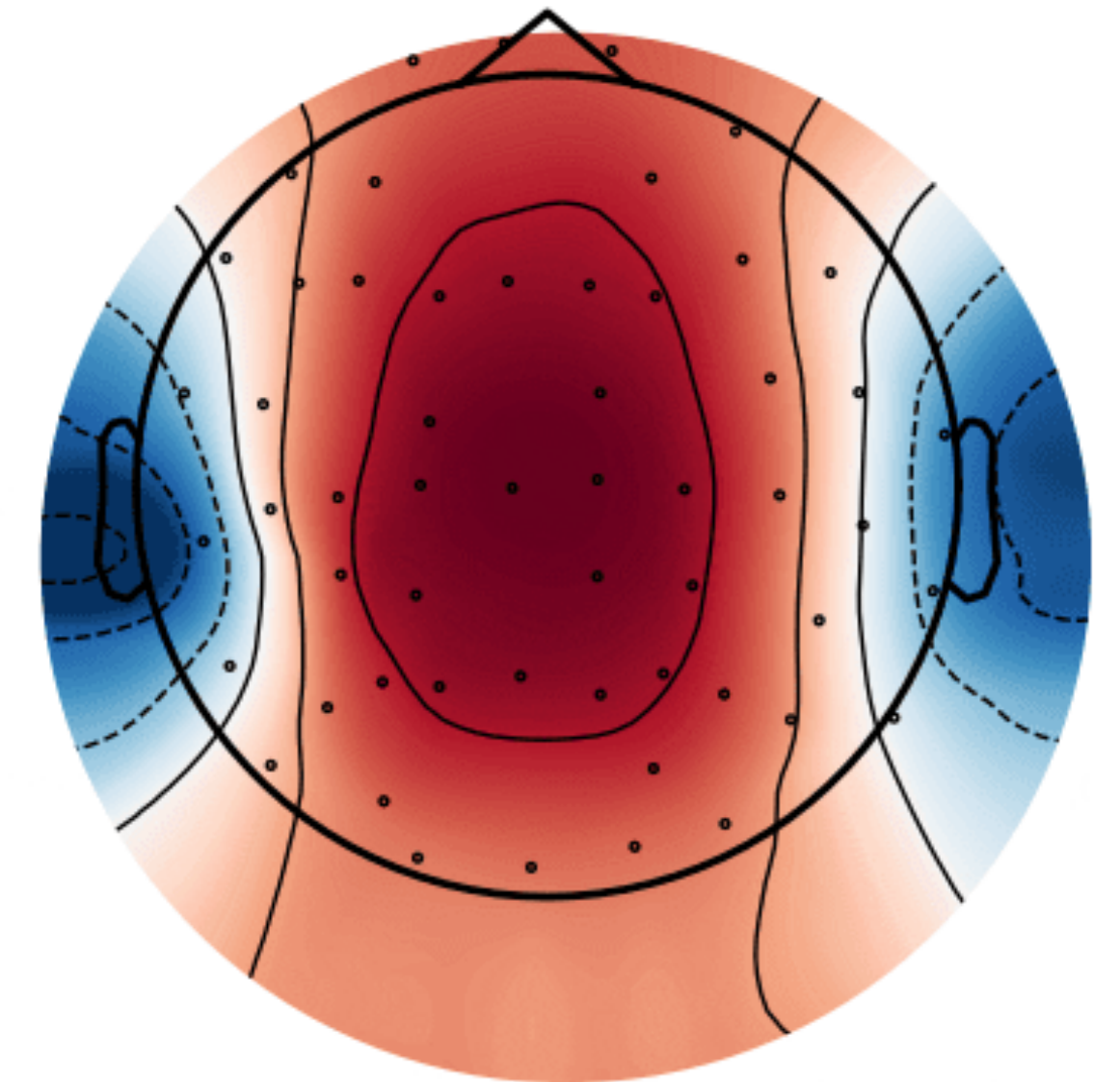
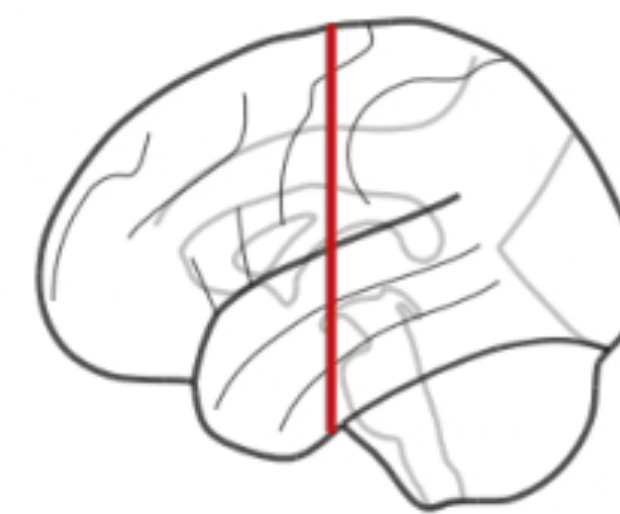
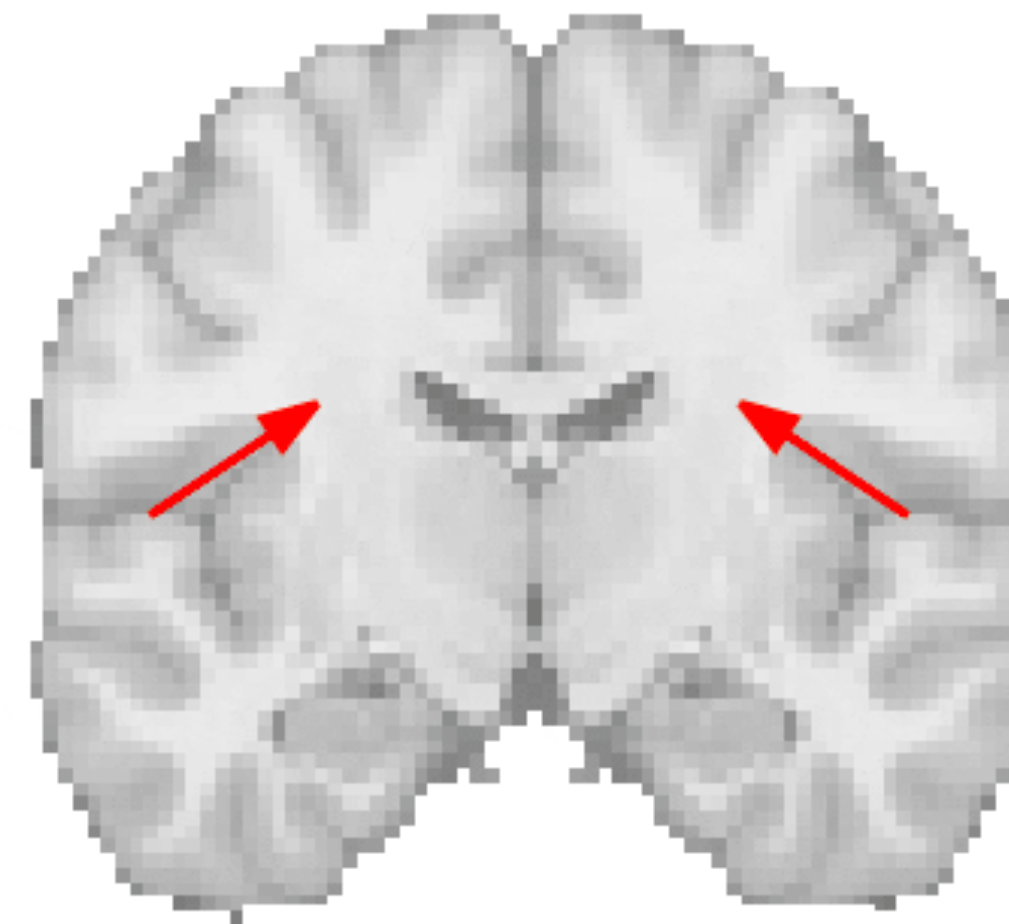


EEG is a mixture of different signals – simulation



how do auditory sources end up on Cz? – simulation

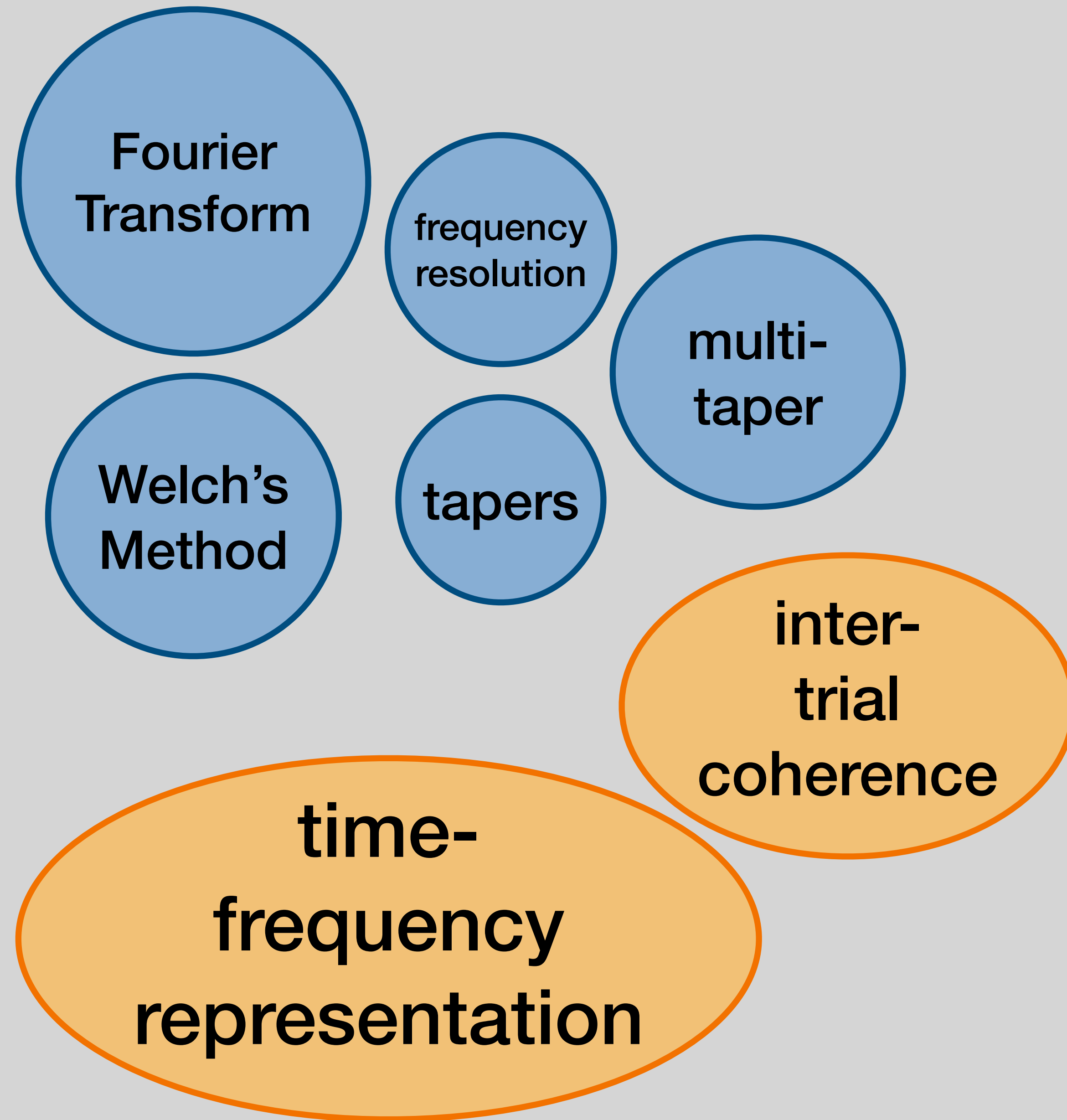
- depending on structure + dynamics, activation can show up on sensor locations that are very far away from source locations



EEG
electrodes

tomorrow: source
estimation lectures +
hands on!

computation



interpretation

